

It's the Sound, not the Pulse: Peripheral Magnetic Stimulation Reduces Central Sensitization through Auditory Modulatory Effects

Reviewed Preprint

v1 • December 6, 2024

Not revised

Spencer S Abssy, Natalie R Osborne, Evgeny E Osokin, Rossi Tomin, Liat Honigman, James S Khan, Nathaniel W De Vera, Andrew Furman, Ali Mazaheri, David A Seminowicz, Massieh Moayed 

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada • Department of Anesthesiology and Pain Medicine, University of Toronto, Toronto, Canada • Mount Sinai Hospital, Toronto, Canada • University of Maryland School of Medicine, College Park, USA • University of Birmingham, Birmingham, UK • Department of Medical Biophysics, Schulich School of Medicine & Dentistry, University of Western Ontario, London, Canada • University of Toronto Centre for the Study of Pain, Toronto, Canada • Division of Clinical & Computational Neuroscience, Krembil Brain Institute, University Health Network, Toronto, Canada

 https://en.wikipedia.org/wiki/Open_access

 Copyright information

eLife Assessment

Abssy et al. carried out a study to test the effects of repetitive peripheral magnetic stimulation (rPMS) on pain perception in an experimental pain model and concluded that the analgesic properties of rPMS could be largely attributed to its auditory component rather than peripheral nerve stimulation per se. While the study presents **valuable** data on the modulation of pain perception in response to the stimulation paradigms that were tested, several issues in the experimental design and interpretation of results render the evidence **incomplete** to support their main claims, which should therefore be revised. In that case, these results could be of interest to pain clinicians and researchers.

<https://doi.org/10.7554/eLife.101986.1.sa3>

Abstract

Repetitive peripheral magnetic stimulation (rPMS) is a non-pharmacological, non-invasive analgesic modality with limited side effects. However, there is a paucity of controlled studies demonstrating its efficacy compared to existing pain management tools. Here, in an initial sample of 100 healthy participants (age 18-40), we compared the analgesic efficacy of two rPMS stimulation protocols—continuous theta burst stimulation (ctbPMS) and intermittent TBS (itbPMS)—against transcutaneous electric nerve stimulation (TENS), a peripheral stimulation technique that is commonly used for pain management. We also included a sham rPMS protocol where participants heard the sound of rPMS stimulation while the coil was placed over their arm, but received no peripheral stimulation. We hypothesized that itbPMS and ctbPMS—but not sham—would reduce pain intensity, pain unpleasantness, and

secondary hyperalgesia evoked by a phasic heat pain (PHP) paradigm on the volar forearm with similar efficacy to TENS. Neither rPMS nor TENS reduced reported pain intensity or unpleasantness ($p > 0.25$). However, ctbPMS and itbPMS significantly reduced the area of secondary hyperalgesia, whereas TENS did not ($F_{3,96} = 4.828$, $p = 0.004$). Unexpectedly, sham rPMS, which involved auditory but no peripheral nerve stimulation, also significantly reduced secondary hyperalgesia compared to TENS. We performed a second study ($n = 32$) to investigate auditory contributions to rPMS analgesia. Masking the rPMS stimulation sound with pink noise eliminated its analgesic effect on secondary hyperalgesia ($p = 0.5$). This is the first study to show that the analgesic properties of rPMS in acute experimental pain may be largely attributed to its auditory component rather than peripheral nerve stimulation.

Introduction

Chronic pain affects between 10 and 50% of the global adult population [59]. Current pain management approaches have significant limitations and there are no interventions that are effective for all patients [47]. Complex procedures such as nerve blocks and implantable neuromodulation devices can reduce chronic pain in some individuals, but these interventions are invasive, costly, and associated with significant side-effects [46]. Non-invasive brain stimulation therapies, such as transcranial magnetic stimulation (TMS), have heterogeneous outcomes and variable long-term efficacy [7]. Pharmacological treatments can be associated with significant side-effects and reduced efficacy over time [2, 43]. Transcutaneous electrical nerve stimulation (TENS) is a common modality for non-invasive treatment of musculoskeletal pain, given its low cost, and the low effort required for use [53]. TENS, however, can only reach superficial tissues [4]. Therefore, there is limited efficacy in existing pain management tools. There is thus a clear need for novel effective pain management tools.

A novel approach of targeting peripheral tissues with focal magnetic pulses—i.e., peripheral magnetic stimulation (PMS)—is becoming an increasingly popular pain management tool [28, 34], largely due to its non-invasive nature and tolerability to physical sensations elicited by PMS [28]. Unlike TENS, PMS can reach deep tissues of the body. In particular, repetitive PMS (rPMS) with theta-burst stimulation (TBS) is of particular interest. Theta oscillations are between 4 and 8 Hz, and TBS is delivered at 5 Hz. The TBS model was developed to mimic hippocampal LTP/LTD firing patterns [25], and theta rhythms play a key role in memory functions [10, 20, 23], but their role in pain is less well understood.

A case study by our group reported that repetitive PMS (rPMS) significantly reduced clinical pain in a patient with intractable glossopharyngeal neuralgia [29]. Another study showed that rPMS can modestly reduce pain and improve functional recovery in patients with acute low back pain, compared to a sham rPMS protocol [35]. Moreover, rPMS outperformed sham treatment in patients with low back pain in functional improvement [35].

While rPMS shows promise, there haven't been good clinical studies with proper controls [38]. This is essential given that rPMS emits rhythmic auditory stimulation, which has been associated with neural entrainment. Indeed, evidence indicates that neural entrainment by rhythmic auditory stimuli can be analgesic [3, 13]. Put another way, it is unknown whether the effects of rPMS are driven by the somatic stimulation of peripheral nerves, or by auditory entrainment.

Here, we explore whether rPMS can significantly reduce pain evoked by a phasic experimental heat pain model. Our first aim is to compare whether different rPMS stimulation parameters can reduce pain intensity, unpleasantness, and the area of secondary hyperalgesia, compared to TENS and a sham condition. To account for potential confounding factors, we also conduct a control

study to assess the impact of the sounds emitted by the magnetic stimulation device during TBS on rPMS analgesia. Additionally, we examine whether there are sex differences in rPMS analgesia by performing sex-disaggregated analyses

Methods

Sample Size Determination

Based on a pilot study with a sample size of $n=5$, we showed that intermittent theta burst PMS (itbPMS; see below for stimulation parameters) reduces pain intensity, pain unpleasantness and secondary hyperalgesia with effect sizes of Cohen's $f=0.63, 0.81$ and 1.3 , respectively. Considering the smallest of these effect sizes, the estimated sample size required to achieve 80% power with an $\alpha=0.0167$ (corrected for 3 outcome measures, with a non-sphericity correction of $0=0.87$, and a correlation amongst representative measures of $R^2=.39$) is 44 participants, using G*Power (v3.1.9.6, Heinrich-Heine-Universität Düsseldorf, Düsseldorf, Germany). Therefore, we need a minimum of 44 participants across 4 intervention arms who complete the study. Furthermore, to perform disaggregated analyses to assess sex differences we doubled the minimum required sample size. We oversampled to ensure we met a minimum of 88 participants for the study, and to account for individuals lost to follow-up or those who withdraw from the study.

Participants

Study 1

A total of 123 healthy participants aged between 18-40 years agreed to participate in the study approved by the University of Toronto Human Research Ethics Board (Protocol# 41856). Exclusion criteria were (1) self-report of neurological, psychiatric or rheumatological disease, including a history of seizures; (2) history of chronic pain; (3) history of chronic illness; (4) clinically significant scores on the Beck's Depression Inventory (>21), which indicates moderate depression or indication of suicidal ideation (>1 on item 9); (5) <28 on Mini Mental State Exam (6) pregnancy and breastfeeding; (7) heat pain ratings $>50/100$ for multiple temperatures $<40^{\circ}\text{C}$ (which indicates hypersensitivity); (8) consistent heat pain rating $<20/100$ for 48°C (which indicates hyposensitivity); (9) inconsistent ratings during the search protocol (i.e., vastly different ratings ($>20/100$ difference) for the same stimulus intensity, or ratings that do not show increases with increased stimulus intensity); (10) pacemaker or any contraindication to receiving magnetic stimulation; (11) use of medication known to affect pain sensitivity (e.g., NSAIDs, anxiolytic, antispastic, acetaminophen) within 24 hours of testing; (12) visible scarring on the volar forearm testing area; and (13) previous experiences with TMS or PMS. Of these 123 participants, 23 were excluded due to hyposensitivity ($n=8$), scored >21 on the BDI or reported suicidal ideation ($n=3$), withdrew ($n=2$), scars on stimulation site ($n=3$), inconsistent pain ratings in the pain calibration stage ($n=2$; see below), missing data ($n=2$), lost to follow-up ($n=2$), and hypersensitivity ($n=1$). The final sample included in this study comprised 100 healthy participants. Figure S1 provides a CONSORT chart of participant recruitment and intervention arm allocation.

Study 2

Thirty-two healthy participants aged between 18-40 consented to procedures approved by the University of Toronto Human Research Ethics Board (Protocol# 41856) and were screened for study eligibility, based on the same exclusion criteria as Study 1. Of these, twenty-four participants (12 males and 12 females) met inclusion criteria and were included in the final sample (see Figure S2).

Experimental design

Study 1

Participants underwent two experimental sessions on different days, at least 48 hours apart: a stimulation session and a control session, counterbalanced across subjects (see **Figure 2**). In the first session, after consenting to procedures, participants were first screened for BDI and MMSE exclusion criteria. Next, they completed the Toronto Academic Health Science Network (TAHSN) demographics questionnaire, and the State-Trait Anxiety Inventory (STAI) [48], as evidence suggests that anxiety can affect pain sensitivity. Participants were then pseudo-randomly assigned to an arm of the study.

Participants then underwent two further procedures: a familiarization protocol and a search protocol to identify a stimulus intensity that would elicit a pain intensity rating of 50/100 (P_{50}). Participants then had an EEG cap mounted, and a 5-minute resting EEG recording was taken. Recording was maintained throughout the experiment with markers for each part of the study (note: we report the EEG data collection for completeness, but these are not analyzed as part of this study and will not be further discussed). Next, the location of the median nerve on the volar forearm was identified for all experiments using a search protocol with the magnetic stimulation coil, and the motor threshold was identified. Depending on the session type (control or stimulation), the participant either received PHP at P_{50} , or a stimulation on the volar forearm over the median nerve territory followed by a PHP at P_{50} , respectively. Finally, we measured the area of secondary hyperalgesia elicited by PHP. We then collected another 5-minute resting state EEG recording (not discussed).

Stimulation Randomization Procedure. We used a pseudo-randomized approach to assign participants to one of four stimulation groups (itbPMS, continuous theta burst PMS (ctbPMS), TENS, and sham ctbPMS). The order of the control and stimulation sessions were counterbalanced across participants.

Heat Stimuli

A thermal stimulation device (QSTLab, Strasbourg, France) with a T11 probe was used to deliver heat stimuli to the volar forearm of participants. Four of the five plates were used to deliver heat over a 3x3cm area.

Familiarization

Familiarization consisted of three 7s heat stimuli at three different temperatures (45°C, 43°C, 47°C) with a 15s interstimulus interval. The ramp rate was set at 7°C/s from a baseline of 32°C, to deliver the target temperature for 5.5s before returning to baseline at 7°C/s. This familiarization protocol allowed the experimenter to assess exclusion/inclusion based on pain sensitivity, and familiarized participants to heat stimuli in the noxious range. After each stimulus, participants provided pain intensity and pain unpleasantness ratings using a verbal numerical rating scale (vNRS). The anchors for the pain intensity vNRS were: 0 - “no pain”, and 100 - “worst pain imaginable.” The anchors for the pain unpleasantness vNRS were: 0 - “not unpleasant” and 100 - “most unpleasant imaginable.” Participants were instructed to rate both pain intensity and unpleasantness upon hearing a verbal cue (“Rate Now”) from the experimenter.

Pain 50

We individually calibrated PHP stimuli to 50/100 on the vNRS for each participant. To do so, participants received various temperatures (39°C, 41°C, 43°C, 45°C, 47°C). The ramp rate was set at 2.5°C/s from a baseline of 32°C, and the stimulus was held at target temperature for 20s before

Figure 1.

Summary of experimental procedures for each intervention arm in Study 1.

Participants attended two sessions: a control session and a stimulation session (arms: itbPMS, ctbPMS, Sham, TENS), separated at least 48 hours. The order of sessions was counterbalanced across participants.

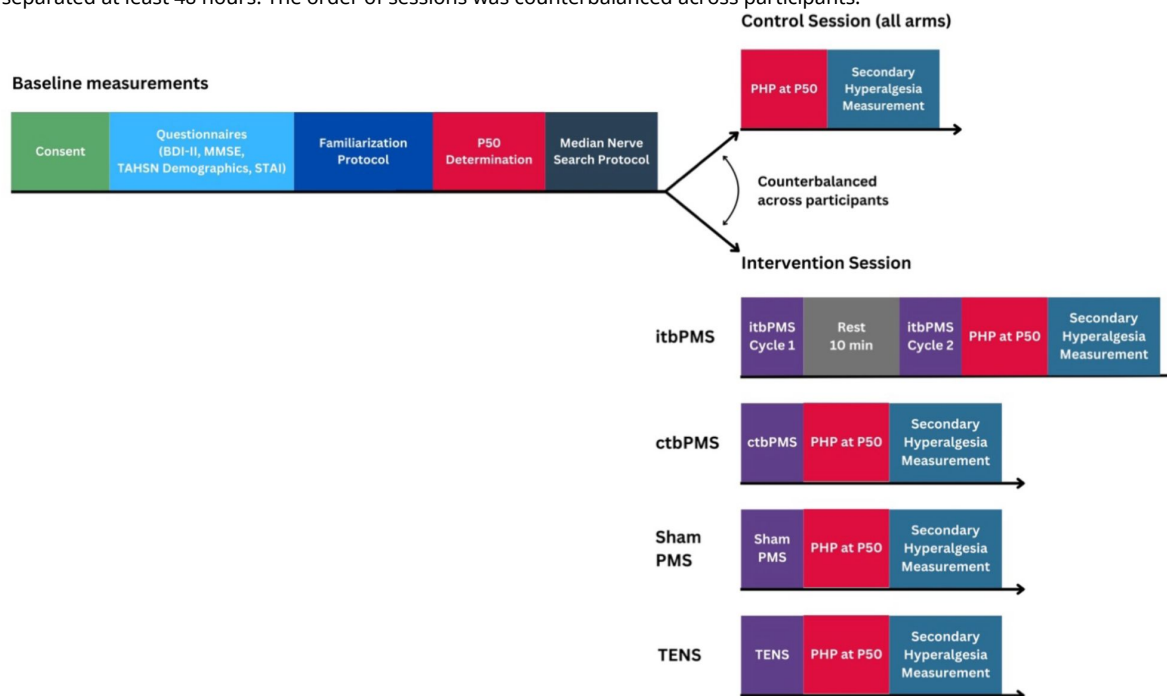
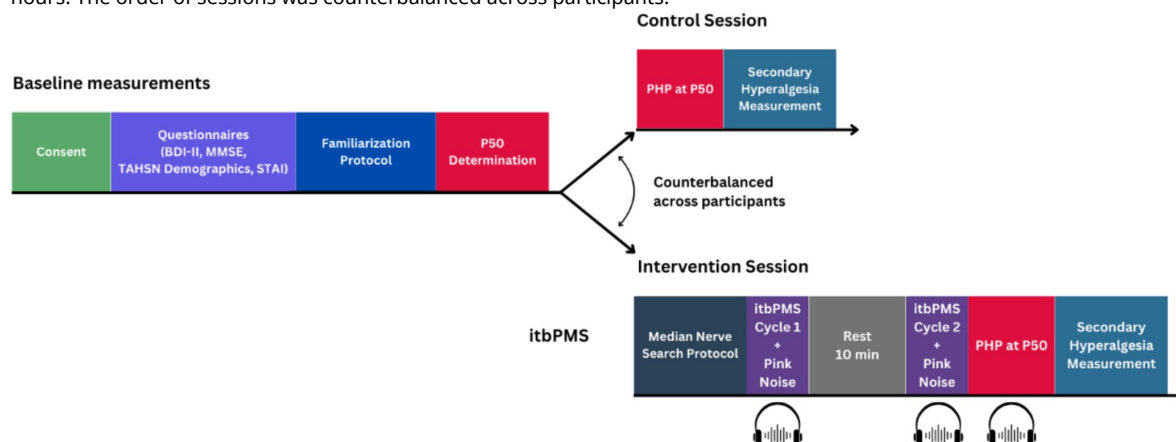


Figure 2.

Summary of experimental procedures for the stimulation session in Study 2.

Participants attended two sessions: a control session and a stimulation session (itbPMS + pink noise), separated by at least 48 hours. The order of sessions was counterbalanced across participants.



returning to baseline at 2.5°C/s, with an interstimulus interval of 10s. Each stimulus (except 47°C) was presented twice, and stimuli were presented in a pseudorandomized order with a rectangular distribution. A sham stimulation was also included (at a baseline of 32°C) to ensure that participants were providing true ratings that reflected the stimuli. Participants provided a pain intensity and pain unpleasantness rating after each stimulus. Stimuli that elicited a rating >80/100 were not repeated to minimize injury. A temperature that elicited 50/100 was used for P₅₀, and was confirmed with a subsequent stimulus.

PHP Protocol

The PHP protocol comprised of five stimuli at P₅₀ presented for 40s with a 20s inter-stimulus interval on the non-dominant volar forearm, as previously done [18]. The stimulus had a ramp rate of 7°C/s and was held at the target temperature for 40s. Pain unpleasantness and pain intensity rating were acquired every 10s during each stimulus.

To minimize habituation during familiarization and P₅₀ protocols, the thermal probe was moved to a new stimulation site on the dominant volar arm. If at any point participants found the pain from the thermal stimuli intolerable, they were instructed to say “stop” and the thermal probe was immediately removed from the arm.

Secondary Hyperalgesia measurement

Secondary hyperalgesia measurement was conducted on the basis of previously published work [40]. Secondary hyperalgesia is defined as the area outside the primary site of stimulation where a noxious mechanical stimulus is felt as hyperalgesic. Punctate mechanical stimuli (256mN PinPrick Stimulator, MRC Systems, Heidelberg, Germany) were used to delineate the border of secondary hyperalgesia. To do so, mechanical stimuli were delivered to the volar forearm along eight orthogonal trajectories radiating from the stimulation site. The stimuli started 6 cm outside the hyperalgesic region and moved toward the stimulation site at 0.5cm increments, until the participant reported an increase in pain sensation. Participants were instructed to report the moment they felt an increase in the sensation of the pinprick. Once they reported the change in sensation, the border was marked, and the procedure was started again along a different trajectory. Trajectories were marked on a digital map, and the area of secondary hyperalgesia was measured in mm² using imageJ [45].

Stimulation

Identification of the Motor Threshold

The motor threshold of the median nerve was identified once a muscle twitch was observed in the innervation territory of the median nerve (e.g., a thumb, middle and index finger twitch). The stimulation intensity was then lowered to find the motor threshold; i.e., when the twitch was barely perceptible. We purposefully used a crude approach for determining the motor threshold to improve translation of the rPMS paradigm/modality to the clinic in future studies.

rPMS Stimulation

rPMS was delivered to the region of the non-dominant volar forearm over the median nerve using a magnetic stimulator (The Magstim Rapid 2+1. Double 70mm AirFilm® Coil (AFC), West Wales, UK). All stimulations were performed at 5% below the motor threshold. The rPMS protocols used in this study comprised of TBS, which refers to a triplet of stimuli presented at 50Hz, repeated at a burst frequency of 5Hz. Two different types of rPMS were used; itbPMS (200 bursts, 1200 pulses total, 41.6 sec cycle time, 2 cycles total, 10 minutes apart) and ctbPMS (500 bursts, 1500 pulses total, 101.0 sec cycle time, 1 cycle total).

Transcutaneous Electrical Nerve Stimulation

TENS was applied to the volar forearm over the median nerve using a high voltage constant current stimulator (Digitimer DS7A, Letchworth Garden City, UK) with small, wired hydrogel electrodes (1 x 1 cm; Electrode Store, Impulse Medical Technologies, Buckley, WA). Electrodes were placed along the proximal-distal axis along the median nerve on the volar forearm, 1.5 cm apart. A train of stimulations was presented using a train delay generator (Digitimer DG2A, Letchworth Garden City, UK). The stimulation intensity was determined by slowly increasing the intensity until the participant reported a painful sensation. Next, the intensity was reduced by 2mA to ensure an intense but non-painful stimulation. The TENS protocol lasted 90s using tonic pulses, with the following parameters: 40Hz, 200 μ s pulse width and the intensity was calibrated to the individual (range: 6-14 mA).

Sham Stimulation

This arm of the study exclusively included participants who were naïve to TMS and rPMS. A concealed speaker was installed in the room, behind the magnetic stimulation device. Auditory ctbPMS stimuli were pre-recorded and the volume and the type of sound resembled that of the rPMS stimulation. The coil was placed over the median nerve on the non-dominant volar forearm, and the magnetic strength was set to 0. Participants did not receive magnetic stimulation but did hear the sound emitted by the magnetic device during a typical ctbPMS stimulation.

Study 2

Participants underwent two experimental sessions on different days, at least 48 hours apart: an itbPMS stimulation session with pink noise and a control session where no stimuli were delivered, the order of which was counterbalanced across subjects (see **Figure 2**). Study 2 follows a similar design as study 1 except that EEG was not collected. In the first session, participants completed the BDI and MMSE for screening purposes. Next, they completed the TAHSN demographics questionnaire, and the STAI. Participants then underwent familiarization and the P₅₀ search protocol to determine PHP stimulus intensity. Next, in the stimulation session only, participants underwent median nerve localization on the volar forearm using a search protocol with the magnetic stimulation coil, and the motor threshold was identified. Depending on the session (control or stimulation) participants then underwent familiarization and either received itbPMS stimulation on the volar forearm over the median nerve territory followed by a PHP at P₅₀, or simply received a PHP at P₅₀. Pain intensity and pain unpleasantness ratings were acquired every 10s during each PHP stimulus. During the itbPMS stimulation and PHP participants heard pink noise through Bose Quiet Comfort II headphones (Framingham, MA). Note that noise cancellation was not turned on. Pink noise is characterized by frequencies in the 40-60Hz range and was played off a YouTube video (<https://www.youtube.com/watch?v=8SHf6wmX5MU&t=343s>; Google, Inc, San Bruno, CA). The intensity of the pink noise was adjusted to participants' comfort while still loud enough to mask the sounds of rPMS delivery. Finally, we measured the area of secondary hyperalgesia elicited by PHP.

Statistical Analyses

Study 1

Questionnaires

We performed a one-way ANOVA with Welch's test for non-equal variances to compare STAI-T, STAI-S, and BDI scores between intervention arms, as differences in these scores could affect pain sensitivity. Significance was set at $p < 0.05$. In cases where there were differences across

intervention arms, the questionnaire measure was included in the models comparing primary outcomes as nuisance covariates.

Differences between intervention arms

All statistical analyses were performed in SPSS (v.28, IBM, Armonk, NY). There were three key outcome measures in the study: (1) change in pain intensity, (2) change in pain unpleasantness and (3) change in secondary hyperalgesia. These change measures are calculated as the stimulation session minus the control session.

We performed three non-parametric ANCOVAs, Quade's test, each with a primary outcome measure (change in pain intensity, change in pain unpleasantness, change in secondary hyperalgesia) across the whole group, as well as sex disaggregated analyses. For the whole group analysis, STAI-T and BDI were modeled as nuisance covariates (see Results-Questionnaires below). For the disaggregated analysis in males, there were no differences in questionnaire measures, and so no nuisance covariates were modeled. For the sex disaggregated analysis in females, STAI-T was significantly different across intervention arms, and was added as a nuisance covariate. Post-hoc independent t-tests were used to determine differences in outcome measures between stimulation types. Statistical significance was set at $p < 0.05$ adjusted for three outcome measures: $p < 0.0167$.

Study 2

Note that as there was only one group for Study 2, we did not perform any statistical comparisons on questionnaires. Descriptive statistics were performed and are presented (see Figure S4). All statistical analyses were performed in SPSS (v.28, IBM, Armonk, NY). There were three key outcome measures in the study: (1) pain intensity, (2) pain unpleasantness and (3) secondary hyperalgesia. To compare these outcome measures between sessions, we performed three paired-sample t-tests (one for each outcome measure). In cases where data were not normally distributed (Shapiro-Wilk's test), a non-parametric Wilcoxon signed-rank test was used. Statistical significance was set at $p < 0.05$ adjusted for three outcome measures: $p < 0.0167$.

We further performed Bayes factor analysis to determine whether the null hypotheses could be accepted (i.e., no change in pain intensity, pain unpleasantness or secondary hyperalgesia between control and stimulation conditions). Bayes factor analysis allows the assessment of relative evidence in favor of either the null or alternative hypothesis: Bayes Factor (BF) < 0.33 is taken as strong evidence of the null hypothesis, and $BF > 3$ is taken as strong evidence in favor of the alternative hypothesis [41]. BFs between 0.33 and 3 are considered to provide no evidence in favor of either hypothesis. The analysis was performed in SPSS v. using the Online Calculator developed by Dienes [12]. To estimate priors, we used the mean difference and the mean standard error from the itbPMS condition from Study 1.

Results

Study 1

Descriptive Statistics

We compared itbPMS, ctbPMS, TENS, and ctbPMS sham (sham) treatments with four independent groups of participants assigned to one of the different interventions. Figure S1 and Table S1 provide a summary of sample demographic data for Study 1. The itbPMS group consisted of 14 males (mean $\pm$ SD age: 25.0 ± 4.10 years) and 12 females (25.1 ± 4.16 years); the ctbPMS group consisted of 14 males (25.7 ± 5.46 years) and 13 females (25.4 ± 5.20 years); the TENS group consisted of 13 males (25.7 ± 5.28 years) and 10 females (26.0 ± 5.01); the sham group consisted of

13 females and 11 males (24.3 ± 5.39 years). Self-reported gender, religious affiliation, and other demographic information can be found summarized in Table S1. Across all arms, the average PHP stimulation temperature used was 45.3 ± 1.5 °C, ranging from 41.0°C - 48.5°C (see Table S2).

Questionnaires

We assessed whether there were differences in the self-report mood questionnaires, BDI-II, STAI-S, and STAI-T at baseline. First, there was no significant difference in BDI-II and STAI-S responses between groups (BDI-II: $W_{3,96} = 2.79$, $p = 0.050$; STAI-S: $W_{3,96} = 2.15$, $p = 0.105$). There was, however, a significant difference between groups in STAI-T baseline characteristics ($W_{3,96} = 3.85$, $p = 0.015$; Table S3).

Sex-disaggregated analysis revealed no significant differences in BDI-II or STAI-S in either males or females. Sex-disaggregated analysis revealed no significant STAI-T differences between males across intervention arms ($W_{3,48} = 2.06$, $p = 0.130$), but did identify a significant difference between females across intervention arms ($W_{3,44} = 3.13$, $p = 0.045$). Given that STAI-T was significantly different between intervention arms, it was included as a nuisance covariate all group comparison models. Furthermore, given that BDI was on the cusp of significance ($p = 0.050$), we felt it prudent to include it as a nuisance covariate. Finally, we did not include STAI-S as a nuisance covariate, given it was not significant in any of the models.

Group Differences

The pain intensity model ($F_{3,96} = 1.390$, $p = 0.251$) and pain unpleasantness model ($F_{3,96} = 0.856$, $p = 0.467$) were not significant, therefore case-wise comparisons were not performed (see **Figure 3**). However, the secondary hyperalgesia model was significant ($F_{3,96} = 4.828$, $p = 0.004$; **Figure 3**). *Post hoc* pairwise comparisons showed significant differences between itbPMS vs TENS ($p = 0.00037$), ctbPMS vs. TENS ($p = 0.011$), and TENS vs sham ($p = 0.011$). In other words, itbPMS, ctbPMS and sham rPMS had significant reductions in the area of secondary hyperalgesia, while TENS had no effect. No other comparisons were significant.

Additionally, we averaged all subject secondary hyperalgesia maps during the control and treatment sessions to visualize the effects of stimulation for the ITBPMS, ctbPMS, TENS, and sham interventions (see **Figure 4**).

Study 2

Table S4 summarizes the sample demographics. This study aimed to investigate whether itbPMS masked by pink noise (PN) could significantly reduce a thermally induced secondary hyperalgesia area compared to control condition—i.e., does masking the sound emitted by rPMS abolish the analgesic effect? The study included 24 participants (mean $\pm$ SD = 20.7 ± 0.62 years): 12 males (20.7 ± 0.62 years) and 12 females (20.8 ± 0.651 years). Self-reported gender, religious affiliation, and race for each participant can be found summarized in Table S4, and summary scores for mood questionnaires (BDI-II, STAI-S, and STAI-T) are provided in Table S5.

We assessed if there were any differences in reported pain intensity, pain unpleasantness, and secondary hyperalgesia area between control and intervention sessions with paired samples *t*-tests. We found no significant changes in intensity ($t = -0.566$, $p = 0.577$) or secondary hyperalgesia ($t = -0.498$, $p = 0.310$; **Figure 5**). Additionally, as unpleasantness was non-parametrically distributed, we used the Wilcoxon signed-rank test and found no significant changes ($W = 187$, $p = 0.304$). We further calculated BF for each of the comparisons. We found evidence for the null hypothesis for pain intensity (BF = 0.051, pain unpleasantness (BF = 0.043), and secondary

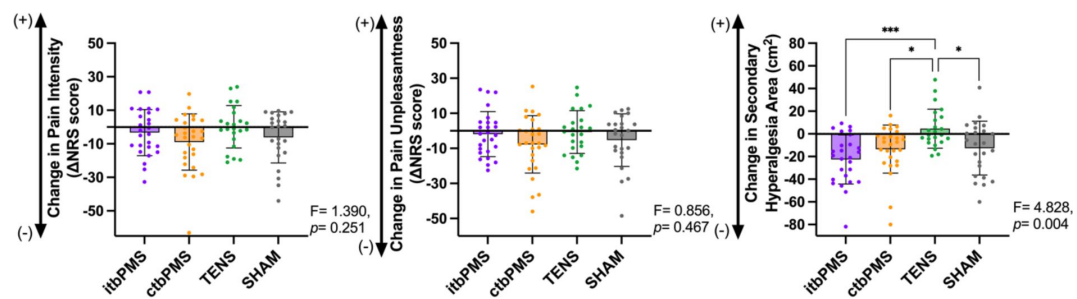


Figure 3

Analysis of intensity, unpleasantness, and secondary hyperalgesia data.

The changes in NRS scores were represented as difference in (intervention – control session) for all intervention arms. Significance is shown with stars (*p<0.05, *** p<0.001). No other comparisons were significant.



Figure 4

Average secondary hyperalgesia map of all conditions within each intervention arm.

The area of secondary hyperalgesia from the intervention session (colored lines) and control session (black) are shown on radial plots in cm. Standard error of the mean is shown in grey for control session, and in color for the stimulation session.

hyperalgesia ($BF=7.70 \times 10^{-8}$). In other words, there were no differences in any of the outcome measures between the control and stimulation conditions. Sex-disaggregated analyses also revealed no significant changes in any outcome measures.

Discussion

This study represents the largest controlled investigation of rPMS analgesia for experimental pain to date. We compared the analgesic efficacy of two rPMS stimulation protocols (ctbPMS and itbPMS) against TENS, a peripheral stimulation technique that is commonly used for pain management worldwide. Importantly, we also included a sham rPMS protocol where TMS and PMS naïve participants heard the itbPMS stimulation sound as it was placed over their arm but received no actual magnetic stimulation. We hypothesized that itbPMS and ctbPMS — but not sham — would reduce pain intensity, pain unpleasantness, and secondary hyperalgesia evoked by a phasic heat pain (PHP) paradigm with similar efficacy to TENS. Contrary to our hypothesis, none of the rPMS stimulations or TENS reduced reported pain intensity or unpleasantness. However, ctbPMS and itbPMS significantly reduced the area of secondary hyperalgesia created by the PHP, whereas TENS — which is considered the clinical standard for non-invasive, non-pharmaceutical pain relief — did not. Unexpectedly, sham rPMS, which involved auditory but no peripheral nerve stimulation, also significantly reduced secondary hyperalgesia compared to TENS. This finding suggested that the sham had greater analgesic effectiveness than TENS, a clinically established but inaudible treatment. This led us to design a second study specifically investigating the auditory contributions to rPMS analgesic effects. We discovered that masking the rPMS stimulation sound with pink noise eliminated its modulatory effect on secondary hyperalgesia. Our results suggest that rPMS can reduce experimentally induced secondary hyperalgesia (a marker of central sensitization) and the analgesic properties of rPMS seem to be driven primarily by auditory rather than peripheral nerve stimulation.

Our study included three pain outcome measures: self-reported pain intensity and pain unpleasantness, and the area of secondary hyperalgesia elicited by PHP. In contrast with previous experimental studies of rPMS [29,35,39], we did not see a reduction in pain intensity nor pain unpleasantness following rPMS stimulation. Our key outcome measure was secondary hyperalgesia, a hallmark of central sensitization, where the region around the site of injury becomes more sensitive to noxious stimuli. The area of secondary hyperalgesia is thought to reflect the degree of sensitization of the second order neurons in the spinal cord [21,30,52]. Therefore, we used the size of secondary hyperalgesia area as a measure of how effective each of our five interventions were at preventing or reducing central sensitization, as this could potentially be used as a tool to prevent the transition to persistent and/or chronic pain [32,57]. For example, one study found that the area of secondary hyperalgesia has been associated with the severity of postsurgical pain in individuals undergoing abdominal surgery [14]. They further reported that treatment groups with larger postsurgical areas of secondary hyperalgesia had longer lasting pain up to one year post-surgically [33]. Interestingly, the authors found that pain intensity measurements were not significantly correlated with the reduction in secondary hyperalgesia area, indicating that they are likely capturing different aspects of the pain experience, and have different underlying mechanisms.

Although using measures of secondary hyperalgesia in experimental studies in healthy adults is relatively uncommon, we are not the first to use this outcome to measure therapeutic outcomes. For example, Salomons and colleagues found that a multi-day cognitive behavioral intervention significantly reduced the area of secondary hyperalgesia induced by a series of painful thermal stimuli and was also associated with reduced pain catastrophizing [42]. Similarly, Meeker and colleagues found that anodal motor cortex transcranial direct current stimulation (tDCS) reduced areas of secondary hyperalgesia through modulation of the descending pain modulatory network [37]. Finally, Iannetti and colleague found that gabapentin was associated with reduced activity

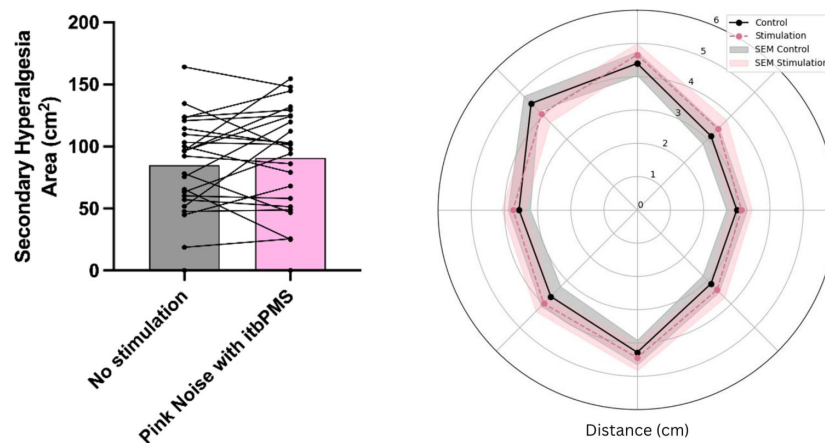


Figure 5

Within-subject comparison of baseline (no stimulation) and itbPMS stimulation with pink noise.

No significant changes in secondary hyperalgesia ($p=0.501$) were reported when participants received no stimulation compared to itbPMS with pink noise. The bar chart (left panel) indicates the mean value of each session, and each line represents a participant. The area of secondary hyperalgesia (right panel) from the intervention session (colored lines) and control session (black) are shown on radial plots in centimeters. Standard error of the mean is shown in grey for control session, and in pink for the itbPMS+pink noise condition.

in the brainstem only when participants experienced experimentally induced central sensitization, measured through the area of secondary hyperalgesia [26]. Together, these studies indicate that secondary hyperalgesia is a modifiable clinically relevant outcome measure, which provides an indirect measure of central sensitization. Such insights can aid in development of targeted therapies aimed at reducing central sensitization and, consequently, chronic pain.

In this study, we used a theta-burst stimulation. Theta oscillations are between 4 and 8 Hz, and theta burst stimulation is delivered at 5 Hz. Theta rhythms play a key role in memory functions [10,20,23], but their role in pain is less well understood. In chronic pain, theta oscillations have higher power compared to healthy individuals [15,44,56]. Notably, two studies found that patients with intractable neuropathic pain had increased theta power, and after effective treatment with thalamic lesioning, theta oscillations normalized [44,49]. Furthermore, evidence suggests that cortical theta burst stimulation can alleviate diabetic neuropathic pain [50]. However, the location of stimulation (the primary motor cortex or the dorsolateral prefrontal cortex) did not affect outcomes, supporting the concept that the auditory component of the stimulation may be driving the observed effects, in line with our study.

The neural mechanism by which the sound of rPMS reduced central sensitization is unclear. One possibility is that the theta-burst stimulation entrained brain oscillations, i.e., auditory entrainment [31]. Previous studies have shown that entrainment effects can be supramodal [1]—i.e., that entrainment with one modality can affect behaviour associated with another modality. Furthermore, entrainment can affect how sensory inputs are perceived [36]. Most studies investigating brain oscillations and pain have focused on alpha and gamma oscillations as these are often the most prominent oscillation bands found to be associated with pain intensity [9,16–19,22,51,58].

One surprising finding in our study was the ineffectiveness of TENS in reducing pain intensity, pain unpleasantness, or secondary hyperalgesia. Although TENS is often used in clinical pain care, the experimental evidence for its ability to relieve pain varies significantly. Recent meta-analyses [27,54,55] found that TENS reduced pain intensity over placebo TENS, but the results were not consistent across all studies, with significant heterogeneity in the pooled data. The authors concluded that while there is some evidence supporting TENS for acute pain, the quality of evidence is moderate to low due to small sample sizes and methodological limitations.

The relative contributions of peripheral nerve stimulation, distraction by rhythmic auditory stimuli or entrainment, and treatment expectations and placebo to the analgesic effect of rPMS require further investigation. Because rPMS is a non-invasive technique with limited side effects, we believe our sham rPMS condition was effective in simulating the real rPMS condition. Unlike TENS which has direct contact with the skin, the rPMS device in our study does not make physical contact and – depending on the level of stimulation delivered – produced limited perceived sensations of tingling or involuntary flexing of the fingers. These physical indicators of rPMS stimulation were not known to participants as they were naïve to receiving peripheral magnetic stimulation of any kind.

One limitation of the present study is the absence of a measure of participants' expectations about how the stimulation would impact their pain. Previous studies of experimental pain have shown that an individual's expectations regarding an intervention can influence their subsequent pain report [5,6,8], and there is robust clinical evidence in the placebo literature that a patient's expectations about a treatment are correlated with their pain outcomes [11]. However, if these expectations are frequently violated, they have reduced effects [24]. Future studies should include this measure to discern how expectations may modulate analgesic experience. Furthermore, the analgesic efficacy of sham rPMS and the lack of statistically significant analgesia in the pink noise rPMS condition does not preclude some contribution of peripheral nerve stimulation in rPMS analgesia. The stimulation parameters used in our and other rPMS studies are

based on standards from cortical stimulation paradigms, and the ideal parameters for peripheral nerve stimulation have yet to be established. Future work should investigate different levels of stimulation with and without the corresponding accompanying auditory stimulation and include electromyography of the targeted peripheral muscles to establish if peripheral stimulation alone is sufficient to induce analgesia and whether the combination of peripheral and auditory stimulation provides more effective relief than either component in isolation.

There are significant therapeutic advantages to auditory theta burst pain management. First, it would be non-invasive, low-cost, accessible and easy to deliver. It would not require expensive magnetic stimulation devices. Second, the selective effects of theta rhythms on reducing or preventing central sensitization, as observed in this study, could be useful as a peri-surgical prophylaxis to prevent post-surgical persistent pain. However, further work is required to establish the reliability and optimization of theta auditory stimulation for acute pain management.

Overall, this study is the first to show that the analgesic properties of rPMS in acute experimental pain may be largely attributed to its auditory component rather than peripheral nerve stimulation. Characterizing the mechanism through which rPMS induces pain relief in other types of pain (clinical, experimental models of neuropathic pain) is an important step before its translation into clinical practice. As rPMS has gained increasing attention as an attractive alternative to current pharmacological treatments because its non-invasive and has few side effects, more high-quality controlled studies are needed to disentangle the mechanisms underlying rPMS-induced pain relief. Indeed, if auditory theta-range stimuli are effective at reducing central sensitization, then the study of underlying mechanisms warrants further investigation, as it presents a low-cost, easy pain management solution.

Data availability statement

Data are included in the supplement of the manuscript.

Statement of Contributions

EEO, NO, SSA: Study design, data collection, analysis, writing

RT, NWDV: data collection, editing

JSK, LH, AF, AM, DAS: Study design, review, editing

MM: Conception of study, funding, analysis, editing, approval of final manuscript

Acknowledgements

EE Osokin was funded by a Medical Institute of Berezina Sergey Scholarship. M Moayed is supported by a University of Toronto Centre for the Study of Pain — Pain Scientist Award, a Canada Research Chair (Tier 2) in Pain Neuroimaging, and the Bertha Rosenstadt Endowment Fund at the Faculty of Dentistry, University of Toronto. The authors have no conflicts to report. This study was funded through Moayed's discretionary funds. SS Abssy is supported by University of Toronto Excellence Award.

Dr. Liat Honigman, who is a co-author on this paper, was a beloved lab member and research associate in the Centre for Multimodal Sensorimotor and Pain Research (CMSPR) at the University of Toronto. She died on March 28, 2024. This, and many other projects in the lab would not have been possible without her expertise, guidance, and support. Liat was kind, smart, and a mentor to many trainees in the CMSPR. She held the highest standards for science, but believed in a compassionate approach to research. She is truly missed.

References

- [1] Albouy P, Martinez-Moreno ZE, Hoyer RS, Zatorre RJ, Baillet S (2022) **Supramodality of neural entrainment: Rhythmic visual stimulation causally enhances auditory working memory performance** *Sci Adv* **8**
- [2] Antman EM, Bennett JS, Daugherty A, Furberg C, Roberts H, Taubert KA, American Heart A (2007) **Use of nonsteroidal antiinflammatory drugs: an update for clinicians: a scientific statement from the American Heart Association** *Circulation* **115**:1634–1642
- [3] Arendsen LJ, Henshaw J, Brown CA, Sivan M, Taylor JR, Trujillo-Barreto NJ, Casson AJ, Jones AKP (2020) **Entraining Alpha Activity Using Visual Stimulation in Patients With Chronic Musculoskeletal Pain: A Feasibility Study** *Front Neurosci* **14**
- [4] Ariel E, Ratmanský M, Levkovitz Y, Goor-Aryeh I (2019) **Efficiency of Tissue Penetration by Currents Induced by 3 Electrotherapeutic Techniques: A Comparative Study Using a Novel Deep-Tissue Measuring Technique** *Phys Ther* **99**:540–548
- [5] Atlas LY (2023) **How Instructions, Learning, and Expectations Shape Pain and Neurobiological Responses** *Annu Rev Neurosci* **46**:167–189
- [6] Atlas LY, Wager TD (2012) **How expectations shape pain** *Neurosci Lett* **520**:140–148
- [7] Beaulieu LD, Schneider C (2015) **Repetitive peripheral magnetic stimulation to reduce pain or improve sensorimotor impairments: A literature review on parameters of application and afferents recruitment** *Neurophysiol Clin* **45**:223–237
- [8] Bingel U, Wanigasekera V, Wiech K, Ni Mhuircheartaigh R, Lee MC, Ploner M, Tracey I (2011) **The effect of treatment expectation on drug efficacy: imaging the analgesic benefit of the opioid remifentanyl** *Sci Transl Med* **3**
- [9] Bott FS, Nickel MM, Hohn VD, May ES, Gil Avila C, Tiemann L, Gross J, Ploner M (2023) **Local brain oscillations and interregional connectivity differentially serve sensory and expectation effects on pain** *Sci Adv* **9**
- [10] Buzsáki G (2002) **Theta oscillations in the hippocampus** *Neuron* **33**:325–340
- [11] Colloca L, Sigaucho M, Benedetti F (2008) **The role of learning in nocebo and placebo effects** *Pain* **136**:211–218
- [21] Hansen MS, Wetterslev J, Pipper CB, Ostervig R, Asghar MS, Dahl JB (2016) **The Area of Secondary Hyperalgesia following Heat Stimulation in Healthy Male Volunteers: Inter- and Intra-Individual Variance and Reproducibility** *PLoS One* **11**
- [22] Heitmann H, Gil Avila C, Nickel MM, Ta Dinh S, May ES, Tiemann L, Hohn VD, Tolle TR, Ploner M (2022) **Longitudinal resting-state electroencephalography in patients with chronic pain undergoing interdisciplinary multimodal pain therapy** *Pain* **163**:e997–e1005
- [23] Herweg NA, Solomon EA, Kahana MJ (2020) **Theta Oscillations in Human Memory** *Trends Cogn Sci* **24**:208–227

- [24] Hird EJ, Charalambous C, El-Deredy W, Jones AKP, Talmi D (2019) **Boundary effects of expectation in human pain perception** *Sci Rep* **9**
- [25] Huang YZ, Rothwell JC (2007) **Theta Burst Stimulation** *Transcranial Brain Stimulation for Treatment of Psychiatric Disorders, Vol. 23* Basel: Karger
- [26] Iannetti GD, Zambreanu L, Wise RG, Buchanan TJ, Huggins JP, Smart TS, Vennart W, Tracey I (2005) **Pharmacological modulation of pain-related brain activity during normal and central sensitization states in humans** *Proc Natl Acad Sci U S A* **102**:18195–18200
- [27] Johnson MI, Paley CA, Jones G, Mulvey MR, Wittkopf PG (2022) **Efficacy and safety of transcutaneous electrical nerve stimulation (TENS) for acute and chronic pain in adults: a systematic review and meta-analysis of 381 studies (the meta-TENS study)** *BMJ Open* **12**
- [28] Kanjanapanang N, Chang KV (2024) **Peripheral Magnetic Stimulation**. StatPearls *Treasure Island (FL)*
- [29] Khan JS, Westwood D, Moayed M (2023) **Ultrasound-guided repetitive pulsed peripheral magnetic stimulation provides pain relief in refractory glossopharyngeal neuralgia: A case report** *Can J Pain* **7**
- [30] Klede M, Handwerker HO, Schmeltz M (2003) **Central origin of secondary mechanical hyperalgesia** *Journal of Neurophysiology* **90**:353–359
- [31] Lakatos P, Gross J, Thut G (2019) **A New Unifying Account of the Roles of Neuronal Entrainment** *Curr Biol* **29**:R890–R905
- [32] Latremoliere A, Woolf CJ (2009) **Central sensitization: a generator of pain hypersensitivity by central neural plasticity** *J Pain* **10**:895–926
- [33] Lavand'homme P, De Kock M, Waterloos H (2005) **Intraoperative epidural analgesia combined with ketamine provides effective preventive analgesia in patients undergoing major digestive surgery** *Anesthesiology* **103**:813–820
- [34] Leung A, Fallah A, Shukla S (2014) **Transcutaneous magnetic stimulation (TMS) in alleviating post-traumatic peripheral neuropathic pain States: a case series** *Pain Med* **15**:1196–1199
- [35] Lim YH, Song JM, Choi EH, Lee JW (2018) **Effects of Repetitive Peripheral Magnetic Stimulation on Patients With Acute Low Back Pain: A Pilot Study** *Ann Rehabil Med* **42**:229–238
- [36] Mazaheri A, Jensen O (2010) **Rhythmic pulsing: linking ongoing brain activity with evoked responses** *Frontiers in human neuroscience* **4**
- [37] Meeker TJ, Keaser ML, Khan SA, Gullapalli RP, Seminowicz DA, Greenspan JD (2019) **Non-invasive Motor Cortex Neuromodulation Reduces Secondary Hyperalgesia and Enhances Activation of the Descending Pain Modulatory Network** *Front Neurosci* **13**
- [38] (2023) **Park S, Park R, Westwood D, Moayed M, Khan JS., 2023.**
- [40] Pedersen JL, Kehlet H (1998) **Secondary hyperalgesia to heat stimuli after burn injury in man** *Pain* **76**:377–384

- [42] Salomons TV, Moayed M, Erpelding N, Davis KD (2014) **A brief cognitive-behavioural intervention for pain reduces secondary hyperalgesia** *Pain* **155**:1446–1452
- [43] Sansone RA, Sansone LA (2009) **Tramadol: seizures, serotonin syndrome, and coadministered antidepressants** *Psychiatry (Edgmont)* **6**:17–21
- [44] Sarnthein J, Jeanmonod D (2008) **High thalamocortical theta coherence in patients with neurogenic pain** *Neuroimage* **39**:1910–1917
- [45] Schneider CA, Rasband WS, Eliceiri KW (2012) **NIH Image to ImageJ: 25 years of image analysis** *Nature methods* **9**:671–675
- [46] Shanthanna H, Bhatia A, Radhakrishna M, Belley-Cote E, Vanniyasingam T, Thabane L, Busse JW (2020) **Interventional pain management for chronic pain: a survey of physicians in Canada** *Can J Anaesth* **67**:343–352
- [47] Shueb SS, Nixdorf DR, John MT, Alonso BF, Durham J (2015) **What is the impact of acute and chronic orofacial pain on quality of life?** *J Dent* **43**:1203–1210
- [48] Spielberger CD (1983) **Manual for the state/trait anxiety inventory (form Y): (self evaluation questionnaire)** Palo Alto: Consulting Psychologists Press
- [49] Stern J, Jeanmonod D, Sarnthein J (2006) **Persistent EEG overactivation in the cortical pain matrix of neurogenic pain patients** *Neuroimage* **31**:721–731
- [50] Thakkar B, Peterson CL, Acevedo EO (2024) **Single Session Effects of Prolonged Continuous Theta Burst Stimulation Targeting Two Brain Regions on Pain Perception in Patients with Painful Diabetic Neuropathy: A Preliminary Study** *J Integr Neurosci* **23**
- [51] Tu Y, Zhang Z, Tan A, Peng W, Hung YS, Moayed M, Iannetti GD, Hu L (2016) **Alpha and gamma oscillation amplitudes synergistically predict the perception of forthcoming nociceptive stimuli** *Hum Brain Mapp* **37**:501–514
- [52] van den Broeke EN, Lenoir C, Mouraux A (2016) **Secondary hyperalgesia is mediated by heat-insensitive A-fibre nociceptors** *J Physiol* **594**:6767–6776
- [53] Vance CG, Dailey DL, Rakel BA, Sluka KA (2014) **Using TENS for pain control: the state of the evidence** *Pain Manag* **4**:197–209
- [54] Vance CGT, Dailey DL, Chimenti RL, Van Gorp BJ, Crofford LJ, Sluka KA (2022) **Using TENS for Pain Control: Update on the State of the Evidence** *Medicina (Kaunas)* **58**
- [55] Walsh DM, Howe TE, Johnson MI, Sluka KA (2009) **Transcutaneous electrical nerve stimulation for acute pain** *Cochrane Database Syst Rev*:C
- [56] Walton KD, Dubois M, Llinas RR (2010) **Abnormal thalamocortical activity in patients with Complex Regional Pain Syndrome (CRPS) type I** *Pain* **150**:41–51
- [57] Woolf CJ, Salter MW (2000) **Neuronal plasticity: increasing the gain in pain** *Science* **288**:1765–1769
- [58] Zhang ZG, Hu L, Hung YS, Mouraux A, Iannetti GD (2012) **Gamma-band oscillations in the primary somatosensory cortex--a direct and obligatory correlate of subjective pain intensity** *J Neurosci* **32**:7429–7438

- [59] Zimmer Z, Fraser K, Grol-Prokopczyk H, Zajacova A (2022) **A global study of pain prevalence across 52 countries: examining the role of country-level contextual factors** *Pain* **163**:1740–1750

Author information

Spencer S Abssy[¶]

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada

ORCID iD: [0009-0001-7044-3566](https://orcid.org/0009-0001-7044-3566)

[¶]Co-first authors (equal contributions)

Natalie R Osborne[¶]

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada

[¶]Co-first authors (equal contributions)

Evgeny E Osokin[¶]

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada

[¶]Co-first authors (equal contributions)

Rossi Tomin

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada

Liat Honigman

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada

James S Khan

Department of Anesthesiology and Pain Medicine, University of Toronto, Toronto, Canada, Mount Sinai Hospital, Toronto, Canada

Nathaniel W De Vera

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada

Andrew Furman

University of Maryland School of Medicine, College Park, USA
ORCID iD: [0000-0001-8055-9610](https://orcid.org/0000-0001-8055-9610)

Ali Mazaheri

University of Birmingham, Birmingham, UK

ORCID iD: [0000-0001-5732-7555](https://orcid.org/0000-0001-5732-7555)

David A Seminowicz

Department of Medical Biophysics, Schulich School of Medicine & Dentistry, University of Western Ontario, London, Canada

ORCID iD: [0000-0003-3111-3756](https://orcid.org/0000-0003-3111-3756)

Massieh Moayed

Centre for Multimodal Sensorimotor and Pain Research, Faculty of Dentistry, University of Toronto, Toronto, Canada, University of Toronto Centre for the Study of Pain, Toronto, Canada, Division of Clinical & Computational Neuroscience, Krembil Brain Institute, University Health Network, Toronto, Canada

ORCID iD: [0000-0002-7324-2540](https://orcid.org/0000-0002-7324-2540)

For correspondence: m.moayed@utoronto.ca

Editors

Reviewing Editor

José Biurrun Manresa

National Scientific and Technical Research Council (CONICET), National University of Entre Ríos (UNER), Oro Verde, Argentina

Senior Editor

Barbara Shinn-Cunningham

Carnegie Mellon University, Pittsburgh, United States of America

Reviewer #1 (Public review):

Summary:

This study from Abssy et al. aims to determine if different non-invasive peripheral stimulation techniques - such as magnetic and electrical stimulations - may influence pain intensity, unpleasantness, and secondary hyperalgesia using a 4-arm parallel-group study. They observed no effect on pain intensity and unpleasantness. Also, they reported that only the TENS (electrical stimulation) did not impact secondary hyperalgesia. They hypothesized that the effects were probably due to the sound emitted by RPMS (magnetic stimulation). In a follow-up study, they tried to determine if covering the sound of RPMS would abolish the effect on secondary hyperalgesia using a single-arm design. They observed no effect of RPMS.

Strengths:

- (1) The research team recruited a relatively large sample size for this type of study.
- (2) The phasic heat pain protocol appears rigorous and well-described.
- (3) The Figures are helpful in facilitating the understanding of the study design and results.
- (4) The statistical analyses appear sound.

Weaknesses:

- (1) The proposed design is not sufficient to answer the research question. The rationale of the study proposed in the introduction is that auditory stimulation may explain the analgesic effects of RPMS. To answer this question, the authors should have used a factorial design using 4 groups (active RPMS + sound; active RPMS + no sound; sham RPMS + sound; sham

RPMS + no sound). Using this design, it would have been possible to determine if the sound, the afferent stimulation, or both are necessary to produce analgesia. Rather, they tested two types of RPMS (iTBS, cTBS) without real rationale, one electrical stimulation and a placebo.

(2) There are multiple ways that the current design could have introduced biases. The study was not randomized but pseudo-randomised. What does that mean? Was their allocation concealment? Was the assessor and data analyst blinded to group allocation? Did an intention to treat analyses were performed? Did the participants were adequately blinded (was it measured)?

(3) The TENS parameters used were not optimal and are not those commonly used in clinical practice. This could have explained the lack of TENS effects. The lack of TENS effects has not been discussed and it is concerning. If TENS had been effective (as expected), the story about the auditory effects would not have been presented as the primary mechanisms underlying the current results.

(4) No primary outcome has been identified. It is important to mention that the interpretation of results is based on the presence of only one statistically significant result. Pain intensity and pain unpleasantness are not affected. This was not properly addressed in the Discussion. What does that mean that secondary hyperalgesia is affected but not pain?

(5) The use of secondary hyperalgesia as a variable requires further clarification. How is it possible to measure secondary hyperalgesia if there is no lesioned tissue? If heat creates secondary hyperalgesia without lesion, what does that mean physiologically? Is it a valid and reliable "pain" variable?

(6) The follow-up study has been designed to cover the RPMS sound using pink noise. However, the pink noise was also present during the PHP measurement. How can we determine whether the absence of change is due to the pink noise during the RPMS or the presence of pink noise during PHP? I don't think this is possible to discriminate.

Appraisal:

(7) Despite all these potential issues, authors interpret their data with high confidence and with several overstatements in the Title, Abstract, and Discussion. The results do not support their conclusions. The fact that auditory stimulation may produce an analgesic effect is a hypothesis, but the current study cannot ascertain it.

<https://doi.org/10.7554/eLife.101986.1.sa2>

Reviewer #2 (Public review):

Summary:

In this article, Abssy, Osokin, Osborne, et al. aimed to demonstrate the effect of Peripheral Magnetic Stimulation (PMS) as a pain relief tool, studying its effects in an experimentally induced pain paradigm applied over healthy subjects. This is a relevant objective, as it will give a proxy indication of its utility as a clinical intervention to treat pain. Shockingly, in the first experiment, the authors found that this effect existed, not only in the active PMS groups but also in the sham PMS. With a clever second experiment, the authors used pink noise to mask the clicking sound and the PMS: this modification abolished the hypoalgesic effect of PMS.

Strengths:

This study presents an adequately calculated sample size ($n = 100$ for study 1 and $n = 32$ for study 2). This gives trustability to the results and allows for a correct disaggregated analysis

to assess gender effects, which correct execution does not often occur. Nuisance variables are adequately addressed, figures and writing are clear, and I especially liked figures 4 and 5 for their easiness of interpretation. They explore two different stimulation protocols for the PMS, extending their results beyond parametrization. Secondary hyperalgesia is a particularly relevant measurement, as it is a common symptom in many relevant painful conditions. Pseudorandomization and counterbalanced design are also appreciated, as well as reinforcement of the results through Bayesian statistical approaches. Regarding the scientific content, the main result (auditory modulation of pain in PMS) is exciting and very interesting by itself and will be relevant for the pain community, granting further research, both from a fundamental and clinical perspective. Personally, I respect that they recognize that results did not match their *a priori* hypothesis, instead of committing HARKing. And it is a very thrilling mismatch for sure!

It will be especially interesting for those among us dedicated to neural stimulation for pain treatment.

Weaknesses:

Although the study presents solid results, some specific concerns make me reluctant to accept the interpretations that the authors take from said results. I list the most important here.

(1) My biggest concern in this paper is that the stimulation protocols are not applied after pain was induced in the subjects, but before. This is not bad in itself, but as the paper presents the stimulations as potential "treatments" it generates a severe mismatch between the objective, context (introduction), and impact (discussion) presented for the experiments, and how they are actually designed. This adds to the fact that healthy volunteers are used here to generate a study with low translational capability, that aims to be translational and provide an indication for clinics (maybe this is why the reduction in pain intensity caused by PMS when applied in patients, reported in references [29, 35 and 39], is not observed here).

(2) TENS treatment duration is simply too short (90s) to be considered a therapeutic TENS intervention. I get that this duration was chosen to match the one of PMS, but TENS is never applied like this in the clinics, in which the duration varies from 10 minutes to an hour (or more). This specific study comparing different durations recommends 40 minutes for knee osteoarthritis pain relief (PMID: 12691335). Under these conditions, this stimulation is more similar to a sham TENS than to a real TENS treatment: I would suggest interpreting it as such. As the paper is right now, it could give the impression that PMS could produce clinical effects not observed in TENS, but while the PMS application resembles a clinical one, the TENS application does not (due to its extremely short duration). As an example, giving paracetamol at a dose 10 times below its effective dose is a placebo, not a paracetamol treatment.

(3) This study measured pain, not central sensitization. Specifically, the effects refer to the area of secondary hyperalgesia. The IASP definition for central sensitization is "Increased responsiveness of nociceptive neurons in the central nervous system to their normal or subthreshold afferent input." (PMID: 32694387). No neuronal results are reported in this article. Therefore, central sensitization is not measured here, and we do not know if it is reduced by sound. This frontally clashes with the title of the article and with many interpretations of the results. For a deep review on this topic, I recommend PMID: 39278607 and the short article PMID: 30416715.

(4) There is no mention of blinding/masking/concealing in this manuscript. Was the therapist blind to whether they applied one protocol, another, or a placebo? Were the evaluators blind, as this can heavily influence their measurements? And the volunteers? Was allocation concealed? Was this blinding measured afterwards? Blinding is, together with randomization, the most important methodological feature for those interventional studies. For example, not introducing blinding and concealing directly makes a study lose 4 out of 10

points in the PEDro scale, failing to fulfill criteria 3, 5, 6, and 7 (<https://pedro.org.au/english/resources/pedro-scale/>). Continuing with methodological considerations, the dropout percentage is high (18% for the first and 25% for the second study), both above the 15% cutoff for criterion 8 of the PEDro, losing another point. It is not mentioned whether the statistical analysis was intention-to-treat or per-protocol. Assuming the second, criterion 9 is failed too. Also, although between-group comparisons are done for study 1, they are not for study 2. Criterion 10 depends on this, so I would recommend doing it to avoid failing it. As it is right now, the study will be a 3/10 on the PEDro scale, being therefore considered "low-quality level evidence". As some of these criteria can be fulfilled in this study, I will recommend doing so to increase its quality level to medium (more in "recommendations for authors").

(5) Data reporting and statistical treatment can be improved, as only differences are reported and regression to the mean is not accounted for in this study. Moreover, baseline levels for the dependent variables (control session) are not accessible for evaluation and they are not compared statistically, making it impossible to know if the groups were similar at baseline. This will imply failing criterion 3 of the PEDro, for a total of 2/10 points.

<https://doi.org/10.7554/eLife.101986.1.sa1>

Author response:

Reviewer 1 (Public Review)

(1) The proposed design is not sufficient to answer the research question. The rationale of the study proposed in the introduction is that auditory stimulation may explain the analgesic effects of RPMS. To answer this question, the authors should have used a factorial design using 4 groups (active RPMS + sound; active RPMS + no sound; sham RPMS + sound; sham RPMS + no sound). Using this design, it would have been possible to determine if the sound, the afferent stimulation, or both are necessary to produce analgesia. Rather, they tested two types of RPMS (iTBS, cTBS) without real rationale, one electrical stimulation and a placebo.

We will clarify that the study design employed was originally designed to determine whether iTBS or cTBS would be more effective to reduce pain. We included TENS as a positive control, and sham as a negative control. We were indeed surprised by the findings, and present them herein. Future RCTs should be performed to reproduce these findings.

(2) There are multiple ways that the current design could have introduced biases. The study was not randomized but pseudo-randomised. What does that mean? Was their allocation concealment? Was the assessor and data analyst blinded to group allocation? Did an intention to treat analyses were performed? Did the participants were adequately blinded (was it measured)?

This study was not designed as an RCT, but rather as experimental study. The study was pseudo-randomized to ensure that the groups had equal allocation and distribution of sexes.

The groups were blinded to the other stimulations (they were not informed of the various arms of the study, through different consent forms).

It was not possible to blind the experimenter as the iTBS and cTBS protocols are very different: iTBS has multiple bursts separated by brief intervals, whereas cTBS is continuous). The data were masked for analysis, and only unblinded at the final stage. We will update the manuscript to reflect these changes.

(3) The TENS parameters used were not optimal and are not those commonly used in clinical practice. This could have explained the lack of TENS effects. The lack of TENS effects has not been discussed and it is concerning. If TENS had been effective (as expected), the story about the auditory effects would not have been presented as the primary mechanisms underlying the current results.

We acknowledge that this is a limitation of the study. A future study should address this. However, we will not remove the arm for transparency.

(4) No primary outcome has been identified. It is important to mention that the interpretation of results is based on the presence of only one statistically significant result. Pain intensity and pain unpleasantness are not affected. This was not properly addressed in the Discussion. What does that mean that secondary hyperalgesia is affected but not pain?

We reiterate that this study was not designed as an RCT, but rather an experimental study with The primary outcomes measures that capture change in were measures of pain sensitivity (pain intensity NRS, pain unpleasantness NRS, and secondary hyperalgesia). We will clarify this in the revised manuscript.

We will now include discussion of the effects being solely on secondary hyperalgesia, and not on pain intensity and unpleasantness.

(5a) The use of secondary hyperalgesia variable is concerning. How is it possible to measure secondary hyperalgesia if there is no lesioned tissue?

Secondary hyperalgesia refers to hyperalgesia assessed in an area adjacent to or remote of the site of stimulation. In general, it is not required to lesion a tissue to activate the nociceptive system or to induce pain. We have cited other studies that have employed secondary hyperalgesia as a pain outcome measure without inducing a lesion.

Hyperalgesia reflects increased pain on suprathreshold stimulation. Then, one measures the subjective response to a painful (i.e. suprathreshold) stimulation, then applies a conditioning stimulation (e.g. heat), and measures the subjective response to the same original stimulus. If the response after conditioning is higher than the baseline measure, hyperalgesia has been induced. Secondary hyperalgesia just refers to hyperalgesia assessed in an area adjacent to or remote of the site of stimulation. In general, it is not required to lesion a tissue to activate the nociceptive system or to induce pain.

(5b) If heat creates secondary hyperalgesia without lesion, what does that mean physiologically?

Secondary hyperalgesia is normally interpreted as a perceptual correlate of central sensitization.

(5c) Is it a valid and reliable "pain" variable?

Yes and yes. A noxious heat stimulus can reliably elicit secondary hyperalgesia (see section 3.2 from Quesada et al. 2021). We also cite several studies that have used secondary hyperalgesia as an outcome measure of central sensitization in pain.

(6) The follow-up study has been designed to cover the RPMS sound using pink noise. However, the pink noise was also present during the PHP measurement. How can we

determine whether the absence of change is due to the pink noise during the RPMS or the presence of pink noise during PHP? I don't think this is possible to discriminate.

We will add a third study that performs the control analysis with the sound of the rPMS masked, but no pink noise otherwise. The study will be performed in two groups: one with pink noise, and one without pink noise.

Appraisal

(7) Despite all these potential issues, authors interpret their data with high confidence and with several overstatements in the Title, Abstract, and Discussion. The results do not support their conclusions. The fact that auditory stimulation may produce an analgesic effect is a hypothesis, but the current study cannot ascertain it.

We believe that the chief concern with the interpretation lies with concerns with the second study. The proposed third experiment will address these concerns.

Reviewer 2 (Public Review):

(1) My biggest concern in this paper is that the stimulation protocols are not applied after pain was induced in the subjects, but before. This is not bad in itself, but as the paper presents the stimulations as potential "treatments" it generates a severe mismatch between the objective, context (introduction), and impact (discussion) presented for the experiments, and how they are actually designed. This adds to the fact that healthy volunteers are used here to generate a study with low translational capability, that aims to be translational and provide an indication for clinics (maybe this is why the reduction in pain intensity caused by PMS when applied in patients, reported in references [29, 35 and 39], is not observed here).

We will reframe these as prophylaxis, rather than treatment. This study was an experimental study originally designed to determine which stimulation parameters (cTBS or iTBS) would be better suited to modulate pain. We performed the study in healthy individuals undergoing acute pain, akin to a person undergoing painful procedure, which could lead to central sensitization and pain persistence (e.g., post-surgical pain). However, before testing this in individuals undergoing actual procedures, it is essential to determine efficacy in people before translation.

Khan et al [29] is a case study with neuropathic pain, whereas our study uses a nociceptive pain model. Lim et al [35] employed 10 sessions of rPMS stimulation in patients with acute low back pain. Similar to our study, the change in VAS driven by rPMS was no different than the sham stimulation. We notice that there is no reference 39, and will correct this.

(2) TENS treatment duration is simply too short (90s) to be considered a therapeutic TENS intervention. I get that this duration was chosen to match the one of PMS, but TENS is never applied like this in the clinics, in which the duration varies from 10 minutes to an hour (or more). This specific study comparing different durations recommends 40 minutes for knee osteoarthritis pain relief (PMID: 12691335). Under these conditions, this stimulation is more similar to a sham TENS than to a real TENS treatment: I would suggest interpreting it as such. As the paper is right now, it could give the impression that PMS could produce clinical effects not observed in TENS, but while the PMS application resembles a clinical one, the TENS application does not (due to its extremely short duration). As an example, giving paracetamol at a dose 10 times below its effective dose is a placebo, not a paracetamol treatment.

We acknowledge that this is a limitation, and will address this in the Discussion of the revised manuscript.

(3) This study measured pain, not central sensitization. Specifically, the effects refer to the area of secondary hyperalgesia. The IASP definition for central sensitization is "Increased responsiveness of nociceptive neurons in the central nervous system to their normal or subthreshold afferent input." (PMID: 32694387). No neuronal results are reported in this article. Therefore, central sensitization is not measured here, and we do not know if it is reduced by sound. This frontally clashes with the title of the article and with many interpretations of the results. For a deep review on this topic, I recommend PMID: 39278607 and the short article PMID: 30416715.

It is widely accepted that central sensitization is the neurophysiological basis of secondary hyperalgesia (see PMID: 11313449; PMID: 10581220).

The reviewer is conflating secondary hyperalgesia due to central sensitization and chronic pain. Whether chronic pain is driven or maintained by central sensitization is not the goal of our study. However, there is ample evidence that nociceptive drive can induce plasticity in the CNS, which alters pain sensitivity, and that these changes facilitate pain.

(4a) There is no mention of blinding/masking/concealing in this manuscript. Was the therapist blind to whether they applied one protocol, another, or a placebo? Were the evaluators blind, as this can heavily influence their measurements? And the volunteers? Was allocation concealed? Was this blinding measured afterwards? Blinding is, together with randomization, the most important methodological feature for those interventional studies. For example, not introducing blinding and concealing directly makes a study lose 4 out of 10 points in the PEDro scale, failing to fulfill criteria 3, 5, 6, and 7 (<https://pedro.org.au/english/resources/pedro-scale/>).

This study was not designed as an RCT, but rather as experimental study. The study was pseudo-randomized to ensure that the groups had equal allocation and distribution of sexes.

The groups were blinded to the other stimulations (they were not informed of the various arms of the study, through different consent forms). However, blinding was not measured afterwards (again, this was not meant to be an RCT).

It was not possible to blind the experimenter as the iTBS and cTBS protocols are very different: iTBS has multiple bursts separated by brief intervals, whereas cTBS is continuous). The data were masked for analysis, and only unblinded at the final stage. We will update the manuscript to reflect these changes.

(4b) Continuing with methodological considerations, the dropout percentage is high (18% for the first and 25% for the second study), both above the 15% cutoff for criterion 8 of the PEDro, losing another point.

In the study, only 2 withdrew after feeling the heat, 2 were lost to follow up, and 2 had incomplete data. That totals 6/123 in Study 1. In study 2, none of the participants that met inclusion/exclusion criteria, and who were 'allocated' to the study were included (0% dropout/data loss).

We are unsure how to address this point, as we had clear inclusion/exclusion criteria, and these could only be measured after consenting. As this is an experimental study performed on healthy individuals in a university setting, we are not able to collect any study related data prior to consent.

We openly reported individuals who did not meet the criteria, and thus were excluded. These criteria are a combination of what is required to collect good quality data, and what we are ethically permitted to do. We understand that in an interventional trial where >15% drop out due to intolerance, or adverse events would indeed be concerning.

(5) Data reporting and statistical treatment can be improved, as only differences are reported and regression to the mean is not accounted for in this study. Moreover, baseline levels for the dependent variables (control session) are not accessible for evaluation and they are not compared statistically, making it impossible to know if the groups were similar at baseline. This will imply failing criterion 3 of the PEDro, for a total of 2/10 points.

This only concerns study 1, as study 2 is a within subject study design. Study 1 provides the raw data in Figure 4. We will provide the raw data for each of the primary outcome measures in a supplemental table in the revision.

<https://doi.org/10.7554/eLife.101986.1.sa0>