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Differential interfacial tension between oncogenic and wild-type populations forms the mechanical basis of tissue-specific oncogenesis in epithelia

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This **important** study reports that an oncogenic population in an epithelium can either be repressed or spread, depending on the tissues. This is explained by hypothesising the existence of a heterotypic tension at the boundary between different cell types, and supported by pharmacological perturbations and numerical simulations using the vertex model. The **solid** study conveys a key message, although some uncertainty remains regarding the origin of the heterotypic tension in relation to acto-myosin organisation in the boundary cells.

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Abstract

Why does the same oncogenic mutation drive tumor formation in some tissues but not in others? While cancer driver mutations are well-documented, their tissue-specific effects remain largely attributed to genetic factors, leaving the biophysical aspects underexplored. Here, we demonstrate that mechanical interactions, specifically interfacial tension between newly transformed and wildtype epithelial cells are critical in determining survival and growth of HRas^{V12} oncogenic mutants in human mammary and bronchial epithelia, leading to contrasting outcomes in the two tissues. In mammary epithelium, isolated oncogenic cells are extruded- a typical mechanism of defense against cancer in epithelia- while oncogenic groups become spatially confined in a kinetically arrested, jammed state, marked by an actomyosin belt at the interface. In contrast, bronchial epithelium permits persistent spreading of the same oncogenic cells, which form long protrusions regardless of colony size. Furthermore, oncogenic clusters in these two tissues exhibit distinct biophysical properties, including variations in cell shapes, intracellular pressure, cell-cell tension, and cellular motility. Using a cell shape-tension coupled bi-disperse vertex model, we reveal that differences in interfacial tension at mutant-wild-type boundaries dictate whether oncogenic cells are eliminated, restrained, or expanded and that modulating interfacial tension alters mutant cell fate within the epithelium. Together, our findings uncover a mechanical basis for tissue-specific oncogenesis by highlighting how differential cellular mechanics at the oncogenic-host cell interface regulate tumor initiation and progression.

Introduction

Cancer has traditionally been understood to be a consequence of deregulated cell proliferation driven by genetic alterations that enable clonal expansion and tumor formation [1]. Interestingly, genomic analysis reveals that many tumor suppressor genes and oncogenes exhibit tissue specificity, meaning they are altered in some cancers but not others [2-4]. Current research suggests that a combination of intrinsic biological factors [4], such as differential epigenetic changes [3,5] and aneuploidy patterns [6-8], as well as extrinsic factors like the tumour microenvironment, including the presence of tissue-specific immune cells [9-10] influences tissue-specific cancer outcomes. However, a relatively underexplored yet crucial aspect of tissue-specific oncogenesis is the mechanical interaction between normal and cancerous cells. To this end, recent studies have highlighted a tumor suppressive behavior in epithelial tissues known as epithelial defense against cancer (EDAC) [11], where transformed cells are expelled from the tissue by surrounding normal cells [12-14]. However, EDAC can fail [14], allowing mutant cells to evade extrusion when the microenvironment becomes tumour-permissive, such as in conditions of increased stiffness [15] or inflammation due to a high-fat diet [16]. The success or failure of EDAC is closely linked to changes in cellular contractility [12-14] and cell-cell adhesions [17], suggesting that the underlying biophysical properties of the tissue play a decisive role in determining the outcome of cell competition. Since these properties can vary across different epithelial tissues, tissue-specific differences in cancer susceptibility may be explained by the varying ability of epithelia to manage newly transformed cells. However, despite these advances, the mechanical basis of tissue-specific oncogenesis remains missing. Specifically, how differences in cellular mechanics at the interface between oncogenic and wild-type populations influence tumor initiation and progression is poorly understood. Addressing this gap could not only enhance our understanding of cancer biology but also open new avenues for tissue-specific therapeutic interventions by identifying what makes certain tissues more permissive to tumor formation.

To this end, we investigated and compared the bio-physical factors influencing early tumorigenesis in human mammary and bronchial epithelial monolayers by sporadically transfecting a subset of healthy cells into oncogenic cells expressing a constitutively active HRas^{V12} protein. We then tracked the fate of these transfected cells and their interactions with the wild-type counterparts in real time via live imaging. Strikingly, HRas^{V12}-mutant cells exhibited contrasting behaviors in the two tissues. In mammary epithelium, isolated transformed cells were frequently extruded. However, when present in groups, extrusion of oncogenic cells was not seen, but instead, they remained spatially confined in a jammed state. In contrast, in bronchial epithelium, single as well as groups of HRas^{V12} expressing cells persisted and exhibited unrestricted expansion over time, regardless of cluster size. To explain these findings, we employed a bi-disperse vertex model of epithelia [18-21] and demonstrated that differences in interfacial tension between wild-type and transformed populations play a crucial role in determining whether mutant cells are eliminated, restrained, or are allowed to persist and expand. Taken together, these findings provide novel insights into the differential outcomes of competitive cellular interactions in the precancer stages and uncover a mechanical basis for tissue-specific oncogenesis.

Results

1. Singlets and groups of HRas^{V12} oncogenic mutants show tissue-specific fates in epithelia

To explore the differences in the premalignant stages across epithelial tissues, we sporadically transfected monolayers of the two non-transformed human epithelial cell lines, MCF10A (mammary) and BEAS2B (bronchial), with a plasmid construct that constitutively expresses HRas^{V12} along with the GFP reporter [Figure 1a [↗](#)]. We then monitored the cellular dynamics over 90 hours. Consistent with previous studies reporting extrusion of single HRas^{V12} mutants in MDCK monolayers [11-15, 22], we observed that isolated HRas^{V12} transfected cells (singlets) surrounded by

wild-type neighbours were extruded from the mammary epithelium [Figure. 1b [↗](#) (upper panel), Supplementary video 1 [↗](#)]. This process correlated with a reduction in shape indices of oncogenic mutants as the density of wild-type cells around them increased [Figure. 1c [↗](#) (upper panel)]. Interestingly, this well-known mechanism of epithelial defense against cancer was impaired in BEAS2B cells, where HRas^{V12} mutants evaded extrusion [Figure. 1b [↗](#) (lower panel), d], and wild-type cell compaction did not restrict their growth [Figure. 1c [↗](#) (lower panel), Supplementary video 1 [↗](#)]. Instead, the mutants in the bronchial epithelium continued to proliferate and exhibited increased elongation with long protrusions [Figure. 1c [↗](#) (lower panel), e, Supplementary video 1 [↗](#)]. Given that cancers frequently arise from fields of oncogenic mutants rather than isolated mutated cells [23-25], we also investigated whether these differential dynamics of mutant singlets would also extend to groups of oncogenic mutants, potentially enabling more aggressive HRas^{V12} growth in bronchial tissue compared to mammary tissue. By adjusting cell seeding conditions, we generated larger groups of HRas^{V12} transfected cells in both MCF10A and BEAS2B monolayers and then tracked the dynamics of these groups over time. In the mammary epithelium, wild-type cells were unable to extrude groups of HRas^{V12}-transfected cells but instead confined them into compact, circular clusters with smooth, rounded interfaces [Figure 1f [↗](#), (upper panel), g (upper panel), Supplementary Video 2 [↗](#)]. As a result, oncogenic clusters gradually demixed from the surrounding wild-type MCF10A population and remained spatially constrained [Figure 1h [↗](#)]. In contrast, HRas^{V12} clusters in the bronchial epithelium gradually spread outward [Figure 1f [↗](#), (lower panel), g (lower panel), Supplementary video 2 [↗](#)], and formed protrusive lamellipodia and developed an irregular interface with surrounding wild-type cells [Figure. 1g [↗](#) (lower panel)]. Together, these striking differences in the dynamics of HRas^{V12} oncogenic cells demonstrate that activation of the same oncogene can lead to distinct outcomes across tissues in terms of growth, spreading, and extrusion. This prompted us to further investigate the unique bio-physical mechanisms driving these variations.

2. Biophysical analysis reveals demixing via jamming of oncogenic clusters in MCF10A but unjamming and protrusive growth in BEAS2B

To understand the mechanisms driving the differential fates of oncogenic fields in the two epithelial tissues, we mapped the bio-physical signatures of wild-type-mutant interactions by subdividing the images into four regions of interests for both monolayers-ROI1: wild type cells distant from oncogenic cells, ROI2: interfacial wild type cells in direct contact with oncogenic cells, ROI3: oncogenic cells at the cluster boundaries in direct contact with wild type cells, and ROI4: oncogenic cells in contact with other oncogenic cells [Figure. 2a [↗](#)]. We then compared the F-actin levels and shapes of both mutant and wild-type populations across these ROIs. Additionally, we employed Bayesian force inference, as previously established [26], to infer the differential tissue stresses associated with cluster formation from the observed cell geometries. Interestingly, the differences across these parameters were apparent not only between wild-type and oncogenic counterparts but also based on the spatial localization of the cells, with cells at the oncogenic-wild type interface exhibiting distinct behaviors, regardless of their origin.

In mammary epithelium, oncogenic clusters were surrounded by a prominent actin belt [Figure. 2b [↗](#) (upper panel), c (upper panel)], coupled with drastically low F-actin levels inside the clusters [Figure. 2b [↗](#) (upper panel), e (left panel)], suggesting that the de-mixing of oncogenic cells in mammary tissue is likely driven by changes in cytoskeletal mechanics. Further, oncogenic clusters in mammary epithelium (ROI4) also exhibited low cell shape indices [Figure. 2d [↗](#) (upper panel), e (right panel)], high internal pressure and low line tension [Figure. 2h [↗](#), j]-characteristics indicative of jamming [27]. In epithelial tissues, the jamming–unjamming transition is closely linked to changes in cell shape [27] and is often quantified using the cell shape index (the ratio of cell perimeter to the square root of area), where lower shape indices correspond to jammed, solid-like states, and higher shape indices reflect unjammed, fluid-like tissue behavior. Notably, both oncogenic cells and wildtype MCF10A cells at the cluster interface (ROI 2 and ROI3) showed F-actin enrichment, while the interfacial wild shape cells show elongated shapes [Figure. 2d [↗](#) (upper

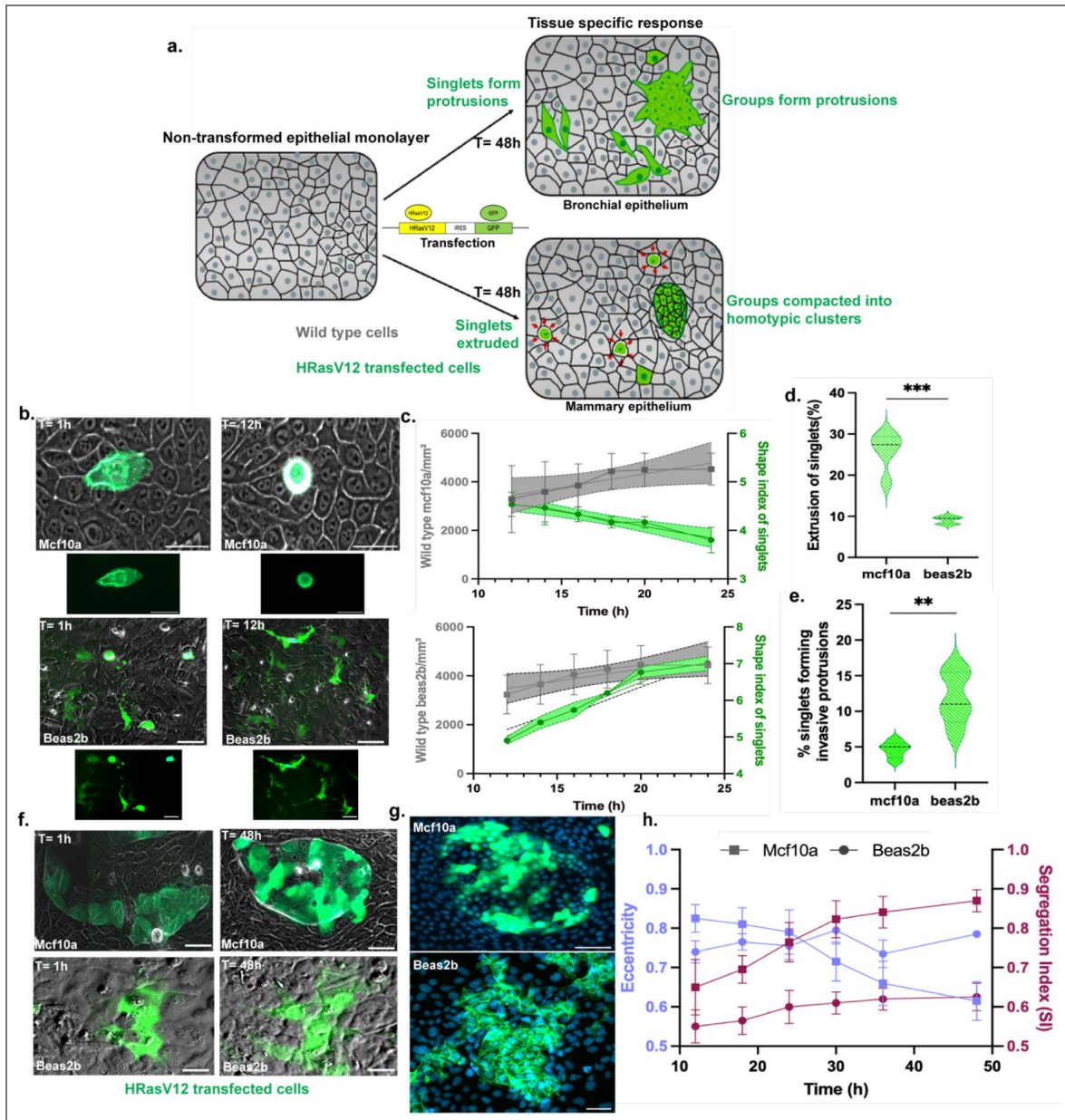


Figure 1. Tissue-specific outcomes of HRas^{V12} oncogenic mutants in epithelial monolayers

(a) Schematic representation of the experimental setup and outcome (b) Representative images showing extrusion of single oncogenic cells (singlets) in mammary epithelium (*upper panel*), but protrusive behavior of the same oncogenic singlets in bronchial epithelium (*bottom panel*) (c) Quantification of shape indices of HRas^{V12} singlets showing a reduction in shape indices, with increasing wild-type cell density in mammary epithelium (*upper panel*), but the opposite trend in bronchial epithelium (*bottom panel*), where HRas^{V12} cells continues to spread. Shaded regions indicate the results simple linear regression analysis with 95% confidence intervals (d) Extrusion rates of HRas^{V12} singlets are significantly higher in mammary epithelium, while (e) Percentage of HRas^{V12} cells forming protrusions is markedly higher in bronchial epithelium. Representative data are plotted from one of three independent experiments with the median shown as a bold dashed line and the first and third quartiles are shown as thin dashed lines. Statistical significance was calculated using Unpaired t-test with Welch's correction. (f) Behaviour of HRas^{V12} oncogenic clusters in the two tissues-In mammary epithelium (*upper panel*), clusters become spatially confined with a smooth, circular interface with the wild-type population, while in bronchial epithelium (*bottom panel*), HRas^{V12} clusters expand, forming long protrusions over time (g) Immunofluorescence images of HRas^{V12} clusters in mammary and bronchial epithelia, highlighting differences in spreading patterns in the two epithelia (h) Quantification of cluster segregation: mammary epithelium exhibits a higher segregation index and reduced eccentricity compared to bronchial epithelium, indicating greater spatial confinement of oncogenic clusters. The segregation index (SI), defined as the average ratio of homotypic and all cell neighbors, quantifies the degree of demixing and is averaged over all cells inside an oncogenic cluster. Data are mean±sem and plotted from different clusters from one representative experiment. (Scale bars= 50 μm)

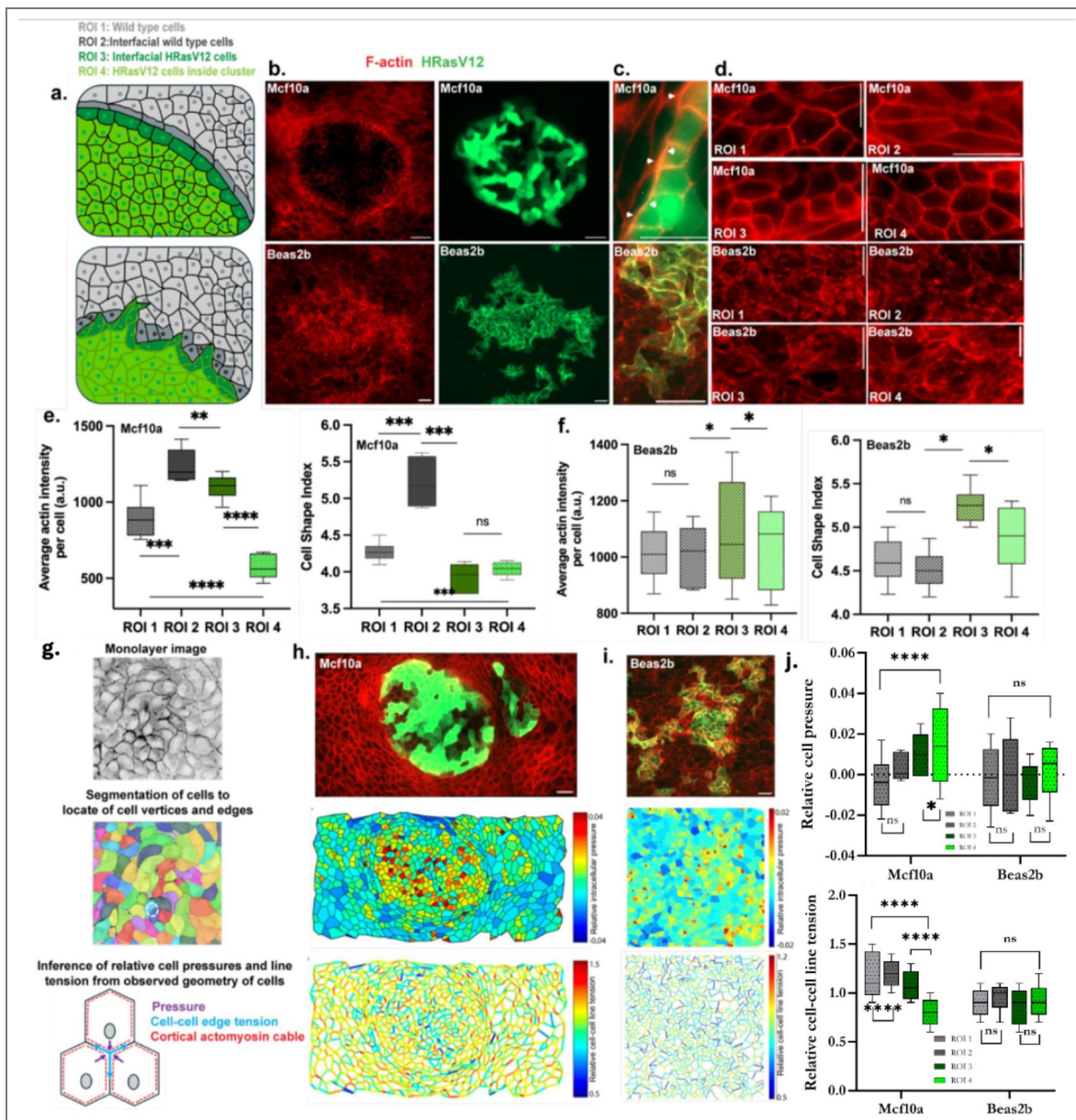


Figure 2. Distinct mechanical signatures of HRas^{V12} clusters in mammary and bronchial epithelia

(a) Representative images showing regions of interest (ROIs) selected for analysis in mammary (*upper panel*) and bronchial epithelia (*lower panel*) (b) Immunofluorescence images of HRas^{V12} clusters stained for F-actin in mammary (*upper panel*) and bronchial epithelia (*lower panel*) (c) Oncogenic cluster–wild-type interface showing distinct actin belt in mammary marked by white arrows (*upper panel*) and absence of it in bronchial epithelia (*lower panel*) (d) ROI-based F-actin stained regions of wild-type and oncogenic cells in mammary (upper panel) and bronchial epithelia (lower panel) revealing distinct shape differences in different regions-in mammary epithelia, wild type cells at the interface show elongated shapes (ROI2), and oncogenic cells inside the cluster show jammed shapes (ROI4), in comparison to wild type cells at a random location (ROI1), while in bronchial epithelia, oncogenic cells (ROI 3 and 4) show more elongated shapes compared to wild-type beas2b cells (e), (f) Quantifications of F-actin intensities and shape indices, in mammary epithelia (e), and bronchial epithelia (f), across the four ROIs confirming jammed oncogenic clusters, with unjamming at the interface, in mammary epithelia and unjammed clusters in bronchial epithelia (g) Schematic illustrating the Bayesian Force Inference pipeline used to estimate relative intracellular pressure and cell-cell edge tension (h) Heatmaps depicting relative cell pressures and cell-cell edge tensions in mammary epithelium, revealing localized mechanical heterogeneity (i) Heatmaps of relative cell pressures and edge tensions in bronchial epithelium, showing a distinct mechanical landscape compared to mammary epithelium (j) Quantification of relative intracellular pressures and cell-cell edge tensions across the four ROIs in mammary (upper panel) and bronchial epithelia (lower panel) highlighting tissue-specific differences. All data represented as mean±sem in box and whisker plots and are plotted from one out of three independent experiments with whiskers extending from the minimum to the maximum values, showing the full range of the dataset including outliers. Line represents the median. Statistical significance was calculated using Unpaired t-test with Welch’s correction. Scale bars= 20 μm

panel), e], indicating that interfacial cellular mechanics play a key role in the de-mixing process as the wild-type cells encircle the oncogenic mutants. This interfacial region enriched with F-actin also contained phosphomyosin [Supplementary Figure. 1a [↗](#)], indicating that a contractile actomyosin belt drives the compaction of oncogenic clusters in mammary epithelia. In contrast, bronchial epithelium exhibited no actin belt formation at the wild type-oncogenic cell interface, and no traits of jamming were observed in the oncogenic clusters [Figure. 2b [↗](#) (lower panel), c (lower panel)]. Instead, oncogenic cells continued to proliferate, displaying elongation measured via higher shape indices and high F-actin expression [Figure. 2d [↗](#) (lower panel), f]-indicative of unjamming behaviour [27,28]. The relative internal cell pressure and cell-cell line tension inferred with Bayesian force inference showed slight or no modulation in the oncogenic clusters, given the general elongated shapes of wild-type cells in BEAS2B cells [Figure. 2i, j [↗](#)]. Together, these findings highlight distinct interfacial mechanics between oncogenic cells and their wild-type neighbors in both MCF10A and BEAS2B monolayers, resulting in differing outcomes in mutant colony growth.

3. PIV analysis reveals kinetic arrest of oncogenic clusters in MCF10A coupled with tangential motion of interfacial cells

To further probe the cellular dynamics that lead to the contrasting fates of the oncogenic mutant colonies in the two tissues, we analyzed cellular velocities during the de-mixing of oncogenic cells, using Particle Image Velocimetry (PIV) on consecutive image pairs from mammary and bronchial monolayers. Interestingly, velocity maps in samples imaged for mutant cluster – wild type dynamics in MCF10A [Supplementary video 3 [↗](#)] revealed an unusual movement pattern at confluency: wild type MCF10A cells exhibited tangential motion around oncogenic clusters [Figure. 3c [↗](#)], which coupled with a drastic reduction in the velocity of oncogenic cells [Figure. 3a [↗](#) (lower panel), d], likely caused their compaction and jamming into clusters. Notably, this tangential movement was unique to wild-type MCF10A cells surrounding oncogenic clusters and was absent in other regions across the monolayer [Figure. 3c [↗](#)] as well as under control conditions-i.e., in the absence of oncogenic mutants [Supplementary video 4 [↗](#)], in both of which a typical velocity drop was observed in MCF10A cells due to density-induced jamming [27-30] [Figure. 3d [↗](#) (upper panel), Supplementary 2]. These results aligned with the observed differences in cell shape indices, where oncogenic clusters underwent jamming, while wild-type cells at the interface exhibited unjamming behavior [29,30]. In contrast, in the bronchial epithelium, mutant clusters remained unjammed, even as surrounding wild-type cells became more crowded [Figure. 3b [↗](#), d (lower panel), Supplementary video 5 [↗](#)]. Additionally, no tangential cellular movement was detected around the oncogenic clusters in the bronchial epithelium. These velocity maps showed negligible deviations from wild type (control) BEAS2B velocity maps [Supplementary video 6 [↗](#)]. Together, these findings suggest that mutant clusters carrying the same oncogene can exhibit drastically different behaviors depending on the epithelial tissue type. Specifically, differences in the dynamics of the interfacial cells drive the demixing and jamming of HRas^{V12} oncogenic cells in mammary epithelium while promoting protrusive, unjammed growth in bronchial epithelium.

4. Bi-disperse vertex model reveals differential interfacial tension between mutant and wild-type population governs tissue-specific response towards oncogenic mutants

To explain the differential dynamics and degrees of demixing of oncogenic clusters observed in the two tissues, we drew inspiration from the differential interfacial tension hypothesis (DITH) [31]. This hypothesis suggests that cell sorting in tissues could occur due to the variations in interfacial tension, as seen in embryonic cell rearrangement, where cells regulate contractility, as well as adhesions to demix from their neighbors [31-33]. To test whether such a mechanism could be applied to the de-mixing of oncogenic clusters from wild-type cells-leading to tissue-specific outcomes, we employed the cell-based bi-disperse Vertex Model (VM). Our model allowed us to simulate an epithelial monolayer and capture the dynamic interactions between wild-type and

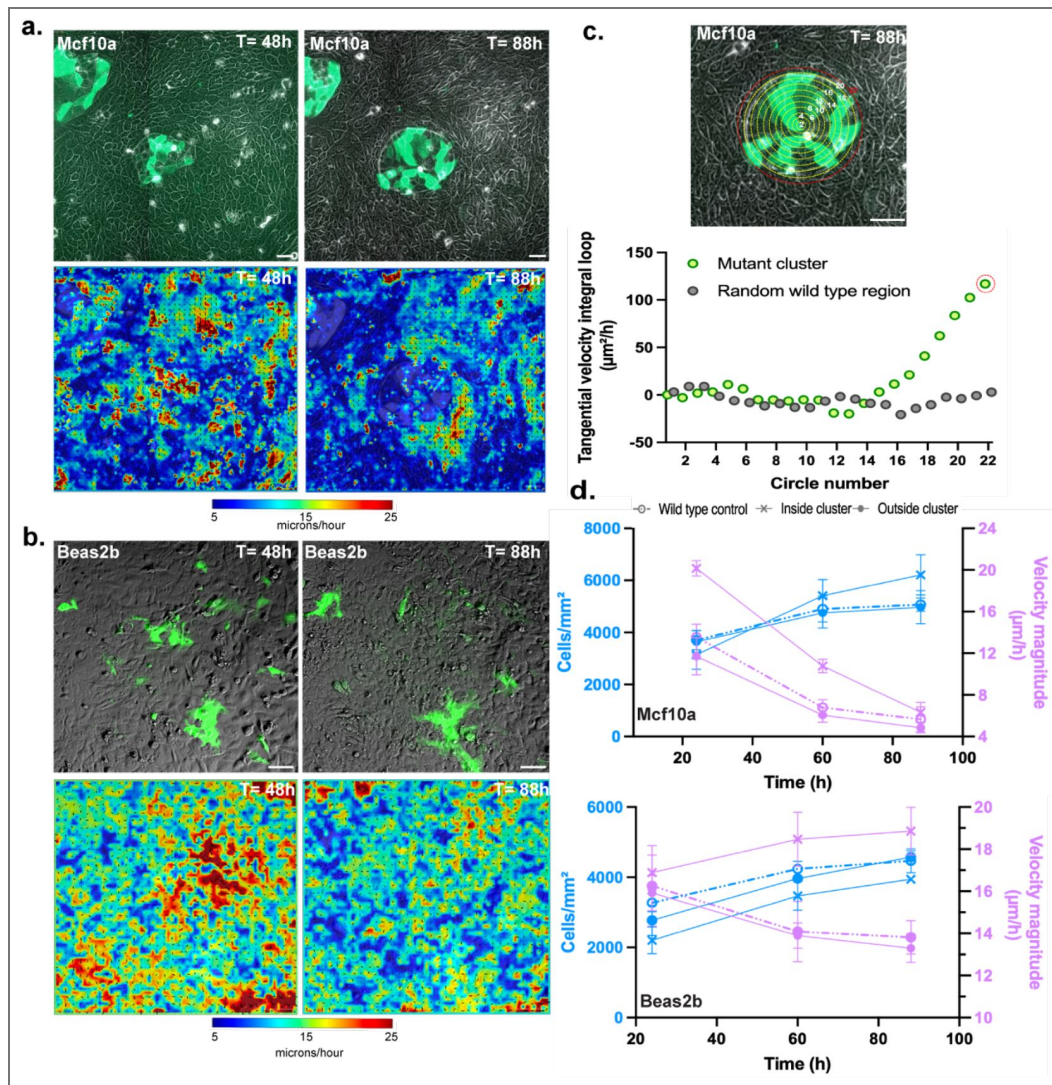


Figure 3. Particle Image Velocimetry (PIV) reveals distinct cellular movement patterns in HRas^{V12} clusters in the two monolayers

(a), (b) Representative snapshots of HRas^{V12} clusters, and the corresponding PIV maps, in mammary (a) and bronchial epithelium (b), as the density of wild type cells increase showing wild type cells along the cluster-wild-type interface exhibit a higher velocity attributed to tangential motion in mammary epithelium (a), but undergo a more kinetically arrested state in bronchial epithelium (b) (c) Oncogenic cluster in MCF10A monolayer with concentric circles drawn from the centre of the cluster, radially outward till its boundary (upper panel) with the red (highlighted) circle representing the one along which tangential velocity was the highest and plot showing tangential motion (expressed as a function of the circles), revealing highest tangential motion (data point highlighted with red) along the interface of oncogenic cluster with the wild-type cells in mammary epithelia (lower panel). No significant tangential motion in random wild-type region (c) Representative snapshots of HRas^{V12} clusters in bronchial epithelium at the same two time points and the corresponding PIV velocity maps (d) Quantification of cellular velocities in local regions as cell densities reach confluency showing oncogenic cells clustered in mammary epithelium (*top panel*) jam and show a significant reduction in velocities. In bronchial epithelium (*bottom panel*) while wild type cells show reduced movement as cell density increased, transfected cells continued to show higher motion, signifying that jamming of wild type cells has no effect on mutants. All data are represented as mean±sem plotted from different clusters from one representative experiment. Scale bars= 50 μm.

mutant cell populations. We analyzed the mechanics underlying the segregation dynamics of mutant clusters by examining the interfacial line tension $\Lambda_{ij}^{M/WT}$ between the oncogenic and wild-type cells [Figure. 4a]. In our model, $\Lambda_{ij} = 0$, for homotypic interfaces, i.e. wild-type-wild type or mutant-mutant interactions, and $\Lambda_{ij} = \Lambda \neq 0$, for heterotypic interfaces between oncogenic and wild type cells. When $\Lambda > 0$, our model ensures that the interface between oncogenic and healthy cells contracts to minimize energy, leading to a reduction in total interfacial length, and when $\Lambda < 0$, our model promotes a rough interface by favouring increased interface between healthy and oncogenic cells [Supplementary Video 7]. The final interface shape is determined by the balance between interfacial tension and the intrinsic perimeter and area elasticity of individual cells [Figure. 4b].

To explain the observed differences in interfacial cellular dynamics, we introduced an active contribution to interfacial tension, which was coupled to the shape of cells at the interface, called shape-tension coupling^[34]. This active interfacial tension is extensile, meaning it elongates cells along the interface depending on their orientation relative to the interface. It originates from the anisotropic distributions of stress-fibres in when cells are under external stress. Hence, we assume that it becomes significant only when the hydrostatic pressure on the interfacial cells exceeds a threshold value Π_0 [Figure. 4b, g].

Remarkably, our model robustly captured the experimentally observed behaviors. As a first check, we compared the experimentally observed differences in the shape indices between interfacial and non-interfacial wild-type and oncogenic cells in both mammary and bronchial epithelium with our model's predictions. For $\Gamma = 0.2$, $\Pi_0 = \{0, 0.1, 0.3\}$, $\Lambda = \{0 - 1.6\}$, our model accurately captured the experimental observations [Figure. 4c]. For stress threshold values lower than $\Pi_0 = 0.3$, we find that the differences in shape indices are non-zero even for $\Lambda = 0$, which is an unphysical situation. This is unphysical because we expect there to be no difference in the shape indices because in principle, there is only one cell type for $\Lambda = 0$. Thus, we have taken $\Pi_0 = 0.3$ for further analyses. To make the comparison between the model and the experiment more robust, we compared other metrics as well.

To quantify the extent of mixing between wild-type and mutant cells, we used the segregation index. Our simulations showed that when $\Lambda < 0$ the segregation index rapidly decreases over time, indicating outward protrusion of the mutant cluster. In contrast, for $\Lambda > 0$ the segregation index remained close to 1, reflecting a compact, jammed cluster [Figure. 4f]. Additionally, we observed that when $\Lambda > 0$, cells within the cluster experience higher internal pressure compared to when $\Lambda < 0$ [Figure 4g], consistent with experimental findings [Figure. 2h,i]. Furthermore, flow field analysis from our simulations [Figure 4h,i] revealed that for $\Lambda > 0$, cell movement aligns tangentially along the cluster boundary—consistent with the MCF10A behaviour—whereas for $\Lambda < 0$ cell motion was uniform throughout the monolayer, resembling the BEAS2B phenotype [Figure. 3a, b]. These comparisons further establish that different values of Λ correspond to different cell types. The same oncogene thus might affect different cell lines differently. We also estimated the probability of single mutant cell extrusion as a function of Λ [Figure. 4j], consistent with the findings from our experiments which show that isolated HRas^{V12} transfected cells are frequently extruded in mammary tissue [Figure. 1b]. Further, to check how actin distribution in the tissue can change in response to the interfacial tension in the model, we performed simulations of a vertex model with interfacial tension and mechanochemical feedback^[35]. The simulation snapshots matched quite well with those from experiment [Appendix figure 5]. Together, our findings demonstrate how interfacial tension-driven mechanics could play a crucial role in determining the competitive dynamics between wild-type and mutant populations, thus providing compelling evidence that cellular and tissue mechanics are key determinants of cell competition.

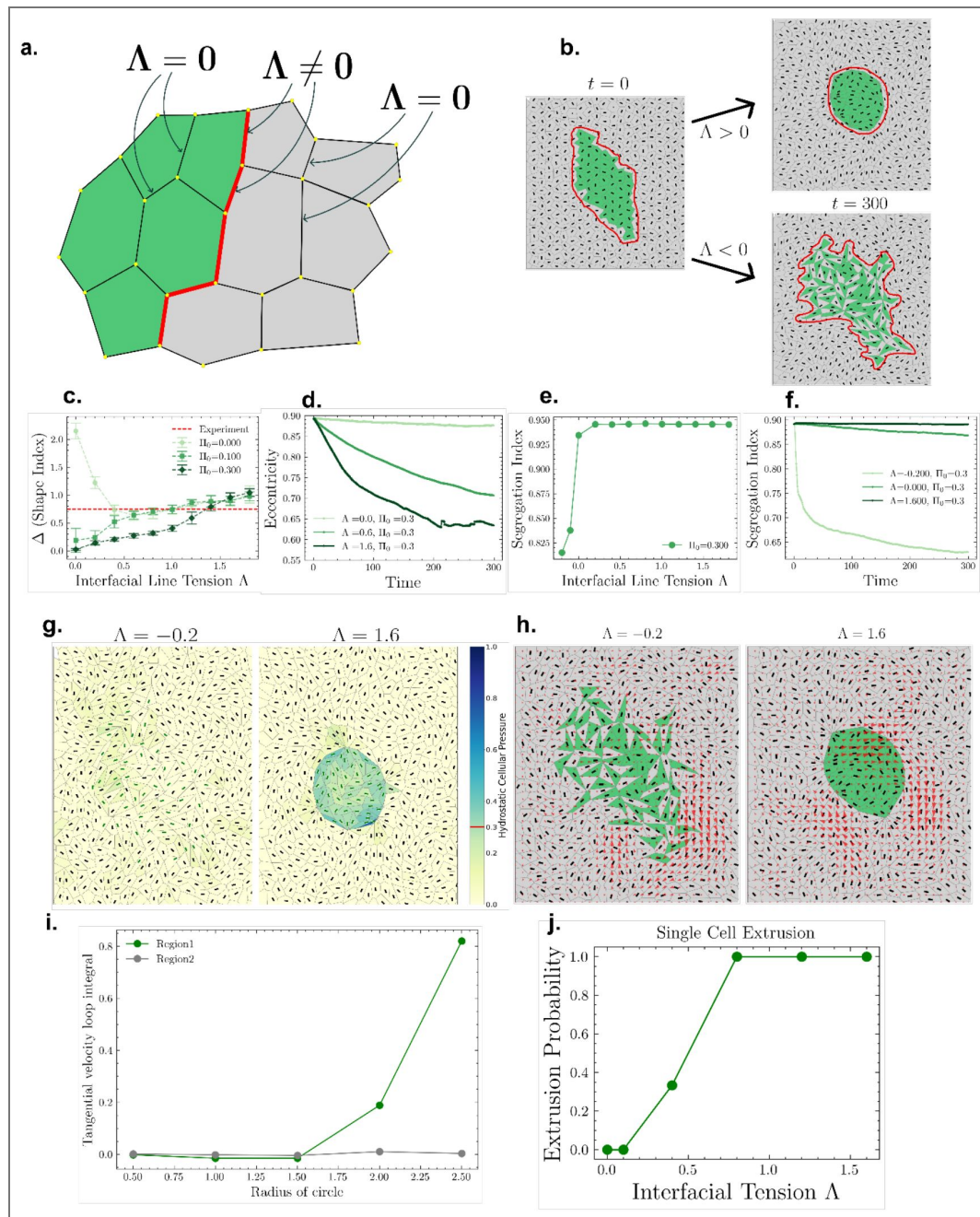


Figure 4. Bi-disperse vertex model reveals interfacial tension-driven segregation of oncogenic clusters

(a) Schematic of the bi-disperse vertex model, where interfacial line tension (red) is applied at the boundary between mutant (green) and wild-type (grey) (b) The value of Λ determines whether the mutant cluster remains compact or spreads into the wild-type population, where the red line gives the outline of the morphology of the mutant cluster interface (c) Difference in shape index between interfacial and bulk cells as a function of Λ (interfacial tension), shown for different stress thresholds. Experimental average (red) overlaid for comparison (d) Eccentricity of mutant clusters (given by the red lines in (b)) over time for different values of Λ (with $\Pi_0 = 0.3$), indicating changes in cluster morphology (e) Segregation index at $t = 300$ as a function of Λ for $\Pi_0 = 0.3$, quantifying the extent of cluster segregation (f) Time evolution of the segregation index for different values of Λ (with $\Pi_0 = 0.3$), demonstrating interfacial tension-driven segregation (g) Hydrostatic pressure maps of mutant and wild-type cells at $t = 300$, with mutant cells labeled by green directors and wild-type cells by black directors (h) Velocity field maps of epithelial monolayers for different values of Λ , revealing flow patterns around oncogenic clusters (i) Tangential velocity loop integral for circles of varying radius centered at the mutant cluster (Region 1) and centered away from the cluster (Region 2), showing tissue-specific velocity variations (j) Extrusion probability of a single mutant cell as a function of Λ , demonstrating how interfacial tension influences mutant cell fate.

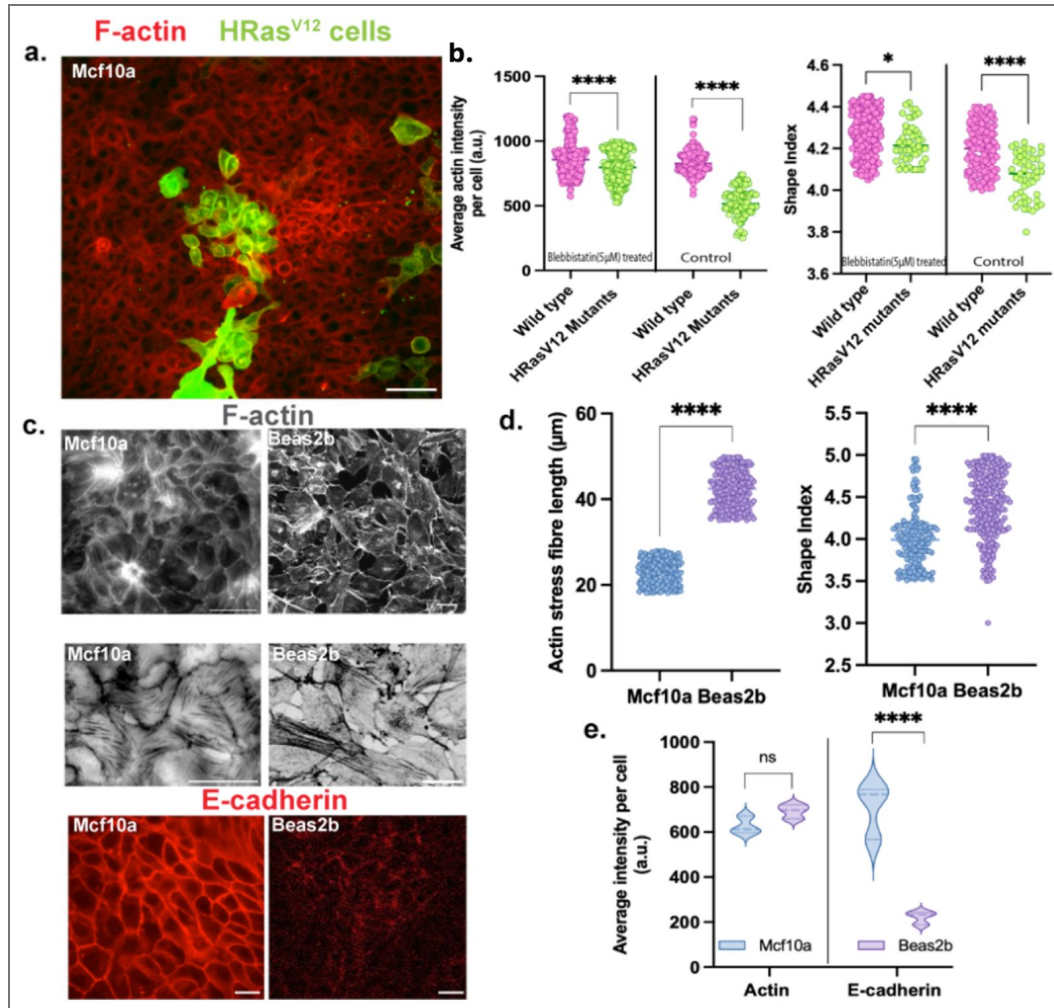


Figure 5. Actomyosin belt disruption prevents mutant cluster compaction in mammary epithelia

(a) Representative actin staining image upon blebbistatin treatment, done after oncogenic induction in mammary epithelial monolayer, showing an absence of an actin belt (b) Quantification of F-actin intensities (left) and shape indices (right), showing difference between oncogenic clusters and wild-type cells in these parameters, is getting small – although not completely vanished because of low concentration of blebbistatin used for the experiment (c) Representative actin and E-cadherin staining images of the wild type monolayers showing shorter stress fibers, higher E-cadherin intensities in MCF10A wild-type monolayer, and the opposite in BEAS2B (d) Plots comparing F-actin stress fiber length (left panel) and shape indices (right panel) in wild-type MCF10A and BEAS2B monolayers. Stress fiber lengths were calculated manually in ImageJ (e) Plots comparing F-actin and E-cadherin levels in the two wild-type tissues. Representative data are plotted from one of three independent experiments with the median shown as a bold line. Statistical significance was calculated using Unpaired t-test with Welch’s correction. Scale bars= 50 μm .

5. Disrupting actomyosin belt using blebbistatin prevents demixing and compaction of mutant clusters in mammary epithelia

Since our model showed that differences in interfacial tension regulate mutant cluster dynamics, with a higher interfacial tension driving cluster compaction [Supplementary video 7 [↗](#)], we reasoned that this tension is mediated by the supracellular actomyosin belt [36] that drives the compaction and segregation of oncogenic clusters in mammary epithelium. Therefore, we investigated whether disrupting the cytoskeletal organization and impairing actomyosin belt formation would affect the demixing and compaction of oncogenic clusters. To test this, we treated MCF10A monolayers with 5 μM blebbistatin, a myosin II inhibitor, to disrupt belt formation. As expected, blebbistatin treatment prevented mutant cluster compaction [Figure. 5a [↗](#)], leading to a loss of their rounded morphology and restoring actin levels and shape indices of mutant cells to wild-type levels [Figure. 5b [↗](#)]. This shift resulted in mutant clusters resembling those observed in bronchial epithelia, suggesting that cytoskeletal organization plays a key role in tissue-specific differences in mutant cluster dynamics. This was also consistent with the fact that interfacial tension between cells arises from the interplay between the cortical actomyosin network and cell-cell adhesion [37]. Additionally, we looked into the inherent differences in cytoskeletal mechanics of the host tissues and observed distinct differences in actin organization between the two tissues. Wild-type bronchial and mammary epithelial cells exhibited comparable F-actin intensities [Figure. 5c [↗](#) (upper panel), e], although the bronchial epithelial cells had longer stress fibers [Figure. 5c [↗](#) (middle panel), d (left panel)]. These cytoskeletal differences were also coupled with significant differences in cell shapes between confluent MCF10A and BEAS2B monolayers with wild-type BEAS2B cells exhibited significantly higher shape indices, indicating elongated, loosely packed morphologies and a lower degree of jamming [Figure 5d [↗](#) (right panel)]. In contrast, mammary epithelial cells had lower shape indices, reflecting a more compact and tightly packed arrangement [Figure. 5d [↗](#) (right panel)]. These differences were also in agreement with the PIV maps of the two wild-type tissues [Supplementary figure 2 [↗](#), Supplementary videos 4 [↗](#) and 6 [↗](#)] where the mammary monolayers underwent a sharper drop in velocities and therefore kinetic arrest, compared to the bronchial epithelia. Bronchial epithelial cells also exhibited weaker cell-cell adhesions, as indicated by reduced E-cadherin staining intensity at cell junctions compared to mammary epithelial cells [Figure. 5c [↗](#) (bottom panel), e]. These weaker adhesions likely contributed to increased cellular motility and a diminished ability to constrain mutant clusters, in contrast to the more stable, compacted clusters observed in mammary epithelium. Together, these findings demonstrate that variations in mechanical properties-including cell shape, actin organization, and adhesion strength-govern the differential responses of mammary and bronchial epithelia to oncogenic mutants and may in turn, influence tumor growth and progression.

Discussion

A central challenge in cancer biology is understanding why some oncogenic mutations are more potent in certain cancers. Large-scale cancer genomics has revealed that many driver mutations are shared across epithelial cancers, yet tumor incidence, progression rates, and invasive potential vary widely between organs [38, 39]. These observations have traditionally been explained through tissue-specific differences in signaling pathways, differentiation states, and mutational landscapes. However, such explanations are incomplete, particularly in the context of early tumorigenesis, where oncogenic mutations are often detected in histologically normal tissues without leading to overt cancer [38]. This raises a fundamental question: what prevents or permits oncogenic cells from expanding at the earliest stages of cancer initiation? The present study addresses this gap by proposing interfacial mechanics between wild-type and nascently transformed cells, as a central organizing principle in early cancer initiation. Rather than focusing oncogenic cells in isolation, our work frames tumor initiation as an emergent outcome of mutant-wild-type interactions within an epithelial collective. From this perspective, the critical determinant of oncogenic fate is not only the presence of a mutation, but how the host tissue mechanically responds to it. This

conceptual shift aligns with growing recognition that epithelial tissues behave as active materials, whose collective mechanical state can either suppress or amplify local perturbations. These insights shed light on the differential susceptibility of epithelial tissues to oncogenic transformation and uncover a mechanical basis for tissue-specific oncogenesis. By demonstrating how interfacial tension at the mutant-wild-type boundary governs whether oncogenic cells are restrained or overgrow, our work shifts the focus from purely molecular pathways to the biophysical constraints that regulate tumor initiation. While previous studies have emphasized the contextual nature of tumorigenesis [2-4] and highlighted the critical role of interactions between healthy and oncogenic cells during epithelial cancer initiation [14, 22, 40], our work integrates and extends these perspectives by demonstrating how interfacial tension at the mutant-wild-type boundary determines whether transformed cells remain constrained or undergo unchecked expansion.

To probe the mechanistic basis of these differences, we applied the Differential Interfacial Tension Hypothesis (DITH) [31,32] and demonstrated that interfacial tension is a key determinant of mutant cluster morphology and dynamics. When interfacial tension between wild-type and mutant populations was positive, mutant clusters shrunk into circular aggregates and stayed constrained. In contrast, a negative interfacial tension resulted in irregular, protrusive clusters that failed to compact and kept growing. Importantly, while the Differential Interfacial Tension Hypothesis poses that segregation results from global differences in the contractility and adhesive properties of two tissues displaying different intrinsic tensions, the results of the present work support a different scenario, where what counts is the difference in the heterotypic interfacial tension, i.e, the tension along the boundary of the wild-type and mutant populations. In line with this, we also showed that disrupting the interfacial actomyosin belt around the mutant clusters in the mammary epithelia, disrupted the restraint on them, preventing their demixing and compaction and shifting cluster behavior to a more unjammed state, similar to the ones in the bronchial system. These findings underscore the role of interfacial cellular mechanics in shaping oncogenic cell fate, with mammary epithelium imposing physical constraints that limit mutant expansion, while bronchial epithelium lacks such mechanical barriers, permitting unchecked growth.

By integrating mechanical constraints into models of cancer initiation, our study provides a framework for understanding how different epithelial tissues resist or permit tumorigenesis. However, while interfacial tension emerges as a key regulator of oncogenic segregation, the molecular pathways driving these mechanical differences remain to be elucidated. Future studies should investigate how targeting specific signaling networks or cytoskeletal components influences interfacial tension and whether modulating these factors could provide therapeutic benefits. Additionally, extending this framework to other oncogenes and tissue types could further elucidate the mechanical principles governing tumor initiation and progression.

In conclusion, this work supports a growing view of cancer initiation as a mechanically regulated, tissue-dependent process rather than a purely mutation-driven event. By positioning interfacial mechanics between oncogenic mutant cells and their wild-type counterparts, alongside genetic and biochemical factors, our findings contribute to an emerging physical understanding of cancer, in which tissue mechanics play an active role in shaping oncogenic fate. Such a framework not only helps explain tissue-specific cancer susceptibility but also suggests that reinforcing mechanical barriers within epithelia may represent an underexplored strategy for limiting early tumor progression.

Materials and methods

Cell culture

Non-transformed human mammary epithelial cell line MCF10A were maintained in complete medium composed of phenol-free Dulbecco's modified Eagle's medium (DMEM-F12, Gibco) supplemented with 5% charcoal-stripped horse serum (Gibco), 10 U ml⁻¹ penicillin and 10 µg ml⁻¹

streptomycin (Pen-Strep, Invitrogen), epidermal growth factor (20 ng/ml; PeproTech), hydrocortisone (0.5 mg/ml; Sigma-Aldrich), cholera toxin (100 ng/ml; Sigma-Aldrich), and insulin (10 µg/ml; Sigma-Aldrich) at 37°C in a humidified incubator with 5% CO₂.

Non-transformed human bronchial epithelium epithelial cell line BEAS2B were cultured in Dulbecco's modified Eagle's medium (DMEM, Gibco) supplemented with GlutaMax (Gibco) and 5% fetal bovine serum (FBS, Gibco) along with 10 U ml⁻¹ penicillin and 10 µg ml⁻¹ streptomycin (Pen-Strep, Invitrogen). Cells were maintained at 37 °C and 5% CO₂ unless mentioned otherwise.

Cell seeding

10⁵ Cells were seeded on fibronectin-coated (10 µg ml⁻¹) glass bottom dishes (35 mm Cellvis) and transfected once they reached 80% confluency (for singlets) and 60% confluency to get transfected groups.

Transfection

Cells were transiently transfected with the Hras^{V12}-GFP expressing plasmid DNA (Addgene #18780) using Lipofectamine 3000 (Invitrogen), following the manufacturer's protocol. Post-transfection, confluent monolayers were either fixed and immuno-stained or imaged directly.

Blebbistatin addition

Blebbistatin was diluted to 5 µM final solution and added 48h post-transfection. Samples were washed after 24 hours and fixed right away.

Immunofluorescence

Cells were fixed with 4% paraformaldehyde (ThermoFisher) diluted in 1X Phosphate buffered saline (PBS, Sigma-Aldrich) for 15 minutes at room temperature. After washing away the fixative with 1X PBS, cells were permeabilized with 0.3% TritonX-100 (Sigma-Aldrich) in 1X PBS. Nonspecific antibody binding was blocked by incubating the samples in blocking solution (2% Bovine Serum Albumin (BSA Sigma-Aldrich) and 2% FBS in PBS) at room temperature for 45 minutes. Further, cells were incubated with primary antibody prepared in blocking/staining solution overnight at 4°C. Post primary antibodies incubation, cells were washed thrice with 1X PBS for 5 minutes per wash and incubated with secondary antibodies conjugated to Alexa fluor 555, Alexa fluor 594 conjugated phalloidin and 4',6-diamidino-2-phenylindole (DAPI) to mark the cell nucleus, prepared in blocking/staining solution, for 2 hours at room temperature. Finally, the samples were washed four times with 1X PBS for 5 minutes per wash before proceeding to microscopy.

Microscopy

Fluorescence images were acquired using 20X objective and 63x oil-immersion objective of a Zeiss Axio Observer 7 Inverted Microscope with a scientific-grade sCMOS camera by Iberoptics. For live imaging, samples were set up on a stage-top incubator and maintained at 37°C and 5% CO₂ throughout imaging.

Image Analysis

Image analysis for this study was performed using Fiji ^[41] except bayesian force inference and particle image velocimetry (PIV) analysis, which was performed in MATLAB (MathWorks). Cellpose ^[42] was used to segment cells to get cell count, shape indices and actin intensities for each cell while Tissue Analyzer ^[43] was used to segment cells for force inference.

Quantification of cluster eccentricity and segregation index

The term 'eccentricity' expresses a size reduction in the contact with neighboring cells. It was quantified using the formula $e = \left(1 - \left(\frac{a}{b}\right)^2\right)$, (where a= the length of the major axes and b= the length of the minor axes of the clusters), with a value closer to 0 indicating a more circular shape.

Eccentricity quantifications were performed on fixed and live tissues using outlines that were manually drawn and measured using Fiji.

The segregation index SI, defined as the average ratio of homotypic and all cell neighbors as done previously [44], quantifies the demixing degree. To quantify the SI, cells of each type were manually counted, and finally, to generate the plots, the SI was averaged over all GFP-labelled cells in one frame.

Bayesian Force Inference

Bayesian force inference was done as described previously [26] to determine the relative cellular pressures and cell-cell edge or line tension.

Particle Image Velocimetry (PIV)

Particle Image Velocimetry (PIV) was done using the PIV Lab package on MATLAB [45]. FFT window deformation (direct Fourier transform correlation with multiple passes and deforming windows) algorithm was used. Velocity maps were obtained by a 3-pass interrogation window of 128×128 pixels that halved after each pass. Tangential velocities were obtained by drawing concentric circles radially outward from the center to a point at the boundary of the mutant clusters and integrated over the entire circle using a custom python code. The output is the tangential velocity as a function of the circle.

Statistical analysis

Statistical analyses were carried out in GraphPad Prism 10. Statistical significance was calculated by Unpaired t-test with Welch's correction. p-values greater than 0.05 were considered to be statistically not significant. Each plot has data pooled from multiple frames of one out of three independent experiments. Violin plots have median shown as a bold dashed line and the first and third quartiles shown as thin dashed lines. Box and whisker plots have whiskers extending from the minimum to the maximum values, showing the full range of the dataset including outliers. Scatter-bar plots were displayed as mean \pm s.e.m. No statistical methods were used to set the sample size. Quantification was done using data from at least three independent biological replicates. For analysis involving live-imaging experiments, data were collected from three independent experiments. All the experiments with representative images were repeated at least three times.

Vertex Model

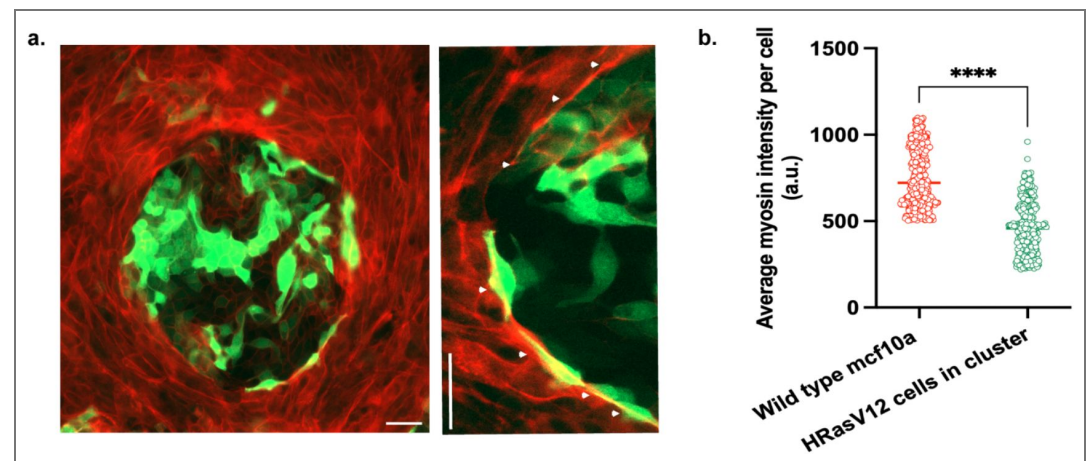
A bi-disperse model is used to demonstrate the role of interfacial tension between two types of cells, specifically the HRas^{V12} mutant and wild-type cells.

$$E_{VM} = \sum_{\alpha \in \text{WT}} \left[\frac{K_{\alpha}^{\text{WT}}}{2} (A_{\alpha} - A_{\alpha}^{0,\text{WT}})^2 + \frac{\Gamma_{\alpha}^{\text{WT}}}{2} (P_{\alpha} - P_{\alpha}^{0,\text{WT}})^2 \right] + \sum_{\alpha \in \text{M}} \left[\frac{K_{\alpha}^{\text{M}}}{2} (A_{\alpha} - A_{\alpha}^{0,\text{M}})^2 + \frac{\Gamma_{\alpha}^{\text{M}}}{2} (P_{\alpha} - P_{\alpha}^{0,\text{M}})^2 \right] + \sum_{\langle ij \rangle} \Lambda_{ij} l_{ij}$$

The first two sums are included in the standard vertex model, whereas the last term is introduced in our model to account for interfacial interactions between cells. Specifically, $\Lambda_{ij} = 0$ for interfaces between same cell types, and $\Lambda_{ij} = \Lambda$ between different cell types. Using a line tension term like Λl_{ij} in the vertex model energy, where the l_{ij} is the length of an interface edge, we can obtain both segregation and spreading dynamics just from energy minimization. This term has been described as heterotypic line tension (HLT) [46]. Due to energy minimization, heterotypic interface length is minimized for $\Lambda > 0$ and maximized for $\Lambda < 0$, leading to segregation of the two cell types in the former case and complete mixing of them in the latter case.

The mutant cluster in the experiments with MCF10A cells showed an actin belt forming along the cluster interface, with the cells along the interface being more elongated than normal. This actin ring is important for the compaction of mutant clusters in the presence of wild-type cells in the epithelial monolayer. An isotropic interfacial tension, such as the Λ_{ij} term in our model cannot capture such anisotropic behaviour. Recently, it has been proposed that such anisotropic behaviour can arise from the anisotropic distribution of the cytoskeletal filaments inside the cell^[40]. The resulting active interfacial tension, called the shape-tension coupling, can generate elongated shapes as observed in the experiments. The elongated cells in the experiments indeed have anisotropic distributions of the stress fibres. Hence, we included the effect of shape-tension in our model. The total interfacial tension is $\Lambda_{ij} + \gamma_{ij}(t; \Pi_0)$, where Λ_{ij} is a time-independent, passive, isotropic tension and γ_{ij} is a time-dependent active tension that depends on the shape of the cells sharing the interface and requires a threshold stress Π_0 to be nonzero. The details of the shape-tension coupling is described in the interface. We find that a nonzero activation stress Π_0 is necessary to reproduce experimentally observed results.

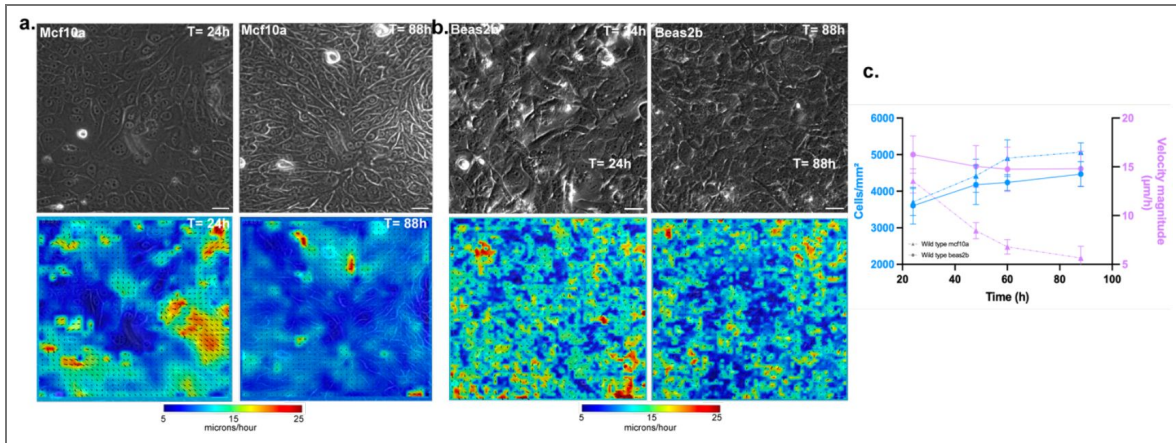
Supplementary figures



Supplementary Figure 1. Myosin belt and per cell myosin intensities (a) Images of ^{HRasV12} cluster in mammary epithelia stained for phosphomyosin (left panel) and phosphomyosin belt around the cluster marked with white arrowheads (right panel) (b) Plot showing lower phosphomyosin levels inside oncogenic clusters in MCF10A. Representative data are plotted from one of three independent experiments with the median shown as a bold line. Statistical significance was calculated using Unpaired t-test with Welch's correction. Scale bars = 50 μm .

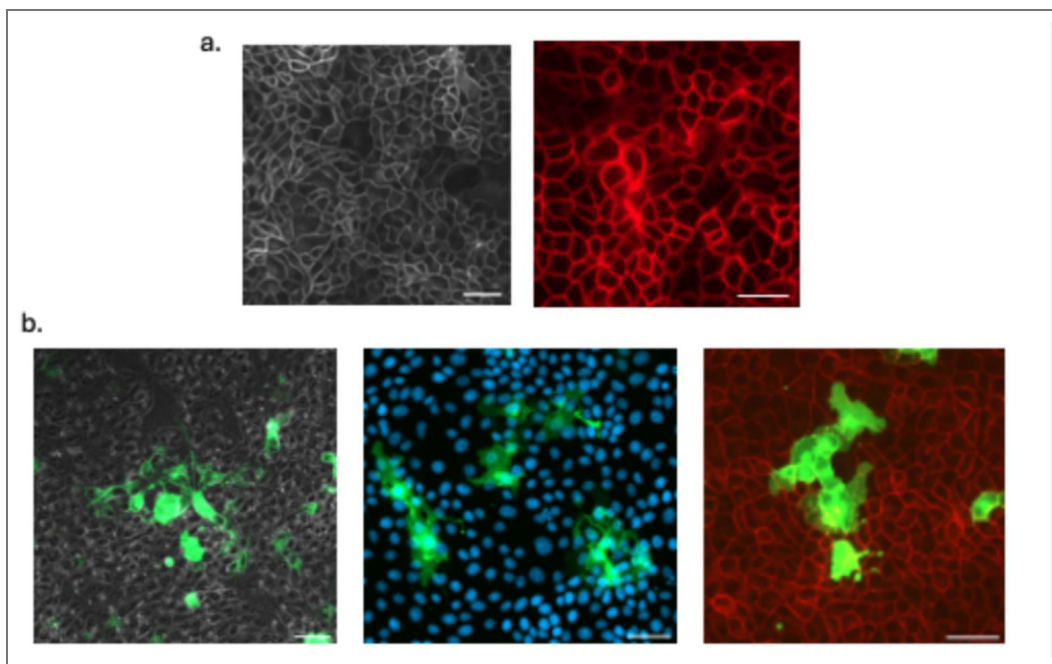
Supplementary Figure 2. PIV maps of wild-type mammary and bronchial epithelial monolayers with increasing cell density

(a) Representative time-lapse images of wild-type (control) mammary epithelium at two different time points, with corresponding PIV velocity maps showing a reduction in overall velocity as cell density increases (b) Representative time-lapse images of wild-type (control) bronchial epithelium at two different time points, with corresponding PIV velocity maps demonstrating a similar reduction in velocity with increasing cell density (c) Quantification of velocity reduction in wild-type mammary and bronchial epithelia as a function of cell density, highlighting tissue-specific differences in collective cell dynamics. All data are represented as mean±sem plotted from different clusters from one representative experiment. *Scale bars= 50 μm.*



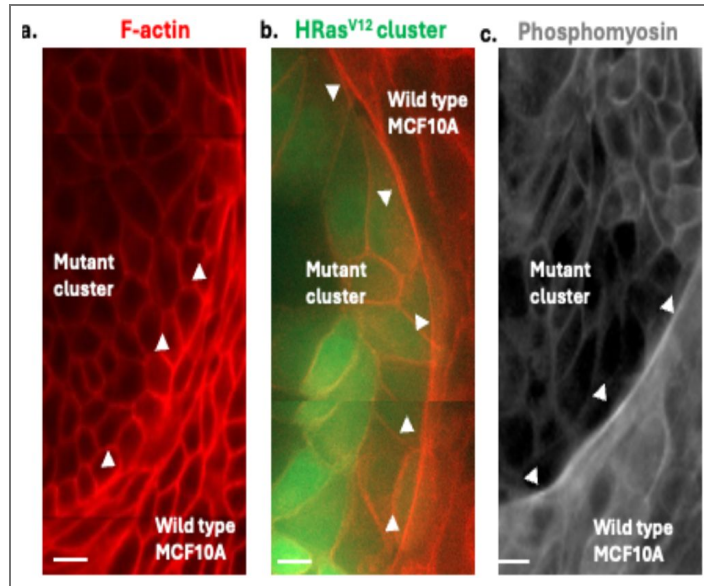
Supplementary Figure 4. HRas^{V12} clusters show invasive phenotype in MDCK monolayer

(a) Representative images of wild-type MDCK monolayers stained for F-actin (left) and E-cadherin (right), showing intact cell-cell junctions. (b) HRas^{V12} clusters expand, forming long protrusions over time. *Scale bars= 50 μm*



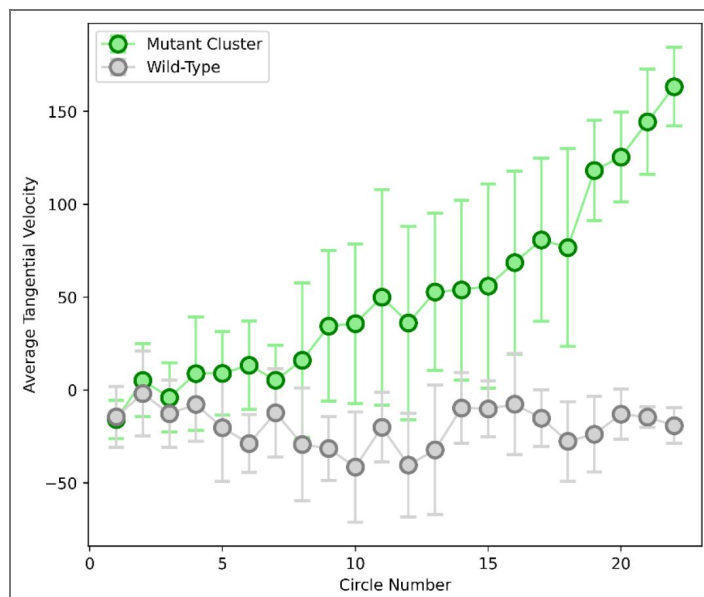
Supplementary Figure 5. Actomyosin enrichment at the interface of HRas^{V12} clusters and wild type MCF10A

(a) Images of HRas^{V12} cluster in mammary epithelia stained for F-actin, showing higher F-actin deposition at heterotypic interfaces (b) Representative image of HRas^{V12} cluster in mammary epithelia stained for Phosphomyosin, showing higher myosin deposition at the heterotypic interface. Scale bars= 10 μm.



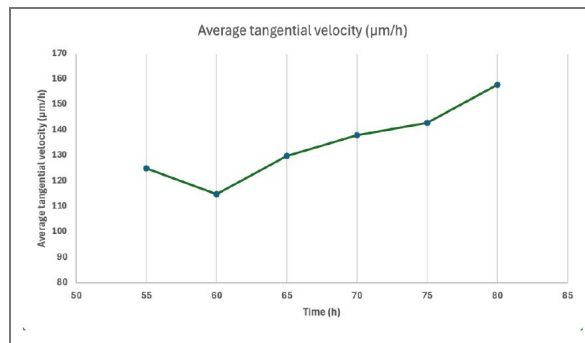
Supplementary Figure 6a. Normalized tangential velocity loop integral plotted vs.

circle number (increasing radius). The integral has been normalized by the perimeter of the circle. The same trend as in the un-normalized analysis is seen. Average has been taken over 8 different wild-type and mutant cluster positions.

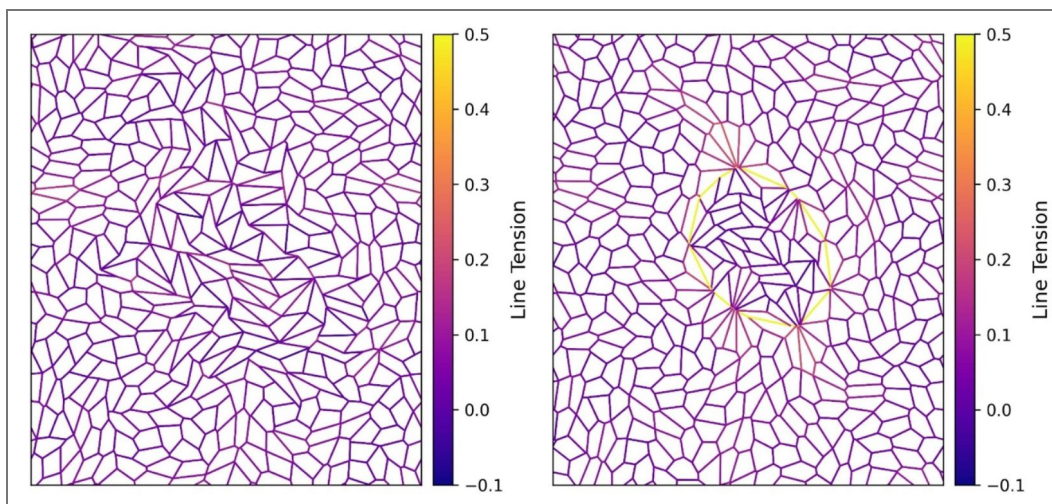


Supplementary Figure 6b. Normalized tangential velocity loop integral plotted for circle number 22 (cells at the interface of the mutant clusters) vs. time.

The integral has been normalized by the perimeter of the circle. We see tangential velocity persists for over 24 hours, till the end of the time-lapse video, starting when the mutants have formed a mature compact, rounded, well defined cluster.



Supplementary Figure 7. Line tensions from simulation for, left panel $\Lambda = -0.2$, and right panel $\Lambda = 1.6$.



Data availability

Data and codes are available upon request.

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Additional information

Author contributions

M.V conceived the project. M.V. and A.D. designed experiments. A.D performed all experiments except the staining on BEAS2B cells, which were performed by A.A. Theoretical model was contributed by P.D and S.S. Analysis and interpretation of experimental data was done by A.D, T.C, T.T, A.A, S.M, A.R and M.V. A.D and M.V developed and wrote the manuscript with help from P.D and S.S. All authors read, discussed and commented on the manuscript.

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Additional files

Supplementary video 1 [↗](#) An HRas^{V12} singlet is extruded from MCF10A monolayer but persists in BEAS2B monolayer, multiply and form long protrusion. *Scale bar= 20 μm.*

Supplementary video 2 [↗](#) A group of HRas^{V12} transfected cells gradually gets confined into a compact cluster in MCF10A monolayer and forms a smooth interface with the wild-type population, while a group of HRas^{V12} transfected cells gradually grows in size in BEAS2B monolayer, forming a jagged interface with the wild-type population along with protrusions. *Scale bar= 50 μm.*

Supplementary video 3 [↗](#) PIV video during formation of a representative HRas^{V12} cluster in MCF10A monolayer. *Scale bar= 50 μm.*

Supplementary video 4 [↗](#) PIV video showing the dynamics of a representative wild-type MCF10A (control) monolayer without any oncogenic mutants. *Scale bar= 50 μm.*

Supplementary video 5 [↗](#) PIV video showing the dynamics of a representative HRas^{V12} cluster in BEAS2B monolayer. *Scale bar= 50 μm.*

Supplementary video 6 [↗](#) PIV video showing the dynamics of a representative wild-type BEAS2B (control) monolayer without any oncogenic mutants. *Scale bar*= 50 μm .

Supplementary video 7 [↗](#) Video showing output of the bi-disperse vertex model with cluster dynamics varying with interfacial tension (Λ).

Appendix 1

Vertex Model Simulation

To understand the cause and the dynamics of interaction between mutant and wild-type population in different epithelial monolayers during cancer initiation, we used a cell-based model of epithelial tissues called the vertex model. A monolayer in the vertex model has total energy given by:

$$E_{VM} = \sum_{\alpha} \left[\frac{K_{\alpha}}{2} (A_{\alpha} - A_{\alpha}^0)^2 + \frac{\Gamma_{\alpha}}{2} (P_{\alpha} - P_{\alpha}^0)^2 \right]$$

In the above energy function, the constant parameters K_{α} is the area modulus which gives the area elasticity of each cell and Γ_{α} is the perimeter modulus which give the elasticity due to the actomyosin cortex. The gradient of this energy function gives the forces on each vertex of the cell, $\vec{F}^{(i)} = -\nabla_{\vec{r}^{(i)}} E_{VM}$, where $\vec{r}^{(i)}$ is the position of the *i*th vertex. The dynamics of each vertex position is given by the overdamped equation of motion:

$$\frac{d\vec{r}^{(i)}}{dt} = \vec{F}^{(i)} + \vec{F}_{act}^{(i)} + \vec{F}_{motility}^{(i)}$$

where $\vec{F}_{act}^{(i)}$ is any active force which might drive the system out of equilibrium. $\vec{F}_{motility}^{(i)}$ is a force which propels individual cells by $\vec{F}_{motility}^{(i)} = v_0 \vec{p}_{\alpha}$, where \vec{p}_{α} is the polarity of a given cell given by $\vec{p}_{\alpha} = (\cos \theta_{\alpha}, \sin \theta_{\alpha})$, where this angle θ_{α} performs rotational diffusion:

$$\partial_t \theta_{\alpha} = \sqrt{2D_r} \eta_{\alpha}(t)$$

where $\eta_{\alpha}(t)$ is a Gaussian white noise with zero mean and correlation $\langle \eta_{\alpha}(t) \eta_{\alpha'}(t') \rangle = \delta(t - t') \delta_{\alpha\alpha'}$.

To capture the dynamics of cell segregation between two different types of cells in a monolayer of normal and oncogenic cells, we can use a bi-disperse vertex model with an interfacial line tension between the two types of cells - called mutant and wild type can be used.

The director of each cell corresponds to the polarization direction of the cell, which can be obtained as the larger eigenvector of its shape tensor, $\underline{G}_{\alpha} = \frac{1}{N^{(\alpha)}} \sum_{i \in \nu_{\alpha}} (\vec{r}^{(i)} - \vec{r}_0^{(\alpha)}) \otimes (\vec{r}^{(i)} - \vec{r}_0^{(\alpha)})$, where the sum is over $N^{(\alpha)}$ vertices of the cell α , and $\vec{r}_0^{(\alpha)}$ is the position of the cell's geometric center. The energy function for the vertex model used is given below:

$$E_{VM} = \sum_{\alpha \in \text{WT}} \left[\frac{K_{\alpha}^{\text{WT}}}{2} (A_{\alpha} - A_{\alpha}^{0,\text{WT}})^2 + \frac{\Gamma_{\alpha}^{\text{WT}}}{2} (P_{\alpha} - P_{\alpha}^{0,\text{WT}})^2 \right] + \sum_{\alpha \in \text{M}} \left[\frac{K_{\alpha}^{\text{M}}}{2} (A_{\alpha} - A_{\alpha}^{0,\text{M}})^2 + \frac{\Gamma_{\alpha}^{\text{M}}}{2} (P_{\alpha} - P_{\alpha}^{0,\text{M}})^2 \right] + \sum_{\langle ij \rangle} \Lambda_{ij} l_{ij}$$

Here, *M* denotes mutant cells and *WT* denotes wild-type cells. The index α denotes cells, and the indices i, j denote vertices and $\langle ij \rangle$ denotes an edge between vertices i and j . The parameters $K_{\alpha}^{\text{M}}, K_{\alpha}^{\text{WT}}$ are the area moduli, $\Gamma_{\alpha}^{\text{M}}, \Gamma_{\alpha}^{\text{WT}}$ are the perimeter moduli of the mutant and wild type respectively, and the Λ_{ij} denotes the interfacial line tension. This interfacial line tension is only along junctions connecting two vertices and depends on the cell type on either side of the junction. Since the system we are considering is bi-disperse, the interfacial line tension can have three values, depending on the identities of cells on either side of a given edge $\langle ij \rangle$:

$$\Lambda_{ij} = \begin{cases} \Lambda_{ij}^{M/M} & \text{if both are mutant cells} \\ \Lambda_{ij}^{WT/WT} & \text{if both are wild-type cells} \\ \Lambda_{ij}^{WT/M} & \text{if one is wild-type and the other is mutant} \end{cases}$$

Shape-tension coupling

In addition to this passive interfacial tension, we can also have an active contribution coming from the shape tension coupling. The shape-tension coupling is mathematically the same as the passive line tension force. The total force is given by:

$$(\Lambda + \gamma_{ij}(t)) \vec{\nabla} l_{ij}$$

$\gamma_{ij}(t)$ depends on the relative orientation of the cell's director \vec{n} and the edge along which the tension acts, \vec{l}_{ij} . Specifically, it has a relaxational dynamics of the form:

$$\dot{\gamma}_{ij} = [\gamma_{ij}(t) - \gamma_{ij0}] / \tau$$

Here $\gamma_{ij0} = -\frac{1}{2} \zeta [\cos 2\theta + \cos 2\theta']$ couples the tension along an edge to the shape of the cells on either side of the edge [Appendix Fig 1].

For $\zeta > 0$, this tension is extensile and leads to the elongation of cells along the boundary. This happens because for the edges which have \vec{n} and \vec{n}' aligned with the edge vector (θ or $\theta' = 0, \pi, 2\pi$), the shape-tension coupling contributes a negative line tension, which favours this alignment. When the edge vectors are not aligned with the edge vector, the contribution is positive, and that edge starts to shrink. Eventually, the interface consists of cells whose directors are always aligned with the interface. Energetically, it counteracts interfaces with $\Lambda > 0$, leading to the formation of elongated cells and tangential flows along the interface. Importantly, we find that cell elongation correlates with the formation of actin belt, leading us to postulate that the shape-tension coupling is activated above a threshold pressure, Π_0 , where the cell pressure is given by $\Pi = -\frac{\partial E_{VM}}{\partial A}$. When $\Lambda < 0$, such as in the BEAS2B cells, we do not observe strong stress-fibre expression. Hence, we believe that it is not activated in those cells.

Simulation Setup

The vertex model energy can be non-dimensionalised by setting a length scale set by $\sqrt{A^0}$. In our simulation we have taken

$$A_\alpha^{0,WT} = A_\alpha^{0,M} = A^0 \quad \forall \alpha$$

and

$$P_\alpha^{0,WT} = P_\alpha^{0,M} = P^0 \forall \alpha$$

Also,

$$\begin{aligned} K_\alpha^{WT} &= K_\alpha^M = K \forall \alpha, \\ \Gamma_\alpha^{WT} &= \Gamma_\alpha^M = \Gamma \forall \alpha \end{aligned}$$

and

$$\Lambda_{ij}^{M/M} = \Lambda_{ij}^{WT/WT} = 0 \forall \langle ij \rangle, \Lambda_{ij}^{M/WT} = \Lambda \forall \langle ij \rangle$$

The non-dimensionalization has been done, which defines the normalized parameters $\bar{\Gamma} = \Gamma / K A^0 \bar{\Lambda} = \Lambda / K (A^0)^{3/2}$. (In further discussions, the normalized parameters will be represented by the symbols Γ and Λ .)

The monolayer modelled by the vertex model can be described by a single number, the shape index, defined by $q = P^0 / \sqrt{A^0}$. Here too, in principle we could have different shape indices for the mutant and wild type cells, but we take them to be the same. Unless otherwise mentioned, we take $\Lambda^{M/M} = \Lambda^{WT/WT} = 0$ and $\Lambda^{WT/M} = \Lambda$.

To simulate the elongation of cells along the interface, $\zeta > 0$ is used for an active extensile contribution to the interfacial tension.

A box containing 20×20 cells has been used with mutant cells placed within a region (non-circular) from the center of the box. The vertices are arranged in a hexagonal lattice with random displacements added to the position of each vertex. Periodic boundary conditions were used to simulate a confluent monolayer.

Parameters

K	1
Γ	0.1
A^0	1
P^0	4.0
l_{min} for T1 transitions	0.04
Δt for time stepping	0.01
v_0 for motility	0.05
D_r for rotational diffusion	0.5
ζ for shape-tension coupling	0.6

To prevent overlaps, a node switch operation is also added to the simulation, which changes the topology of the network [21].

Extrusion Probability Calculation

Simulations with just a single mutant cell were run for a range of differential interfacial line tension values ($\Lambda = 0, 0.1, 0.4, 0.8, 1.2, 1.6$) with shape tension coupling. The simulation was run till the area of the mutant cell fell below a threshold area = 0.1, after which we consider the mutant cell to be extruded. 9 different random initial seeds were run and analysed. Each seed gives a binary result – either extruded or not. This was used to calculate the extrusion probability.

Need for Shape-Tension Coupling – Elongation Along Interface

Shape-tension coupling has been used here in accordance with the experimental observation that the cells at the interface are aligned and elongated along the interface [Fig. 2h]. Below, difference between shape indices of cells at the interface and away from the boundary is plotted versus the interfacial tension in the case of no shape-tension coupling [Appendix Fig 2]. The red dashed line represents the experimental value of the shape index difference. The blue line is the shape index difference between two randomly chosen groups of cells (half of the total number of cells in each group is taken). At zero line-tension, the difference in shape index between interface cells and cells away from the interface is same as that between randomly chosen groups of cells, which is expected since there should be no interface at zero line-tension. The no shape-tension data presented here are averaged over 19 seeds. Although the results without shape-tension coupling reaches experimental values at high enough differential tension [Appendix Fig 2], a closer inspection of the simulation results show that the cells are just squeezed and are aligned perpendicular to the interface, which is contrary to what is seen in experiments [Fig. 2h].

Calculating the average of the absolute value of the dot product of the nematic director and the interface edge for simulations with and without shape-tension coupling [Appendix Fig 3] clearly shows that with shape-tension coupling, the cells align and elongate along the interface as is seen in experiment, given by an interface dot product value > 0.5 at high enough line-tension values. Further, shape-tension coupling or biased edge tension has been used before to model for cell elongation during embryo elongation [47] and here we use it as an active line-tension force, which elongates cells along the interface, in addition to the differential tension which is passive.

Vertex Model with Mechanochemical Feedback

Although the difference in actin between mutant and wild-type have not been incorporated in the model presented in the manuscript, we could see how the actin levels change in response to the interfacial tension formed between the mutant and wild-type cells by adding a mechanochemical feedback in the model. As given in [35], we can model the behaviour of tissues using a vertex model with mechanochemical feedback. It has been shown that incorporating these feedback loops in the vertex model captures the biologically realistic features of epithelial tissues seen in experiment [35]. In particular, to model the actin distribution in monolayers with mutants and wild-type, we can use a vertex model with interfacial tension and MCFL-I [35]. When we incorporate MCFL-I in our model, we can observe how the normalized contractility $\bar{\Gamma} = (1/K)(1/A_0)$, and normalized line tension $\bar{\Lambda} = -(\Gamma/K)(P_0/A_0^{3/2})$ changes with different line tensions. The normalized contractility is associated with the bulk actin or the bulk compressibility, and the normalized line tension is associated with the junctional actin of the cells. The equations for MCFL-I can be written as:

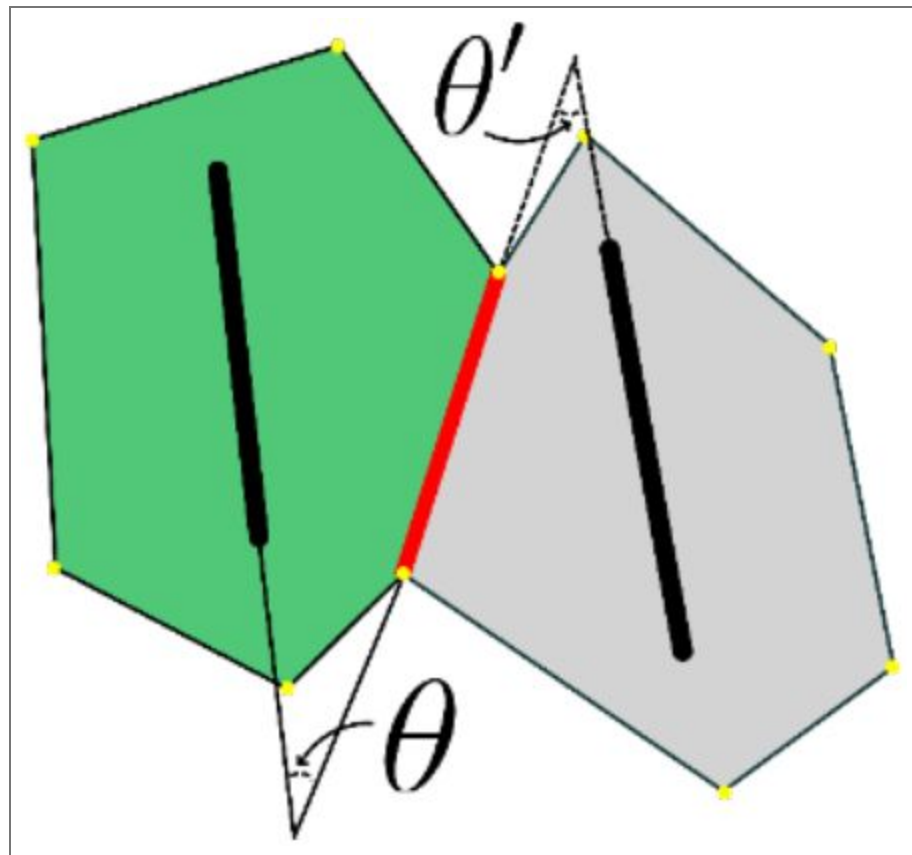
$$\begin{aligned}\tau_A \dot{A}_0 &= -[A_0 - \hat{A}_0] \\ \tau_P \dot{P}_0 &= -[P_0 - \hat{P}_0]\end{aligned}$$

Thus, with MCFLs, the vertex model does not have fixed A_0 and P_0 . The cells dynamically change these parameters depending on the vertex model dynamics. The constitutive relations for the \hat{A}_0 and \hat{P}_0 are given below [35]:

$$\begin{aligned}\hat{A}_0 &= 2a_0 p_{\text{bound}} \\ \hat{P}_0 &= 2q_0 \sqrt{a_0} (1 - p_{\text{bound}})\end{aligned}$$

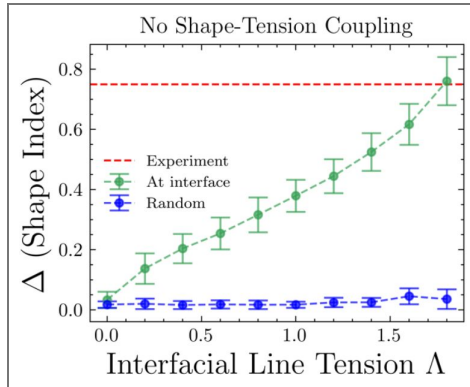
Here, $p_{\text{bound}} = 1/(1 + (A/\hat{A})^2)$, which is the probability of myosin binding and \hat{A} is a model parameter which depends on the dissociation constant of myosin [35]. We consider \hat{A} to be the same for both mutant and wild-type ($\hat{A} = 1.3$). A positive differential interfacial tension can lead to compression (decrease in area) of the mutants whereas a negative differential interfacial tension can lead to relaxation of cell area of the mutants. This will lead to different A_0 and P_0 across the monolayer, and thus different $\bar{\Gamma}$ and $\bar{\Lambda}$, which provides an understanding of the different actin levels.

For positive differential interfacial tension, the mutants are compressed which leads to decrease $\bar{\Gamma}$ and an increase in $\bar{\Lambda}$ (Figure 1 [35]). In the figures below, we plot the $\bar{\Gamma}$ as the bulk actin and the $\bar{\Lambda}$ as the junctional actin. Since our model has a differential line tension, the normalized line tension of an edge will also have a contribution from Λ , thus $\bar{\Lambda} = -(\Gamma/K)(P_0/A_0^{3/2}) + (1/K)(\Lambda/A_0^{3/2})$. The spatial distribution of actin in the mutant and wild-type seen in experiments matches well with the snapshot from simulations, where the bulk actin is low within the cluster as compared to the wild-type [Appendix Fig 4 [35]]. For negative differential interfacial tension too, we see that the actin levels are not very different between the mutant cluster and the wild-type [Appendix Fig 5 [35]].

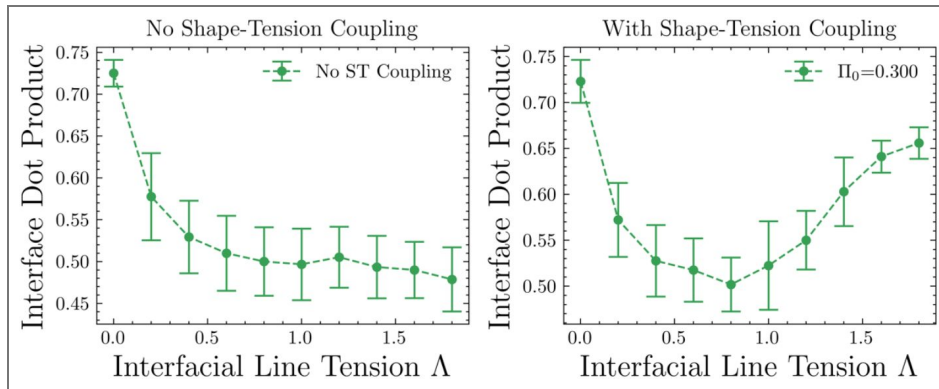


Appendix Fig 1. Illustration of shape-tension coupling at the mutant (green)-wild-type (gray) interface (red), where angles θ_1 and θ_2 represent the orientation of boundary cells relative to their shared edge

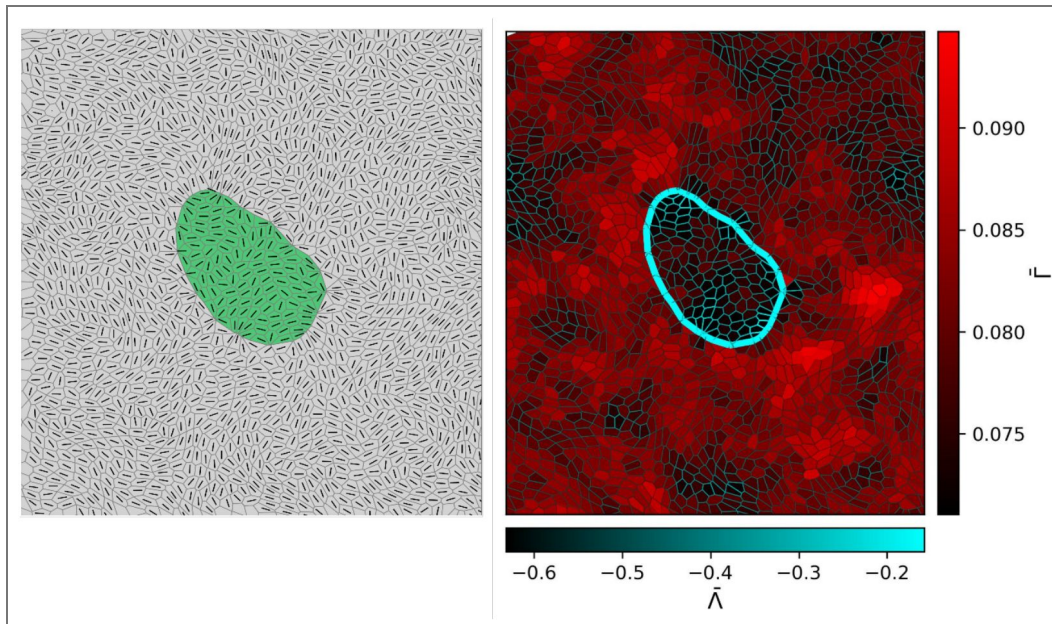
Appendix Fig 2. Shape indices versus the interfacial line tension for no shape-tension coupling.

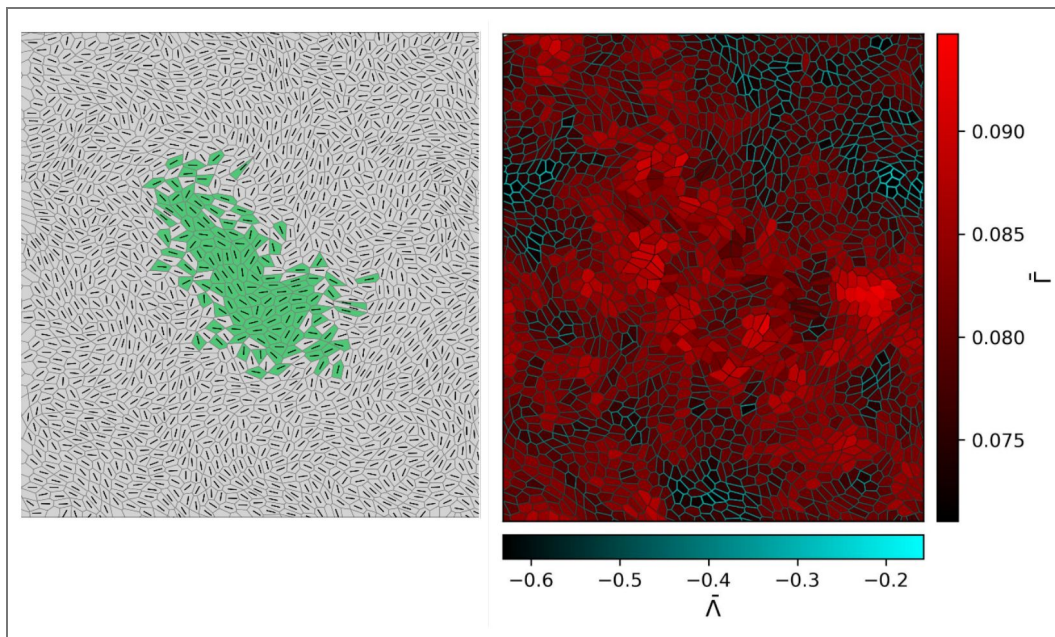


Appendix Fig 3. Interface dot product for different interfacial line tension with and without shape-tension coupling.



Appendix Fig 4. For positive differential interfacial tension ($\Lambda > 0$), the mutant cluster has lower bulk actin level compared to the wild-type cells surrounding it.





Appendix Fig 5. For negative differential interfacial tension ($\Lambda < 0$), the mutant cluster does not have a very different actin level compared to the wild-type cells surrounding it.

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Peer reviews

Reviewer #1 (Public review):

Summary:

The behaviour of cells expressing constitutively active HRas is examined in mosaic monolayers, both in MCF10a breast epithelial and Beas2b bronchial epithelial cell lines, mimicking the potential initial phase of development of carcinoma. Single HRas-positive cells are excluded from MCF10a but not Beas2b monolayers. Most interestingly, however, when in groups, these cells are not excluded, but rather sharply segregated within a MCF10a monolayer. In contrast, they freely mix with wt Beas2b cells. Biophysical analysis identifies high tension at heterotypic interfaces between HRas and wild-type cells as the likely reason for segregation of MCF10a cells. The hypothesis is supported experimentally, as myosin inhibition abolishes segregation. The probable reason for lack of segregation in the bronchial epithelium is to be found in the different intrinsic properties of these cells, which form a looser tissue with lower basal actomyosin activity. The behaviour of single cells and groups is recapitulated in a vortex model based on the principle of differential interfacial tension, under the condition of high heterotypic interfacial tension.

Strengths:

Despite being long recognized as a crucial event during cancer development, segregation of oncogenic cells has been a largely understudied question. This nice work addresses the mechanics of this phenomenon through a straightforward experimental design, applying the biophysical analytical approaches established in the field of morphogenesis. Comparison between two cell types provides some preliminary clues on the diversity of effects in various cancers.

Weaknesses:

Although not calling into question the main message of this study, there are a few issues that one may want to address:

(1) One may be careful in interpreting the comparison between MCF10a and Beas2b cells as used in this study. The conditions may not necessarily be representative of the actual properties of breast and bronchial epithelia. How much of the epithelial organization is reconstituted under these experimental conditions remains to be established. This is particularly obvious for bronchial cells, which would need quite specific culture conditions to build a proper bronchial layer. In this study, they seemed to be on the verge of a mesenchymal phenotype (large gaps, huge protrusions, cells growing on top of each other, as mentioned in the manuscript).

As an alternative to Beas2b, comparison of MCF10a with another cell line capable of more robust *in vitro* epithelial organization, but ideally with different adhesive and/or tensile properties, would be highly interesting, as it may narrow down the parameters involved in segregation of oncogenic cells.

(2) While the seminal description of tissue properties based on interfacial tensions (Brodland 2002) is clearly key to interpreting these data, the actual "Differential Interfacial Tension Hypothesis" poses that segregation results from global differences, i.e., juxtaposition of two tissues displaying different intrinsic tensions. On the contrary, the results of the present work support a different scenario, where what counts is the actual difference in tension ALONG the tissue boundary, in other words, that segregation is driven by high HETEROTYPIC interfacial tension. This is an important distinction that should be clarified.

(3) Related: The fact that actomyosin accumulates at the heterotypic interface is key here. It would be quite informative to better document the pattern of this accumulation, which is not clear enough from the images of the current manuscript: Are we talking about the actual interface between mutant and wt cells (membrane/cortex of heterotypic contacts)? Or is it more globally overactivated in the whole cell layer along the border? Some better images and some quantification would help.

(4) In the case of Beas2b cells, mutant cells show higher actin than wt cells, while actin is, on the contrary, lower in mutant MCF10a cells (Figure 2b). Has this been taken into account in the model? It may be in line with the idea that HRas may have a different action on the two cell types, a possibility that would certainly be worth considering and discussing.

Comments on revisions:

There is still one last point that should be made even clearer:

The system is being modelled based on the principle of INTERFACIAL TENSION, a description pioneered by the works of Steinberg and of Harris, and nicely conceptualized by Brodland (2002). Now the observed behaviour is a perfect case of sorting based on higher interfacial tension AT the boundary between cell types (with nice additional documentation of local actin and myosin enrichment in the revised manuscript). What needs to be made crystal clear is that this is NOT equivalent to the model of DITH ("DIFFERENTIAL INTERFACIAL TENSION HYPOTHESIS") (Brodland 2002, Krieg et al 2008). It is important to stop using DITH in this context, as it leads to confusion and misinterpretations. Indeed, DITH predicts cell/tissue sorting based on differences in interfacial tension WITHIN the two cell types. While DITH accounts for relative POSITIONING (one tissue engulfing the other), it is now established that this is not the motor for cell sorting and tissue segregation, the key parameter is being heterotypic tension at the heterotypic interface. I thus invite the authors to avoid the terms "differential"/DITH, and rather use either "interfacial tension", or specifically to "HIGH HETEROTYPIC INTERFACIAL TENSION".

Related: the authors correctly cite Canty et al NatComm2017 when discussing this phenomenon. I suggest to add an additional key supporting reference "D.M. Sussman, J.M. Schwarz, M.C. Marchetti, M.L. Manning, Soft yet sharp interfaces in a vertex model of confluent tissue, Phys. Rev. Letters 120 (2018) 058001". One may also include another pioneer work in Drosophila is "M. Aliee, J.C. Roper, K.P. Landsberg, C. Pentzold, T.J. Widmann, F. Julicher, C. Dahmann, Physical mechanisms shaping the Drosophila dorsoventral compartment boundary, Curr. Biol. 22 (2012) 967-976."

<https://doi.org/10.7554/eLife.106893.2.sa2>

Reviewer #2 (Public review):

Summary:

The authors investigate the behavior of oncogenic cells in mammary and bronchial epithelia. They observe that individual oncogenic cells are preferentially excluded from the mammary epithelium, but they remain integrated in the bronchial epithelium. They also observe that clusters of oncogenic cells form a compact cluster in mammary epithelium, but they disperse in the bronchial epithelium. The authors demonstrate experimentally and in the vertex model simulations that the difference in observed behavior is due to the differential tension between the mutant and wild-type cells due to a differential expression of actin and myosin.

Strengths:

- * Very detailed analysis of experiments to systematically characterize and quantify differences between mammary and bronchial epithelia

- * Detailed comparison between the experiments and vertex model simulations to identify the differential cell line tension between the oncogenic and wild-type cells as one of the key parameters that are responsible for the different behavior of oncogenic cells in mammary and bronchial epithelia

Weaknesses:

- * It is unclear what is the mechanistic origin of the shape-tension coupling, which is used in the vertex model, and how important that coupling is for the presented results. Authors claim that the shape-tension coupling is due to the anisotropic distribution of stress fibers when cells are under external stress. It is unclear why the stress fibers should affect an effective line tension on the cell boundaries and why the stress fibers should be sensitive to the magnitude of the internal isotropic cell pressure. In experiments, it makes sense that stress fibers form when cells are stretched. Similar stress fibers form when cytoskeleton or polymer networks are stretched. It is unclear why the stress fibers should be sensitive to the magnitude of internal isotropic cell pressure. If all the surrounding cells have the same internal pressure, then the cell would not be significantly deformed due to that pressure and stress fibers would not form. Authors should better justify the use of the shape-tension coupling in the model, since most of the observed behavior is already captured by the differential tension even if there is no shape-tension coupling.

- * The observed difference of shape indices between the interfacial and bulk cells in simulations in the absence of differential line tension is concerning. This suggests that either there are not enough statistics from the simulations or that something is wrong with the simulations. For all presented simulation results, the authors should repeat multiple simulations and then present both averages and standard deviations. This way it would be easier to determine whether the observed differences in simulations are statistically significant.

<https://doi.org/10.7554/eLife.106893.2.sa1>

Author response:

The following is the authors' response to the original reviews

Public Reviews:

Reviewer #1 (Public review):

(1) One may be careful in interpreting the comparison between MCF10a and Beas2b cells as used in this study. The conditions may not necessarily be representative of the actual properties of breast and bronchial epithelia. How much of the epithelial organization is reconstituted under these experimental conditions remains to be established. This is particularly obvious for bronchial cells, which would need quite specific culture conditions to build a proper bronchial layer. In this study, they seemed to be on the verge of a mesenchymal phenotype (large gaps, huge protrusions, cells growing on top of each other, as mentioned in the manuscript).

We thank the reviewer for this important point. We agree that our experimental conditions do not fully recapitulate the *in vivo* architecture of either breast or bronchial epithelia. As the reviewer points out, the two cell lines need typical culture conditions to grow in an *in-vivo* like architecture, such as acinar structures for mammary tissue, and a pseudostratified architecture for the bronchial tissue, and it certainly would be interesting to subject the cell lines in these organotypic architectures and study the fate of oncogenic mutant cells. However, this would be an independent study on its own and is out of the scope of the current manuscript. Here, we intend to compare these two well-established epithelial lines from mammary and bronchial epithelial tissues, with distinct intrinsic mechanical and organisational properties, in minimal culture conditions, and study how just the context of having two different sources of epithelial cells can change the fate of oncogenic cells present in the wild-type population. We have now also performed experiments with the MDCK cell line, which is not like the BEAS2B line, and has well-defined cell-cell adhesions [Supplementary figure. 4a], and epithelial morphology, and shown that the fate of HRasV¹² mutants is different here as well, as compared to the MCF10A cell line.

(2) As an alternative to Beas2b, comparison of MCF10a with another cell line capable of more robust in vitro epithelial organization, but ideally with different adhesive and/or tensile properties, would be highly interesting, as it may narrow down the parameters involved in the segregation of oncogenic cells.

We agree with the reviewer and in line with this suggestion, we have repeated the key experiments using Madin-Darby Canine Kidney (MDCK) cells, a well-established model epithelial cell line. Our results show that even though MDCK cells show significantly distinct properties compared to BEAS2B cells (MDCK being more epithelial like than BEAS2B), the dynamics of the HRasV¹² clusters in both these systems are similar [Supplementary figure. 4b], and distinctly different from the mammary epithelial cells (MCF10A). We did not observe the formation of an actin belt around HRasV¹² clusters in MDCK monolayers, which indeed forms in MCF10A monolayers. Additionally, in MDCK cells, the HRasV¹² mutant clusters are not under compaction or jamming, instead, they form protrusions similar to the ones seen in BEAS2B monolayers. These results solidify our hypothesis of tissue-specific differences in the mechanics of cancer initiation.

(3) While the seminal description of tissue properties based on interfacial tensions (Brodland 2002) is clearly key to interpreting these data, the actual "Differential Interfacial Tension Hypothesis" poses that segregation results from global differences, i.e., juxtaposition of two tissues displaying different intrinsic tensions. On the contrary,

the results of the present work support a different scenario, where what counts is the actual difference in tension ALONG the tissue boundary, in other words, that segregation is driven by high HETEROTYPIC interfacial tension. This is an important distinction that should be clarified.

We thank the reviewer for this insightful comment. As correctly noted, Brodland's 2002 work provided a foundational formulation of the Differential Interfacial Tension Hypothesis (DITH), which frames tissue organization in terms of effective interfacial tensions.

While in its original form, DITH emphasised segregation as a consequence of global differences in the intrinsic (bulk) tensions of juxtaposed tissues, our results specifically show that segregation is determined by local interfacial mechanics between transformed- and host cells. These local interfacial dynamics, however, is related to global contractility of cells- From our experiments with blebbistatin, we have observed a loss in the efficiency of segregation upon reducing global contractility, consequently inhibiting the formation of the interfacial actomyosin belt, which serves as the source of the interfacial tension between healthy and mutant populations. Therefore, the differences in local interfacial mechanics stem from intrinsic global contractility of cells in discussion here.

We have also clarified this distinction more clearly in the discussion and have explicitly stated that while DITH provided the foundation for conceptualizing tissue mechanics, our findings on transformed cell- healthy cell interactions specifically demonstrate that a higher efficiency of segregation is driven by high heterotypic interfacial tension at the tissue boundary.

(4) Related: The fact that actomyosin accumulates at the heterotypic interface is key here. It would be quite informative to better document the pattern of this accumulation, which is not clear enough from the images of the current manuscript: Are we talking about the actual interface between mutant and wt cells (membrane/cortex of heterotypic contacts)? Or is it more globally overactivated in the whole cell layer along the border? Some better images and some quantification would help.

We agree that a detailed visualisation of actomyosin distribution would strengthen our conclusions. We have now added a few more images of the interface to the Supplementary Data [Supplementary figure. 5], which show that cortical actin accumulates in individual cells, at the wild type cell-mutant cell interface, and actin levels go up in both wild type and mutant populations at the interface. This is also clear from the quantifications of different region of interests [Figure 2e], which is done by segmenting individual cells in these regions and quantifying actin intensity in each cell.

(5) In the case of Beas2b cells, mutant cells show higher actin than wt cells, while actin is, on the contrary, lower in mutant MCF10a cells (Author response image 2). Has this been taken into account in the model? It may be in line with the idea that HRas may have a different action on the two cell types, a possibility that would certainly be worth considering and discussing.

We thank the reviewer for raising this important point. While a direct experimental dissection of how HRasV¹² mutation affects actin levels in BEAS2B and MCF10A cells individually is beyond the scope of the present study, we do not rule out the possibility that a HRasV¹² mutation may exert cell-type-specific biochemical effects on actin regulation in these two epithelial systems.

Although the difference in actin between the mutants and the wild-type cells has not been incorporated into the model presented in the manuscript, we have now shown how actin levels change in response to the interfacial tension formed between the mutant and wildtype cells by adding a mechanochemical feedback to the model. Rather than prescribing intrinsic

differences in actin levels between mutant and wild-type cells, we asked whether the feedback between the actin cytoskeleton and mechanical stress alone is sufficient to generate the observed actin reorganization. To address this, we incorporate a mechanochemical feedback loop (MCFL-I), originally developed in our earlier work [35], into the vertex model framework. This feedback captures the experimentally observed coupling between cell shape, actomyosin organization, and mechanical stress (i.e., heterotypic interfacial tension), and has previously been shown to reproduce biologically realistic epithelial behaviours such as dynamic cell shapes and heterogeneous actomyosin distributions [35].

In this framework, actin is not introduced as an explicit or intrinsic variable. Instead, changes in actomyosin organization emerge dynamically in response to mechanical stresses. Specifically, MCFL-I allows the preferred area and preferred perimeter of cells to evolve depending on cell shape and actomyosin binding, rather than remaining fixed. From these evolving parameters, we compute the normalized contractility, $\bar{\Gamma} = (1/K) (1/A_0)$, which we interpret as a proxy for bulk actin, and normalized line tension $\bar{\Gamma} = (1/K) (1/A_0)$ which we interpret as a proxy for junctional actin. These normalized quantities provide size-independent measures of actomyosin organization across the tissue.

The equations for MCFL-I can be written as:

$$\begin{aligned}\tau_A \dot{A}_0 &= - [A_0 - \hat{A}_0] \\ \tau_p \dot{P}_0 &= - [P_0 - \hat{P}_0]\end{aligned}$$

Thus, with MCFLs, the vertex model does not have fixed A_0 and P_0 . The cells dynamically change these parameters depending on the vertex model dynamics. The constitutive relations for the \hat{A}_0 and \hat{A}_0 are given below [1]:

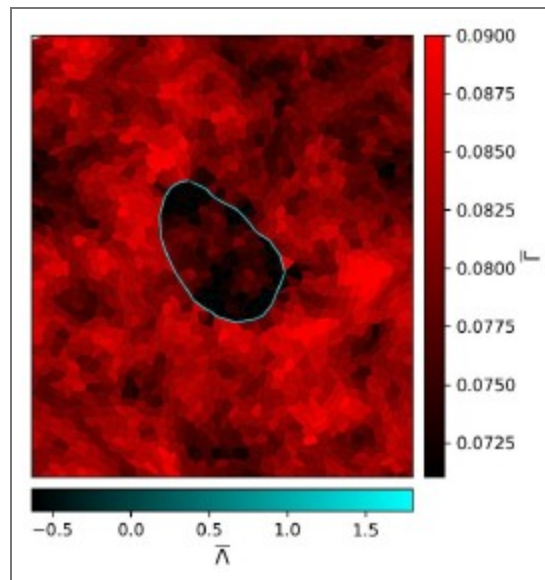
$$\begin{aligned}\hat{A}_0 &= 2a_0 p_{\text{bound}} \\ \hat{P}_0 &= 2q_0 \sqrt{a_0} (1 - p_{\text{bound}})\end{aligned}$$

Here, $p_{\text{bound}} = 1 / (1 + (A/\hat{A})^2)$ is the fraction of myosin bound to actin as a function of cell area A . This nonlinear dependence arises from the load or strain-dependent binding of myosin to actin, and $p_{\text{bound}} = 1 / (1 + (A/\hat{A})^2)$ is a model parameter which is proportional to the binding affinity of myosin to actin in the absence of any strain. We consider $p_{\text{bound}} = 1 / (1 + (A/\hat{A})^2)$ to be the same for both mutant and wild-type across the monolayer via MCFL-I, and thus reduced bulk actin and increased junctional actin [Appendix figure. 4], consistent with experimental observations. Conversely, when differential interfacial tension is weak or negative, mutant and wild-type cells experience similar stresses, and the model predicts minimal differences in actin organization [Appendix figure. 5]. $p_{\text{bound}} = 1 / (1 + (A/\hat{A})^2)$. Importantly, both mutant and wild-type cells obey identical mechanochemical rules in the model. Differences in actin organization arise solely due to differences in mechanical stress generated by differential interfacial tension. Positive differential interfacial tension compresses mutant cells within clusters. This will lead to different $p_{\text{bound}} = 1 / (1 + (A/\hat{A})^2)$ and P

Thus, while HRasV¹²-dependent biochemical effects may indeed differ between BEAS2B and MCF10A cells, our results demonstrate that mechanical interactions at mutant– wild-type interfaces are sufficient to generate distinct actin signatures in the two tissues, without invoking cell-type-specific actin regulation. We have added the details of the mechanochemical feedback loop in the model to the Appendix to emphasize that the model tests the sufficiency of mechanics-driven actin reorganization rather than excluding additional biochemical contributions.

Although it looks that even for $\Lambda > 0$ we see that the normalized line tension $\bar{\Lambda}$ seems to be negative. This is however just an artefact of the colorbar limits we have used to compare with

the $\Lambda < 0$ case. If we plot with different colorbar limits, we see that the interface has $\bar{\Lambda}$ as shown in Author response image 1.



Author response image 1.

Reviewer #2 (Public review):

(1) It is unclear what the mechanistic origin of the shape-tension coupling is, which is used in the vertex model, and how important that coupling is for the presented results. The authors claim that the shape-tension coupling is due to the anisotropic distribution of stress fibers when cells are under external stress. It is unclear why the stress fibers should affect an effective line tension on the cell boundaries and why the stress fibers should be sensitive to the magnitude of the internal isotropic cell pressure. In experiments, it makes sense that stress fibers form when cells are stretched. Similar stress fibers form when the cytoskeleton or polymer networks are stretched. It is unclear why the stress fibers should be sensitive to the magnitude of internal isotropic cell pressure. If all the surrounding cells have the same internal pressure, then the cell would not be significantly deformed due to that pressure, and stress fibers would not form. The authors should better justify the use of the shape-tension coupling in the model and also present simulation results without that coupling. I expect that most of the observed behavior is already captured by the differential tension, even if there is no shape-tension coupling.

The reviewer is correct in stating that most of the observed behaviour is already captured by the differential tension, without the shape-tension coupling. However, the shape tension coupling has been used here in accordance with the experimental observation that the cells at the interface are aligned and elongated along the interface [Fig. 2h], which can not be captured without the shape-tension coupling. The difference between shape indices of cells at the interface and away from the boundary is plotted versus the interfacial tension in the case of no shape-tension coupling [Appendix figure 2]. The red dashed line represents the experimental value of the shape index difference. The blue line is the shape index difference between two randomly chosen groups of cells (half of the total number of cells in each group is taken). At zero line-tension, the difference in shape index between interface cells and cells away from the interface is same as that between randomly chosen groups of cells, which is expected since there should be no interface at zero line-tension. The no shape-tension data presented here are averaged over 19 seeds. Although the results without shape-tension

coupling reaches experimental values at high enough differential tension [Appendix figure 3], a closer inspection of the simulation results show that the cells are just squeezed and are aligned perpendicular to the interface, which is contrary to what is seen in experiments [Fig. 2h].

Calculating the average of the absolute value of the dot product of the nematic director and the interface edge for simulations with and without shape-tension coupling [Appendix figure 3] clearly shows that with shape-tension coupling, the cells align and elongate along the interface as is seen in experiment, given by an interface dot product value > 0.5 at high enough line-tension values. Further, shape-tension coupling or biased edge tension has been used before to model for cell elongation during embryo elongation [45] and here we use it as an active line-tension force, which elongates cells along the interface, in addition to the differential tension which is passive. This additional quantification of the alignment and elongation of cells along the interface will be added to the Appendix.

(2) The observed difference of shape indices between the interfacial and bulk cells in simulations in the absence of differential line tension is concerning. This suggests that either there are not enough statistics from the simulations or that something is wrong with the simulations. For all presented simulation results, the authors should repeat multiple simulations and then present both averages and standard deviations. This way, it would be easier to determine whether the observed differences in simulations are statistically significant.

The difference in shape indices between the interfacial and bulk cells in simulations has now been calculated over 11 different seed values. The observed differences in simulations, along with the standard deviations have been plotted in Figure 4b. This figure will be updated to include the standard deviations. The nonzero difference in shape index in the absence of differential line tension for low values of stress threshold is due to the shape-tension coupling acting even at low differential tension. Thus, a non-zero, sufficiently high value of the stress threshold is required in our model with shape-tension coupling. This has also been stated in section 4 of the paper. The importance of the shape-tension coupling has been stated in response to the previous point.

(3) The authors should also analyze the cell line tension data in simulations and make a comparison with experiments.

The line tension for each edge can be calculated as $\sum_{\text{cells } \alpha \in \text{edge}} \Gamma (P_{\alpha} - P_0) + \Lambda l_{\text{edge}}$.

Although the line tension distributions look similar to the ones obtained from Bayesian Force Inference, a better comparison is between the normalized line tension and actin seen in experiment as we have discussed under point (4) asked by Reviewer 1.

Recommendations for the authors:

Reviewer #2 (Recommendations for the authors):

(1) The authors claim that the negative tension $\Lambda < 0$ resembles the Beas2b phenotype. This is not consistent with the expression of actin in Figure 2f, which seems very similar in all four regions of interest (ROIs). Also, the segregation index data for Beas2b in Figure 1h looks very different from the demixing parameter in Figure 4f for the negative value of Λ .

In the model presented in the previous version of the manuscript, actin differences have not been incorporated. We have only added an interfacial line tension, which might arise only at the interface between cells. In response to comment (4) from Reviewer 1, we have considered a vertex model with mechanochemical feedback and interfacial line tension to understand

how actin distribution in the tissue is affected by interfacial tension. The results presented match very well with experimental images.

The reviewer has rightly pointed out that the segregation index (SI) data presented in Fig. 1h have a different trend compared to those in Fig. 4f. However, it is essential to note that in the simulation, the initial condition is one in which the mutant cluster is already fully segregated, and thus, at the initial time point. This is not the case in experiments, and at initial time points. Thus, the two plots are not directly comparable and only show how SI changes in our simulations. It is more effective to compare the final time points in Fig. 2f with those in Fig. 4e, where we observe that Mcf10a has a higher SI compared to Beas2b, and the case with $\Lambda > 0$ has a higher SI than the case with $\Lambda < 0$. This supports our claim that $\Lambda < 0$ resembles the Beas2b phenotype and $\Lambda > 0$ resembles the Mcf10a phenotype.

(2) It is unclear how the threshold pressure $P_{i,0}$ is implemented for the shape-tension coupling in the vertex model. Is the value of the additional tension γ_{ij} equal to 0 if the internal pressure is below that threshold?

The stress threshold is implemented for the shape-tension in the vertex model in the following way. The line tension forces can be written as:

$$\vec{F} = \vec{F}_{\text{passive}} + \vec{F}_{\text{shape-tension}}$$

where, $\vec{F}_{\text{passive}} = \Lambda \nabla l_{ij}$ and $\vec{F}_{\text{passive}} = \Lambda \nabla l_{ij}$. If the stress on the cell is below the threshold, $\vec{F}_{\text{passive}} = \Lambda \nabla l_{ij}$ then $\vec{F}_{\text{passive}} = \Lambda \nabla l_{ij}$ for those cells.

(3) In vertex model simulations, the authors use identical parameters for wild-type and mutant cells. This does not seem to be consistent with experimental observations in Figure 2, where the expression of actin is different, and also, cell shape indices are different for the wild-type and mutant cells. The authors should comment on how that choice affects their simulation results.

We thank the reviewer for this comment. As noted in our response to comment 4 from reviewer 1, we have now attempted our simulations after adding a mechanochemical feedback to the model. Here, both wild-type and mutant cells follow identical mechanochemical rules within the vertex model. This choice does not imply that the cells are mechanically identical in the tissue; rather, it allows us to test whether differences in cell shape and actin organization can emerge purely from mechanical interactions.

By incorporating the mechanochemical feedback loop (MCFL-I), the model captures how heterotypic interfacial tension redistributes mechanical stresses between mutant and wild-type cells. These stresses lead to differences in cell area, perimeter, and shape, which are then translated via MCFL-I into distinct bulk and junctional actin signatures. Consequently, even though the intrinsic parameters are the same, the emergent mechanical environment reproduces the experimentally observed differences in actin intensity and cell shape indices (as shown in Figure 2).

Thus, our approach demonstrates that the experimentally observed heterogeneity between mutant and wild-type cells can arise solely from interface-driven mechanical effects, without prescribing any cell-type-specific parameters in the model.

(4) Also provide data for cell line tensions in the vertex model, which can then be compared with the experimental data in Figure 2. This is especially important because the differential cell line tension at the interface of mutants and wild-type cells seems to be playing a very important role.

The cell tensions from the vertex model have been plotted in the response to main comment (3) from Reviewer 2. Since the interfacial tension has been included as an extra term in the vertex model by hand, it is not trivial to simply compare the line tensions from the vertex

model to the experimental data. However, we can understand how the tensions are by looking at the normalised tension and normalised contractility plotted as a response to comment (4) from Reviewer 1. Those plots are from a vertex model with mechanochemical feedback and the plots match well with experimental actin images.

(5) In Figure 2j, the authors should report the relative cell pressure and line tension for all four ROIs. The data is only shown for the wild-type cells and for mutants in clusters, even though the figure caption states that the data is presented for all four ROIs. It would also be useful to report the cell tension at the interface between the mutant cells and wild-type cells since this is the key parameter for the vertex model simulations.

We agree and have updated the graph [Figure 2j].

(6) The tangential motion of cells around oncogenic clusters only shows up towards the end of Supplementary Video 3. It is unclear whether this is a transient effect or whether this tangential motion would persist for a longer time.

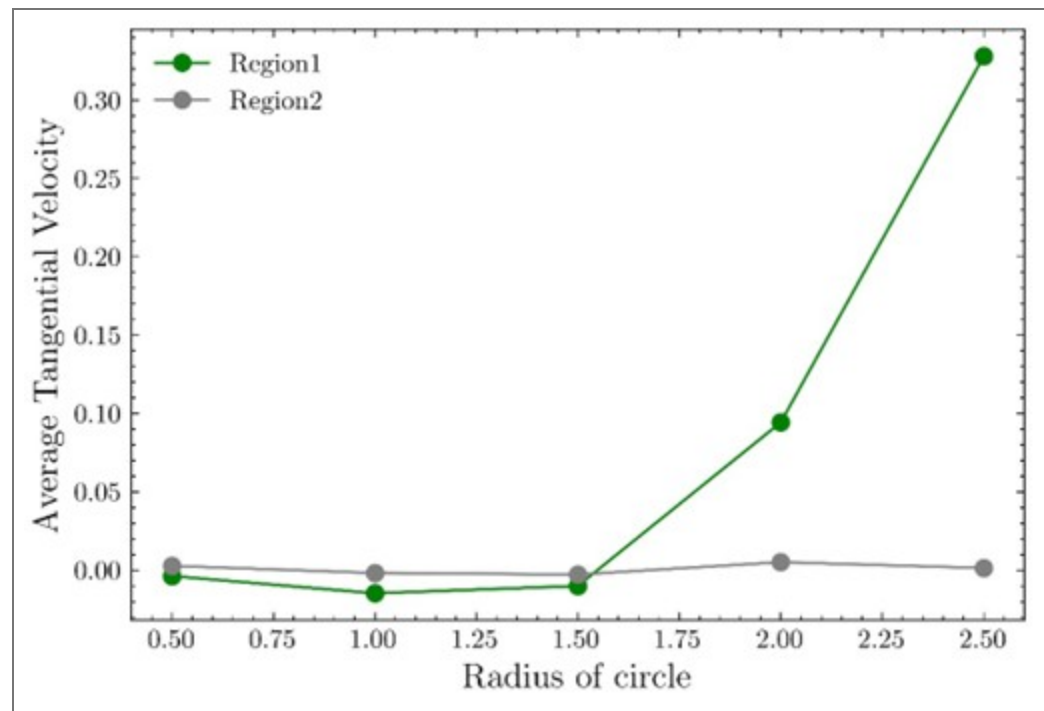
We thank the reviewer for raising this point. In our experiments, tangential cell motion in the wild type population along the boundary of oncogenic cluster consistently emerges as the oncogenic cluster becomes compacted. We have plotted tangential velocity in interfacial wild type cells over time (Supplementary Fig. 6b), and show that such a motion persists at the cluster-wild-type interface, until the end of time-lapse recordings in all cases.

(7) It is very awkward that the authors are representing an integral of the tangential velocity over different loops in Figures 3c and 4i. Thus, it is very hard to separate how much of the increase in the integrated velocity is due to larger loops and how much is due to changes in the average tangential velocity. Since different loops have different perimeters, it would have been better to report the average tangential velocity by dividing the integrated tangential velocity by the perimeter length of each loop. In the methods, the authors state that the concentric circles go from the center to a point twice the radius of the mutant cluster, but this is not consistent with the image in Figure 3c, where the concentric circles seem to go only to the boundary of the mutant cluster.

We thank the reviewer for raising the point regarding the dependence of the loop-integrated tangential velocity on the perimeter length. While the circulation (loop-integrated tangential velocity) indeed scales with loop size, it increases with radius only if tangential velocity components are directionally coherent along the loop.

In our data, concentric-loop analysis centered on mutant clusters reveals a systematic increase in tangential motion with radius, with the largest values occurring at the outermost loops corresponding to the cluster–tissue interface. In contrast, applying the identical analysis to randomly selected wild-type regions does not yield any monotonic increase with radius, despite the increasing perimeter of the loops, and instead shows fluctuations around zero. This control demonstrates that the observed increase around mutant clusters is not a trivial geometric consequence of larger loop size but reflects the emergence of coherent tangential motion specifically at the mutant cluster boundary.

To further address the reviewer's concern, we additionally computed the mean tangential velocity by normalizing the loop-integrated tangential velocity by the loop perimeter. As shown in Supplementary figure. 6a, this normalization preserves the same qualitative trend: tangential motion peaks near the periphery of mutant clusters, whereas no such trend is observed in wild-type regions. We therefore conclude that both metrics capture the same physical phenomenon: enhanced tangential cell motion localized to the mutant cluster boundary, consistent with the behavior observed in the time-lapse videos.



Author response image 2. From simulation data

(8) The authors should comment on how jamming and unjamming are related to shape indices because some readers may not be familiar with them.

We have updated the same in the text of Results 2.

(9) In the captions of Figure 3, the authors state that the bronchial epithelium gets kinetically arrested. This is not evident from the data in Figure 3d, where the velocity magnitude drops just a little bit for the bronchial epithelium, and it remains much higher compared to the mammary epithelium at long times.

We agree with this comment, and that using the word, kinetically arrested, for Beas2b cells is misleading, since their motion is much higher, even after the initial drop. We have updated the text in the caption accordingly.

(10) It is unclear why the authors have used the segregation index for analyzing experiments and the demixing parameter for analyzing simulations. Both parameters are trying to quantify the same thing, so it would have been better to use the same quantity for both experiments and simulations to enable easier comparison.

We agree that using the same quantity for both experiments and simulation would enable easier comparison. Thus, we have replaced the demixing parameter with segregation index in Figure 4.

(11) It is unclear what experimental data were used for shape indices in Figure 4c. Was it the data from Mcf10a or Beas2b? It is also unclear which ROIs were used because different ROIs have very different shape indices in experiments, according to Figure 2e,f.

We have used the experimental $\Delta(S_{\text{interface}} - S_{\text{ROI}}) = 0.75$, which is a rough estimate of the difference between the shape indices for ROI 2 (interface), and ROI 1, ROI 3 and ROI 4 (away from interface) from Fig. 2 e for MCFL10a.

(12) The authors find that the differences in shape indices are non-zero even for $\Lambda=0$ for some threshold pressure parameters $P_{i,0}$ in Figure 4c. This should not

happen because all the cells are identical in that case. This suggests that either there are not enough statistics from the simulations or that something is wrong with the simulations. How is this simulation data obtained? Is it from a single simulation, or is this averaged over a certain number of simulations? Authors should perform multiple simulations and report both the mean values and the standard deviation.

We have addressed this in the response under main comments (1) and (2) from Reviewer 2.

(13) It is unclear how the cell extrusion was simulated in the vertex model.

Extrusion probability calculation: Simulations with just a single mutant cell were run for a range of differential interfacial line tension values ($\Lambda = 0, 0.1, 0.4, 0.8, 1.2, 1.6$) with shape tension coupling. The simulation was run till the area of the mutant cell fell below a threshold area = 0.1, after which we consider the mutant cell to be extruded. 9 different random initial seeds were run and analysed. Each seed gives a binary result – either extruded or not. This was used to calculate the extrusion probability. We have added this section to the Appendix.

(14) The authors claim that HRas^{V12} clusters in bronchial epithelium grew on top of one another, but it is not clear how this can be observed in Figure 2b or in any other Figure.

We thank the reviewer for raising this point. Our original statement that cells were growing on top of each other was based on observations from the Z-stack images, which allowed us to resolve cell positions along the apico–basal axis. However, since these Zstack data are not included in the current manuscript, we agree that this claim cannot be directly supported by the figures shown. We have therefore removed this statement from the text and restricted our conclusions to what is directly supported by the presented data.

(15) In the main text, the authors state that bronchial epithelial cells exhibited higher F_{actin} intensities compared to mammary bronchial cells, but this difference is not statistically significant according to Figure 5e.

We agree with the reviewer and have thus changed the text because even though the F_{actin} intensities seemed higher in bronchial epithelium visually, the difference was not statistically significant.

(16) The definition of eccentricity is incorrect in the text. The authors state that the eccentricity is quantified as the ratio of the length of the minor axis to the major axis of an ellipse. According to this definition, the eccentricity would be 1 for a circle and not 0.

We have updated the definition of eccentricity in the text to the correct one, including the correct equation.

(17) It is unclear whether the active force F_{act} is used in the vertex model simulations. The active force is defined, but then its value is never specified. Note that the motility force is also an active force, so it is unclear why the motility and active forces were separated.

In our model, the line tension force arising from the shape tension coupling is the active force. We agree that the motility force is also an active force, however, in the absence of any directional movement for instance, the homeostatic tissues in discussion here, we have discounted the role of motility force in our mode, presented here.

(18) The authors use inconsistent naming for different types of epithelia throughout the manuscript. MCF10A cells are referred to as either mammary epithelium or breast epithelium, and Beas2b cells are referred to as either lung epithelium or bronchial epithelium. Because of the very broad spectrum of journal readers, it may not be obvious to all readers that different names refer to the same cell types.

We have updated the text to keep the naming consistent throughout.

(19) Many references to individual figure panels in the main text are incorrect. The authors should carefully check all the references to figures.

We apologize for these errors. We have updated the incorrect references after carefully reviewing the entire manuscript.

(20) In Figure 5, panel b is incorrectly labeled as d.

We have corrected the same.

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