

Reviewed Preprint

v1 • April 23, 2026

Not revised

✉ For correspondence:

d.bush@ucl.ac.ukm.walker@ucl.ac.uk

[§] Present address: Neurologie, Département des Neurosciences Cliniques, Geneva University Hospitals and University of Geneva, Geneva, Switzerland

Competing interests: M.W. has acted as a consultant for Seer and EpilepsyGtx. He is a founder shareholder in EpilepsyGtx. He has received honoraria from Eisai, Angelini, and UCB pharma.

Funding: See [page 23](#)

Reviewing editor: Helen Scharfman, Nathan Kline Institute, United States

© 2026, Sheybani et al. This article is distributed under the terms of the [Creative Commons Attribution License](#), which permits unrestricted use and redistribution provided that the original author and source are credited.

Fast-ripples are emergent properties of neuronal networks

Laurent Sheybani^{1,2,3,5}, Yichen Qiu¹, Prince Kumar Singh⁴, Umesh Vivekananda^{1,2,3,5}, Neil Burgess^{1,5}, Beate Diehl^{1,2,3}, Andrew McEvoy^{1,2,3}, Anna Misericocchi^{1,2,3}, James A Bisby⁶, Tawfeeq Shekh-Ahmad⁴, Gabriele Lignani¹, Daniel Bush⁷✉, Matthew C Walker^{1,2,3}✉

¹Research Department of Epilepsy, UCL Queen Square Institute of Neurology, University College London, London, United Kingdom • ²National Hospital for Neurology and Neurosurgery, University College London Hospitals NHS Foundation Trust, London, United Kingdom • ³NIHR University College London Hospitals Biomedical Research Centre, London, United Kingdom • ⁴The Institute of Drug Research, The School of Pharmacy, Faculty of Medicine, The Hebrew University of Jerusalem, Jerusalem, Israel • ⁵Institute of Cognitive Neuroscience, University College London, London, United Kingdom • ⁶Division of Psychiatry, University College London, London, United Kingdom • ⁷Department of Neuroscience, Physiology and Pharmacology, University College London, London, United Kingdom

eLife Assessment

This **valuable** study addressed a key question in epilepsy research: whether the recordings of very fast oscillations in the brain (>250Hz, fast ripples) reflect underlying pathology or might be a property that emerges from a neuronal network at random. The strengths of the study are the importance of the question, the multiple methods, and the **solid** evidence. However, there are limitations to the methods that should be addressed.

<https://doi.org/10.7554/eLife.110803.1.sa3>

Abstract

Fast-ripples have been proposed as a promising biomarker in epilepsy, but their specificity remains unclear. In particular, it is uncertain whether they reflect chance coincident neural activity or distinctly generated pathological entities. We combined *in silico* simulations, neuronal cultures, a rodent model of hippocampal epilepsy, and human microwire recordings to investigate whether fast-ripples occur more frequently than expected by the chance aggregation of action potentials. Our simulations showed that chance aggregation can generate fast-ripples and predicted higher occurrence during wakefulness, which was confirmed in rodent recordings. The likelihood of exceeding chance depended on biological system complexity and vigilance state: fast-ripples in neuronal cultures did not surpass chance, whereas those in awake – but not sleeping – rodents did. Similarly, the frequency of fast-ripples in awake human recordings was ~30% greater than expected by chance. As such, our findings suggest that most fast-ripples reflect stochastic network activity rather than distinctly generated pathological entities, challenging prevailing assumptions about their pathogenesis and biomarker specificity.

Introduction

In epilepsy, disease biomarkers are central to diagnosis and treatment, in particular the decision on where to operate (Duncan et al., 2006 [↗](#); Ewen et al., 2025 [↗](#); Zijlmans et al., 2019 [↗](#)). Two main classes of biomarker can be defined. On the one hand, some biomarkers share the same generative mechanisms as the disease itself, making them highly valuable and specific. Other biomarkers are epiphenomena that emerge from activity related to, but not specific to, the disease. While they can also be valuable, great care must be taken not to overinterpret their relevance in diagnostic studies. Importantly, in epilepsy, most biomarkers are epiphenomena. For example, interictal epileptiform discharges and neuroimaging findings provide only indirect spatial information on

the epileptogenic zone – i.e., the parenchyma that needs removal to obtain seizure freedom (Krumholz et al., 2015 [↗](#); Mégevand et al., 2014 [↗](#); Sheybani et al., 2025b [↗](#); Zijlmans et al., 2019 [↗](#)).

Another electrophysiological biomarker that has gained considerable attention is fast-ripples (FRs). FRs are high-frequency oscillations that are proposed to be specific to brain regions that generate seizures (Dimakopoulos et al., 2024 [↗](#); Jacobs et al., 2010 [↗](#), 2008 [↗](#); Nevalainen et al., 2020 [↗](#)), although conflicting results exist in the literature (Dimakopoulos et al., 2024 [↗](#); Klimes et al., 2019 [↗](#); Lisgaras and Scharfman, 2023 [↗](#); Roehri et al., 2018 [↗](#); Sheybani et al., 2019 [↗](#), 2018 [↗](#); Zijlmans et al., 2012 [↗](#), 2009 [↗](#)). FRs are detected in the local-field potential (LFP) at high frequency ranges (lower band: 200-250 Hz (Dimakopoulos et al., 2024 [↗](#); Roehri et al., 2024 [↗](#)); higher band: 500-550 Hz (Dimakopoulos et al., 2024 [↗](#); Roehri et al., 2024 [↗](#); Sheybani et al., 2018 [↗](#))). While lower frequency (< 200 Hz) LFP fluctuations primarily relate to post-synaptic, i.e., dendritic potentials (Cohen, 2017 [↗](#); Staba, 2012 [↗](#)), this higher frequency activity is primarily dictated by local action potentials (APs) (Logothetis, 2002 [↗](#); Ray et al., 2008 [↗](#)). Indeed, previous studies have consistently demonstrated that FRs reflect sequences of APs generated at a specific frequency or inter-spike interval (Dzhala and Staley, 2004 [↗](#); Foffani et al., 2007 [↗](#); Ibarz et al., 2010 [↗](#); Staba, 2012 [↗](#); Ylinen et al., 1995 [↗](#)).

Despite decades of research into FRs (Ylinen et al., 1995 [↗](#)), it remains unclear whether they represent distinct pathological entities unique to epilepsy or arise from coincident neural activity that may be more prevalent in, but is not specific to, epileptic networks. The recent identification of high-frequency oscillations in neurodegenerative diseases supports this conceptual shift (Lisgaras and Scharfman, 2023 [↗](#)). Hence, FRs could emerge when there is chance clustering of APs giving rise to an oscillatory pattern. Alternatively, they could occur as pathological entities distinct from other brain processes, characterized by their own specific mechanisms of generation. Conceptually, this distinction is similar to the finite monkey theorem, which states that letting a monkey press randomly on a typewriter will eventually lead to it writing the entire works of Shakespeare. Hence, FRs could either be the product of a succession of chance clusters of APs (i.e., English letters) or distinct entities (i.e., full English words, Fig. 1a [↗](#)).

Here, using an *in silico* model, multi-electrode array (MEA) recordings of neuronal cultures, an animal model of focal epilepsy, and human microelectrode recordings, we asked whether FRs are distinct phenomena or result from the chance clustering of APs. This is central to understand whether the high incidence of FRs in the epileptogenic zone (Dimakopoulos et al., 2024 [↗](#); Jacobs et al., 2008 [↗](#)) is simply a byproduct of altered network properties such as firing rate and synchronization, or whether the epileptogenic parenchyma displays intrinsic characteristics that generate FRs independent of these properties. Our results show that the majority of FRs in rats and humans occur as a result of chance clustering of APs, that this proportion fluctuates along the sleep-wake cycle, and that the occurrence of emergent FRs is constrained by the overall size of the neural population, neural firing rate and synchronization. These results call for a re-evaluation of the role of FRs as specific biomarkers of epilepsy and support their high susceptibility to changes in neural excitability. This contrasts with the view that they mainly represent specific products of the epileptogenic parenchyma, independent from network properties (Bragin et al., 2000 [↗](#)).

Results

FRs can occur as emergent phenomena *in silico*

In the finite monkey theorem, it has been calculated that the universe would most likely end before the entire works of Shakespeare would be written (Woodcock and Falletta, 2024 [↗](#)). Similarly, it could be that the mean firing rate of a neural population and its level of synchronization are such that it very rarely leads to emergent FRs within the duration of an EEG recording or human lifespan. To test this, we first constructed a simulation based on background activity sampled from a human intracranial microelectrode recording, and inserted APs arising from incremental numbers of neurons (population of 1-2000 neurons, 50 steps), with progressively increasing mean firing rates (1-20 Hz, 50 steps) and level of synchronization (50 steps

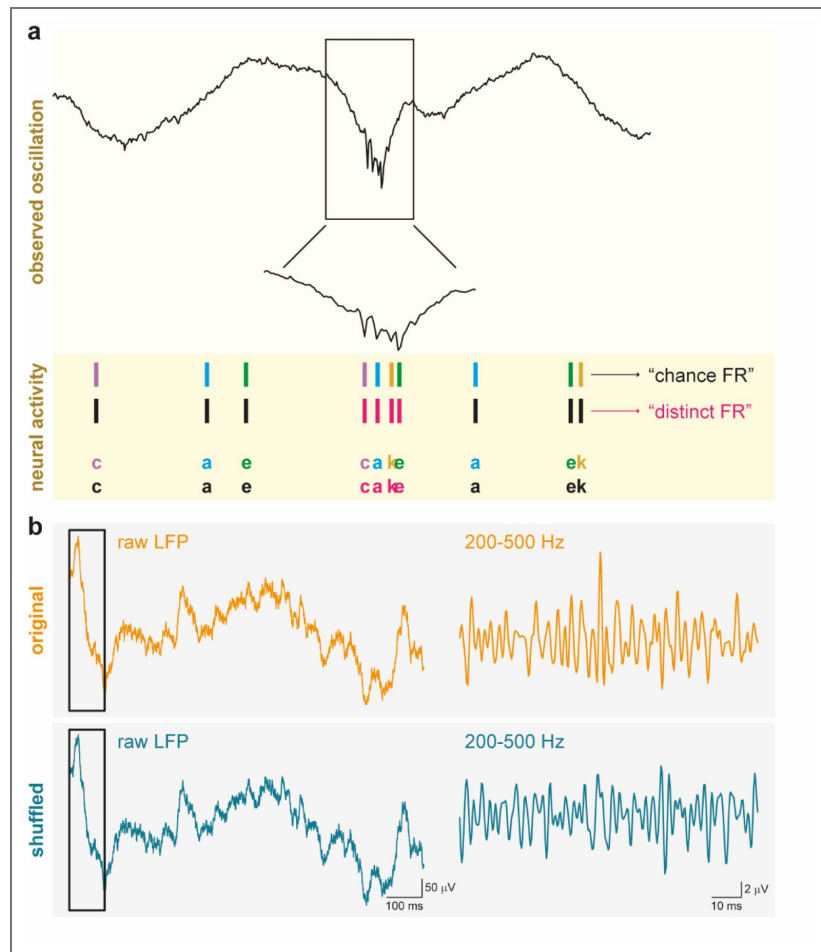


Figure 1. Are FRs “chance activities” or “distinct phenomena”?

(a) Fast-ripples (FRs) can arise by the chance plesiochronous firing of neurons or can be generated as distinct entities akin to a pathological motif. Similarly, words can emerge either by chance when tapping randomly on a typewriter, or as individual lexical entities. (b) To investigate the relative proportion of true and chance FRs, we shuffled EEG signals within the frequency band of interest (200-500 Hz). This disrupts any ‘true’ FRs and therefore allows us to estimate the incidence of chance FRs. The black rectangles on the left are filtered and expanded on the right.

exponentially related to the Fano factor, a measure of the dispersion of neural discharges, Fig. 2a and Supplementary Fig. 1. Similar approaches have been described previously (Zanos et al., 2011). Numerous studies have shown that high frequency activity in the LFP reflects neuronal discharges (Fedele et al., 2020; Manning et al., 2009; Quiroga et al., 2004; Ray et al., 2008) and that neuronal discharges are the building blocks of FRs (Foffani et al., 2007; Ibarz et al., 2010; Staba, 2012), supporting our approach. The model confirmed that FRs can emerge by chance, i.e., as a result of randomly inserting APs (Fig. 2b), and display the expected spectral signature of FRs (Fig. 2c-d).

Emergent FRs index neuronal population, firing rate and synchronization

Different simulations, i.e., with different neuronal count, firing frequency and synchronization parameters, could lead to the same incidence of FRs (Fig. 2e). Hence, we next tested whether changes in the incidence of FRs was random across simulations or whether it could be predicted by changes in neuronal count, firing frequency and/or synchronization. An absence of stochasticity would imply that FR incidence is dictated by one, or a combination of, these parameters.

We found that across the space of 125,000 (i.e., 50*50*50) parameter values, we observed a structured pattern in the number of detected FRs (Fig. 2f-i). We then sought to determine if this pattern was constrained by neuronal count, firing rate and synchronization. To do so, we ran a gradient boosted tree (GBT) to predict the number of detected FRs based on these three features. The GBT predicted a distribution of FR densities which was similar to the true density of FRs (Fig. 3a-b) across solution points ($r^2=0.73$, $p<0.0001$, Fig. 3c). When shuffling the three parameters (neuronal count, firing rate, synchronization), we found that the explained variance (R^2) was significantly lower than the variance explained by the original GBT model (mean \pm standard deviation [SD] at chance level: 0.02 ± 0.001 , $p=0.002$, Fig. 3d), confirming that neuronal count, firing rate and synchronization are significant predictors of the incidence of FRs. Importantly, this analysis excludes the possibility that detected FRs were only those already present in the background microelectrode signal, which was fixed across all simulations. Hence, not only can FRs emerge due to coincident neural firing, but their incidence indexes the size of the neuronal population, its mean firing rate and level of synchrony.

FR rate is at chance level in neuronal cultures

The model described above predicts that FRs can occur as the result of chance firing. We hypothesized that in a simple biological system such as a neuronal culture, FRs would not be more frequent than this expected “chance rate”. To test this, we recorded the activity of neural cultures using MEAs under a baseline condition and after administration of the GABA_A receptor antagonist picrotoxin, a pro-seizure compound that increases network excitability and the generation of epileptiform activity (Supplementary Fig. 2). We hypothesized that if FRs arise purely from chance firing, then temporally shuffling these recordings while conserving their spectral properties (Supplementary Fig. 3) would disrupt any oscillatory structure, leaving only FRs that occur due to chance. We identified FRs in original signals (Fig. 4a), but they were not significantly more frequent than in the shuffled signals (main effect of shuffling: $F(1,15)=0.99$, $p=0.33$, Fig. 4b). In addition, we did not identify a main effect of picrotoxin ($F(1,15)=1.53$, $p=0.24$) or shuffling * picrotoxin interaction ($F(1,15)=1.11$, $p=0.31$). Hence, neural networks with limited complexity (Kim et al., 2020; Saglam-Metiner et al., 2024; Sanchez-Vives and McCormick, 2000; Timofeev and Chauvette, 2017) fail to generate FRs beyond that expected from the chance coincidence of APs, even after increasing network excitability.

FR rate is predicted by neural firing rate and synchronization

Next, we used a rodent model of temporal lobe epilepsy to study the emergence of FRs *in vivo*. Across week-long recordings, and in line with the known variability of FRs across time (Gliske et al., 2018), we observed a diurnal variation in FR rate (Fig. 5a-c, orange trace). By comparing

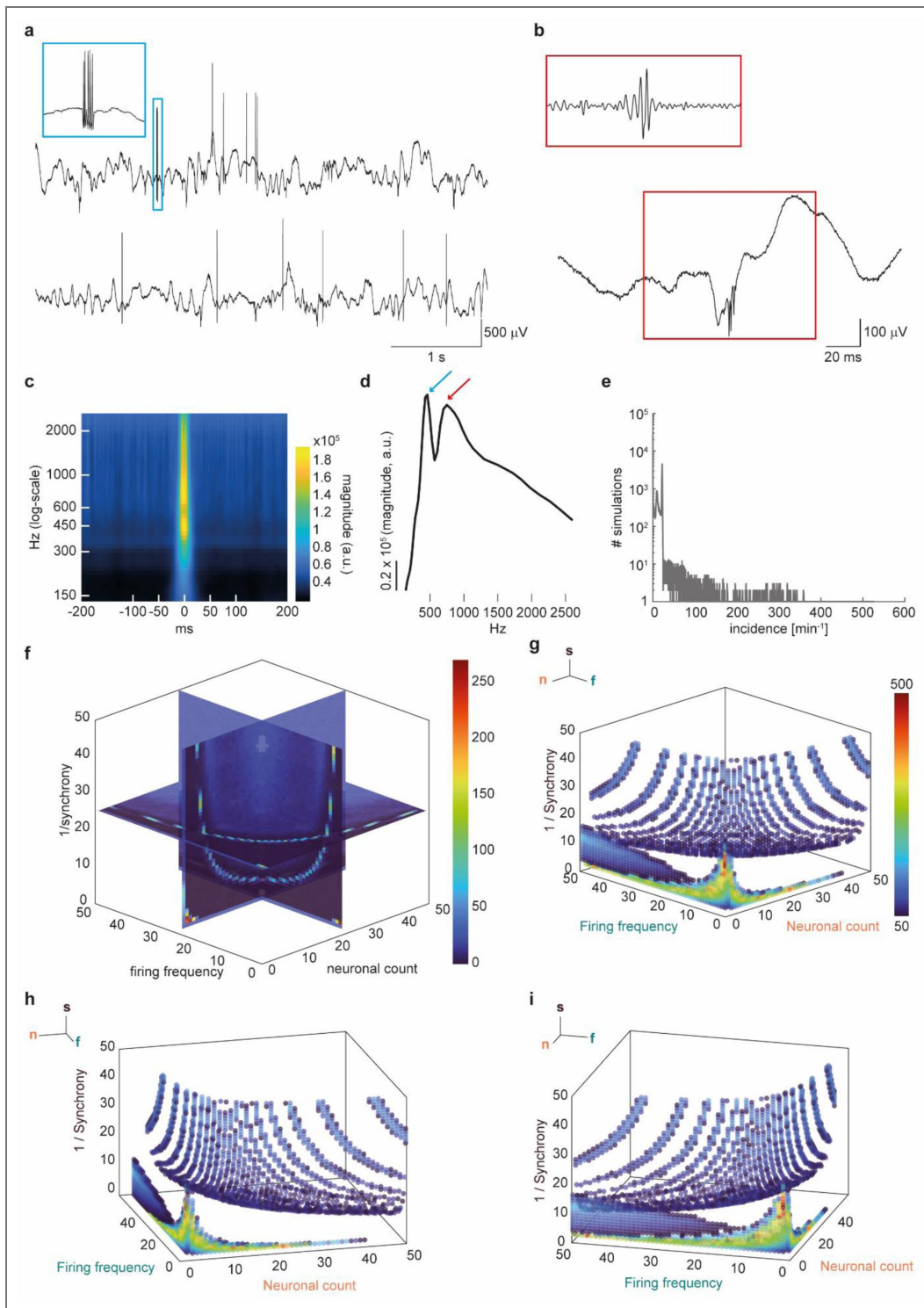


Figure 2. Fast-ripples (FRs) can arise from stochastic neural firing

(a) Example of 5-s activity from 2 signals with inserted action potentials (APs). Across their entire length (480-s), both signals contain a similar number of APs but the upper trace displays more synchrony than the lower trace, where firing is even. The blue squares highlight a burst of highly synchronized APs. (b) Identification of FRs in simulated signals. (c) Time-frequency representation of detected FRs in simulated signals. (d) Spectrogram of detected FRs in simulated signals. The left peak (blue arrow) reflects FRs and the right peak (red arrow) reflects individual APs. (e) Number of simulations (y-axis) per FRs rate (x-axis). (f) Number of detected FRs across all simulations (50×50×50=125,000) with varying numbers of neurons, mean firing frequency, and synchronization. FRs do not occur randomly; a pattern can be identified, indicating that these three parameters control the expression of FRs. (g-i) Solution points for > 50 FRs to better highlight the pattern of expression. n=neuronal count, f=firing rate, s=synchronization.

Figure 3. Neural count, firing frequency and synchronization constrain the emergence of FRs

(a) Density of FRs across the 125,000 solution points of the simulation. (b) Density of FRs across the 125,000 solution points predicted by a gradient boosted tree (GBT). As seen, the distribution is very similar with (a). (c) All solution points predicted by the GBT (y-axis) along corresponding solution points of the original simulation (x-axis). The correlation is significant ($r^2=0.73$, $p<0.0001$). (d) *Blue* Performance of the GBT to predict FR number, should FRs be randomly distributed across values of neural count, firing frequency and synchronization (500 permutations). *Orange* Performance of the GBT to predict FR number in actual simulations.

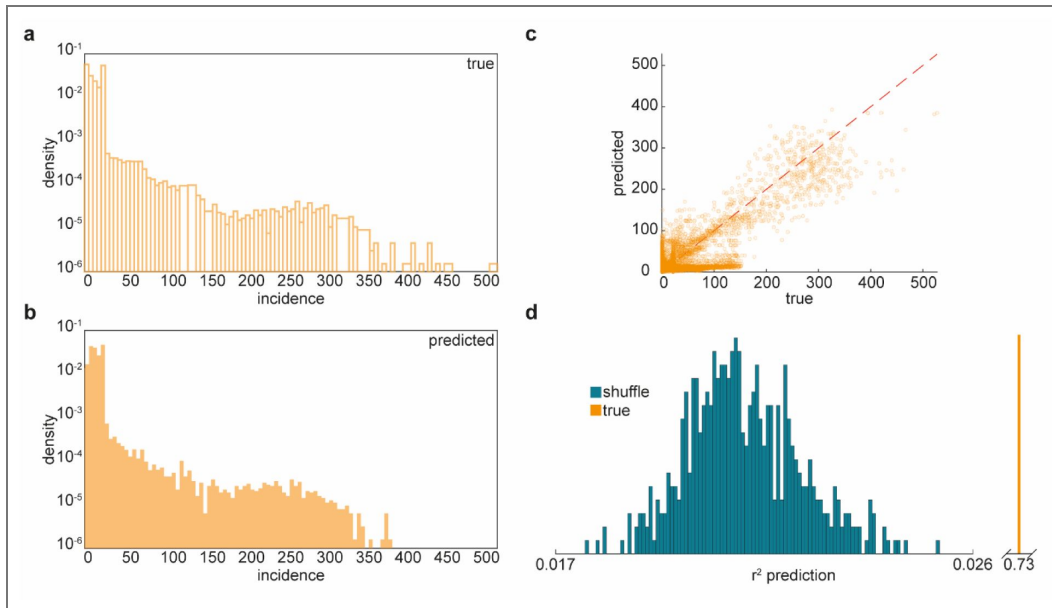
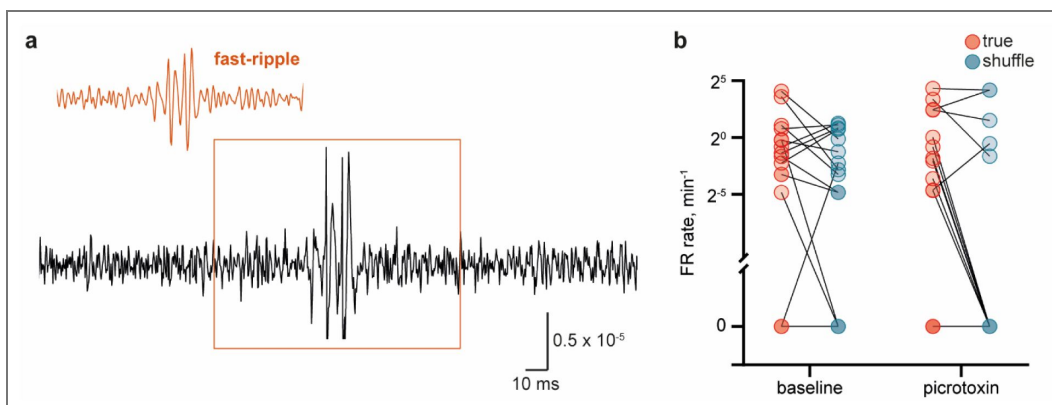


Figure 4. FRs in neural culture

(a) Example of a detected FR in an MEA recording of neural culture. (b) In the MEA recordings, there are no more FRs than expected by chance ('shuffle') during baseline or in a pro-epileptic state following application of picrotoxin.



FR rate to delta power, we could infer how FRs evolve across different vigilance states, assuming that high and low delta activity reflect sleep and wake periods respectively (Osorio-Forero et al., 2024). FRs were more frequent during periods of presumed wakefulness: indeed, FR incidence was strongly modulated by delta activity (Supplementary Fig. 4a) and peaked at delta power troughs (Supplementary Fig. 4b). Importantly, these findings were robust to the specific method used to detect FRs (Supplementary Fig. 4c) (Padmasola et al., 2024; Sheybani et al., 2019, 2018). Furthermore, we confirmed that the higher incidence during wakefulness was not due to movement artifacts (Bénar et al., 2010). Indeed, FRs were visually concordant with those described in the literature (Supplementary Fig. 5) and not associated with surges in broadband high frequency activity that might reflect muscle artifacts (Supplementary Fig. 6).

Given our simulation results, we hypothesised that this diurnal variance may arise from fluctuations in firing rates and synchronization, which are known to decrease and to increase during sleep, respectively (Frauscher et al., 2016; Miyawaki et al., 2019; Staba et al., 2002; Watson et al., 2016). To test this, we first established the peaks of FR rate variability, which, as expected, were identified at 24-hour intervals (Supplementary Fig. 7). Based on this period, we then randomly sampled different simulations to generate synthetic results at hourly intervals over 70 days, with the only constraint being that firing rate decreases and synchronization increases during sleep (Frauscher et al., 2016; Miyawaki et al., 2019; Staba et al., 2002; Watson et al., 2016). Sleep was defined as a 12-hour period surrounding the maxima of delta activity, which also peaked at 24 hour intervals (Fig. 5b). Using only these two constraints, the model exhibited a daily fluctuation of FR rate, which was higher during wake than sleep (Fig. 5a and 5c, green trace). The actual rate of FRs was significantly more correlated with the predicted rate (median r^2 coefficient, IQ range: 0.07, [0.04-0.12]) than with a shuffled version of the predicted rate (0.0009, [0.0009-0.001], $p=0.008$, Wilcoxon test) and the ability of the model to predict periods of high and low incidence rate of FRs was significant (mean AUC \pm SD: 0.64, \pm 0.05, $p<0.0001$, one-sample t-test, Fig. 5d). Furthermore, the periodogram of FR incidence in virtual EEGs also displayed a clear peak at 24 hours (Supplementary Fig. 8). Hence, changes in neural firing rate and synchronization across the sleep-wake cycle can explain the increased incidence of FRs during wakefulness *in vivo*.

The relative proportion of distinct and chance FRs depends on brain state

That neural firing rate and synchronization modulate chance FR incidence does not exclude the possibility that distinct FRs may still occur. To determine the proportion of distinct FRs in our chronic *in vivo* recordings, we again computed the incidence of FRs in original and temporally shuffled signals. Similar to the rate of FRs in the original signal, we observed a daily fluctuation of FRs in the shuffled signal (Fig. 5a, blue trace) and in the ratio of FR rate in the original to shuffled signal (Fig. 5a, purple trace). We then tested if this ratio varies depending on brain state, i.e., sleep vs wake. As already shown, and similar to FR rate, delta activity fluctuated with a period of 24 hours, reflecting sleep periods (Fig. 5b, top). We filtered delta activity at the corresponding frequency (Fig. 5b, middle and bottom) and identified peaks and troughs of this filtered signal (Fig. 5b, open and grey disks). We then compared the ratio of FR rates (original : shuffled) at these timepoints using a 2-way ANOVA (condition kainate: before vs after; condition delta: at peaks vs at troughs). We found a significant kainate * delta interaction ($F(1,7)=17.1$, $p=0.004$, Fig. 5e). Post-hoc testing showed that the ratio of original : shuffle FR rates was higher at delta troughs than peaks after kainate injection (0.51, [0.37-0.65], adjusted $p<0.001$), but not before (mean difference, 95% CI: 0.16, [0.02-0.30], $p=0.12$). Importantly, the ratio decreased at delta peaks after kainate injection (0.24, [0.10-0.38], adjusted $p=0.02$, Fig. 5e) but not at delta troughs (-0.11, [-0.25 to 0.03], adjusted $p=0.41$, Fig. 5e). Furthermore, it shows that the probability of observing FRs that arise purely from the chance clustering of APs varies with brain state.

Last, we found that before kainate injection, the FR rate ratio was not greater than 1, whether it was computed at delta power troughs (1.5, [1-2], adjusted $p=0.09$) or peaks (1.3, [0.8-1.9], adjusted $p=0.41$). Hence, in non-epileptic animals, FRs are no more frequent than expected by chance. In

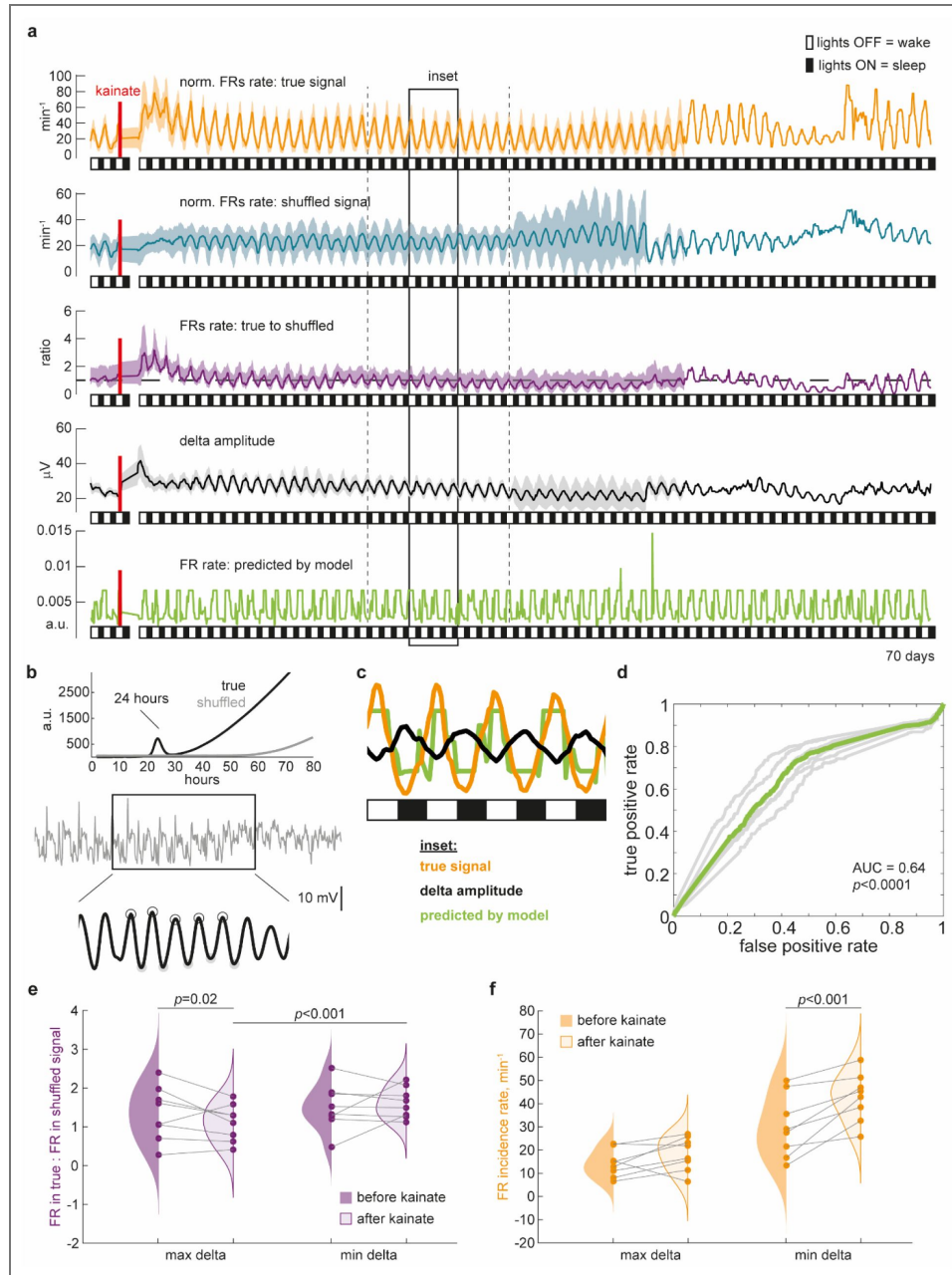


Figure 5. The proportion of FRs as distinct entities varies across the sleep-wake cycle

(a) Incidence of FRs in the original signal (orange trace), shuffled signal (blue), the ratio of FR incidence in the original to shuffled signals (purple), delta amplitude (black) and predicted incidence of FRs across time. Here and after, these metrics are sampled at a rate of h^{-1} . (b) Periodogram of delta amplitude across days. A clear peak at 24 hours is seen in original (black) but not shuffled (grey) data. (c) Fluctuation of FR incidence across days in the data (orange) and as predicted by the model (green), overlaid on fluctuations in delta amplitude. (d) AUC of the model to predict high (above median) and low (below median of individual rats' FR incidence rate) values of FR incidence rate. The AUC is significantly above chance level, i.e., 0.5 (mean \pm SD: 0.64 \pm 0.05, $p < 0.0001$, one-sampled t-test). Each grey line is one animal, the green line is the average across animals. (e) Two-way ANOVA comparing the ratio of FR incidence rate in original to shuffled signals, before and after kainate injection, sampled at delta peaks (max delta) and troughs (min delta). There is a significant kainate * delta interaction ($F(1,7)=17.1$, $p=0.004$) and post-hoc tests show that the ratio is different before and after kainate injection only at delta peaks (mean difference, 95%: 0.24, [0.10-0.38], $p=0.02$). (f) Two-way ANOVA comparing the incidence rate of FRs before and after kainate injection, sampled at delta peaks and troughs. We observed a significant kainate * delta interaction ($F(1,7)=14.7$, $p=0.006$). The incidence rate after kainate injection increased only when sampled at delta troughs (12.6 min^{-1} , [9.0-16.3], $p < 0.001$) and not peaks (4.2 min^{-1} , [0.5-7.9], $p=0.12$).

contrast, after kainate injection, we observed a FR rate ratio that was significantly greater than one at delta troughs (mean, 95% CI: 1.6, [1.3-2], adjusted $p=0.006$, one-sampled t-test) but not peaks (1.1, [0.7-1.5], adjusted $p>0.99$, one-sampled t-test). This indicates that, in contrast to non-epileptic animals, epileptic animals exhibit more FRs than would be expected by chance, but only during wakefulness. Note that this ratio was significantly different between delta troughs and peaks after kainate ($p=0.0003$, paired t-test). Hence, the specificity of FRs to epilepsy is shaped by vigilance states.

Diurnal variation of FR rate as a confound in their interpretation

In practice, clinicians calculate the absolute incidence of FRs, and not the ratio of original to shuffled FRs. Hence, we then asked whether the absolute rate of FRs is impacted by the sleep-wake cycle. Indeed, the periodicity of FR rate could contribute to discrepant interpretations regarding the impact of kainate injection. Visually, while FR rate at troughs of FR incidence seems relatively stable after kainate injection, the FR rate at peaks of FR incidence tends to increase (Fig. 5a [↗](#), orange). To assess this statistically, we computed a 2-way ANOVA, comparing the incidence rate of FRs before and after kainate injection at the peaks and troughs of delta amplitude identified previously (Fig. 5b [↗](#)), and found a significant kainate * delta interaction ($F(1,7)=14.7$, $p=0.006$, Fig. 5f [↗](#)). Post-hoc testing showed that FR rate was higher after than before kainate injection at delta power troughs (mean difference, 95% CI: 12.6 min^{-1} , [9.0 to 16.3], adjusted $p<0.001$), but not at delta peaks (4.2 min^{-1} , [0.5 to 7.9], adjusted $p=0.12$). This confirms that changes in FR incidence after induction of epilepsy varies across the sleep-wake cycle. Hence, the absolute rate of FRs increases after kainate injection during wakefulness (Fig. 5f [↗](#)). However, the lack of change in terms of FRs ratio (original : shuffled) during wakefulness, after kainate injection (Fig. 5e [↗](#)), makes it likely that this absolute change is due to changes in general network excitability, rather than the emergence of FRs as distinct entities.

The majority of FRs also occur by chance during wakefulness in humans

Finally, we asked whether FRs in the human brain were more frequent than expected by chance. To do so, we examined intracranial microelectrode recordings from 10 patients who underwent presurgical epilepsy evaluation. Microwires were implanted in the mesial temporal lobe in all subjects and recordings were obtained during wakefulness. We proceeded again by shuffling the original data and then identifying FRs in the original and shuffled signals (Fig. 6a [↗](#)).

We found a main effect of signal type (original vs shuffled: $F(1,770.4)=20.62$, $p<0.001$, Fig. 6b [↗](#)), confirming that FRs are more frequent in the original signal than expected by chance. Specifically, the original recordings displayed ~ 1.6 times more FRs than shuffled recordings, such that about 3 FRs can be considered distinct pathological entities for each 5 FRs occurring by chance ($8/5 = 1.6$), making distinct FRs only 37.5% of all those detected (Fig. 6c [↗](#)). Interestingly, the proportion of distinct to chance FRs in these awake subjects is similar to that seen in awake rats (Fig. 5e [↗](#)). To verify that the shuffling procedure was not underestimating the proportion of FRs in the original data, we used 5 other shuffling algorithms that were conceptually different (see Methods). None of them displayed a significantly different rate of FRs in original than in shuffled data (Supplementary Fig. 9 [↗](#)).

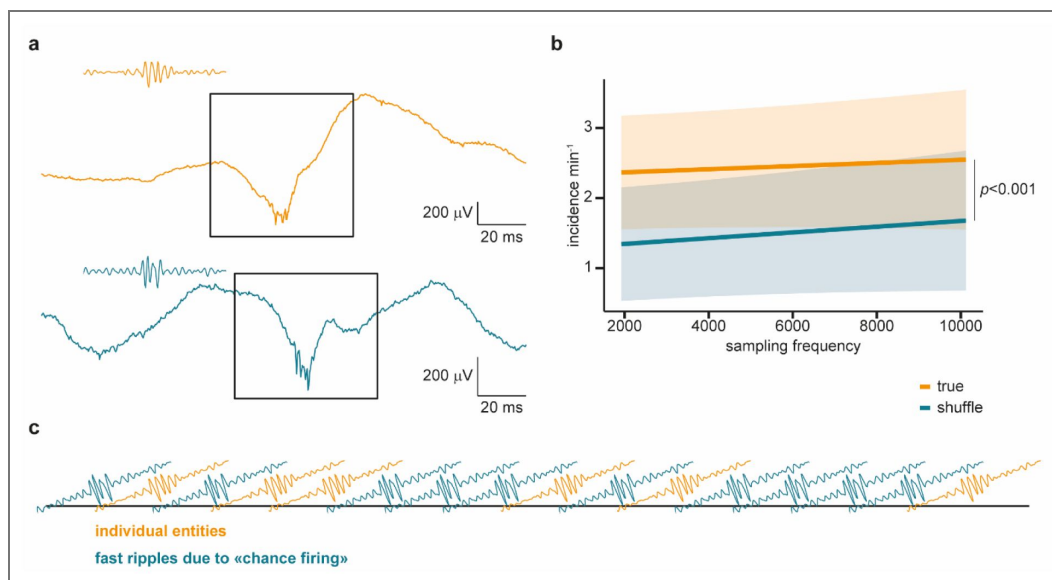


Figure 6. FRs as distinct entities in humans are uncommon

(a) Example of a FR detected in the original signal (orange) and shuffled signal (blue). (b) Incidence of FRs per minute in the original and shuffled signals, across sampling frequencies (3,000; 4,000; 5,000; 6,000; 8,000; 10,000; 15,000 Hz) to assess any possible effect of sampling frequency. We observed only a main effect of signal type (original vs shuffle, $F(1, 770.4)=20.62$, $p < 0.001$) but no interaction ($F(1,770.4)=0.05$, $p=0.82$) or main effect of sampling frequency ($F(1,13.2)=0.47$, $p=0.51$). (c) Illustration of the proportion of FRs in the original signal and in the corresponding shuffled signal. This ratio is of 3:5. Hence, distinct FRs account for only 37.5% of all detected FRs.

Discussion

Here, we report that distinct FRs, i.e., those that do not emerge as the chance clustering of APs, account for around a third (37.5%) of all detected FRs during wakefulness in humans. Furthermore, both the incidence rate and relative proportion of distinct FRs vary with brain state, making this electrophysiological entity more complicated to interpret than previously thought (Menendez de la Prida et al., 2015 [↗](#); Roehri et al., 2018 [↗](#)). Although different network properties can lead to similar incidences of FRs (Fig. 2e [↗](#)), as is the case across different levels of excitability in MEA recordings (Fig. 4b [↗](#)), our results indicate that FRs are linked to different network properties (Fig. 2 [↗](#)–3 [↗](#)).

In our rodent data, we were initially surprised to find a higher rate of FRs during wakefulness. However, previous studies only indicate that physiological vs pathological FRs are more easily discriminated during NREM sleep (von Ellenrieder et al., 2016 [↗](#)) and that their incidence varies during sleep (Von Ellenrieder et al., 2017 [↗](#)), but in hours-long recordings, no differences in incidence have been noted in the mesial temporal lobe (Dümpelmann et al., 2015 [↗](#)). While short recordings (10 min) have provided suggestive evidence of a higher rate during sleep (Bagshaw et al., 2009 [↗](#)), they should be interpreted with care, given the variability of FRs across time (Gliske et al., 2018 [↗](#)). The prediction from our *in silico* simulation aligns with our experimental findings (higher rate during wakefulness, when firing rates increase and synchrony decreases), further supporting our conclusions.

The fact that our *in silico* simulations predict a higher rate of FRs during wakefulness, based on the assumption of higher synchronization and lower firing rates during sleep (observed in multiple studies (Frauscher et al., 2016 [↗](#); Miyawaki et al., 2019 [↗](#); Staba et al., 2002 [↗](#); Watson et al., 2016 [↗](#))), further supports the hypothesis that intrinsic network parameters contribute to changes in FR incidence. We found not only that the sleep-wake cycle is associated with a varying proportion of distinct to chance FRs, but also that this changes after kainate injection. This is crucial in epileptology, where the question of how specific FRs are to the epileptogenic parenchyma remains open (Dimakopoulos et al., 2024 [↗](#); Roehri et al., 2018 [↗](#); Sheybani et al., 2019 [↗](#), 2018 [↗](#); Zijlmans et al., 2012 [↗](#), 2009 [↗](#)). Hence, FRs reflect and are highly susceptible to changes in network excitability. This is consistent with recent findings of HFOs in neurodegenerative diseases (Lisgaras and Scharfman, 2023 [↗](#); Shandilya et al., 2024 [↗](#)), where hyperexcitability could potentially be a driver of cognitive decline (Vossel et al., 2016 [↗](#)). Moreover, a recent study on ripples (70-180 Hz) reported that these events can largely be attributed to changes in background noise levels (Van Schalkwijk and Helfrich, 2026 [↗](#)).

In conditions of constant neural population size and firing rate, high synchronization leads to FRs that are clearly distinguishable from background, while low synchronization leads to a more continuous oscillatory background (see Fig. 2a [↗](#) for illustration). It has previously been shown that brain regions with HFOs clearly distinguishable from the background are more likely to be part of the seizure-onset zone (Melani et al., 2013 [↗](#); Minthe et al., 2020 [↗](#)). Importantly, this pattern is also more likely to occur during sleep (Minthe et al., 2020 [↗](#)). This again supports the validity of our model, which also assumed more synchronization during sleep. Since this pattern is more prevalent during sleep and can differentiate brain regions from inside and outside the seizure-onset zone, it could also explain why sleep recordings are better at identifying the seizure-onset zone than wake recordings (Sheybani et al., 2025a [↗](#)).

How do we reconcile our findings with reports of specific mechanisms underlying the generation of FRs? Indeed, several candidate mechanisms have been identified, including a necessary role of gap junctions (Curot et al., 2023 [↗](#); Demont-Guignard et al., 2012 [↗](#); Draguhn et al., 1998 [↗](#); Dzhala and Staley, 2004 [↗](#); Fabo et al., 2023 [↗](#); Foffani et al., 2007 [↗](#); Köhling and Staley, 2011 [↗](#); Schlingloff et al., 2025 [↗](#); Schmitz et al., 2001 [↗](#); Sheybani et al., 2019 [↗](#); Traub et al., 2001 [↗](#); Valero et al., 2017 [↗](#)). However, most studies report mechanisms that are likely or even proven to impact network properties, such as firing rate, synchronization or even neuronal count, which we have shown contribute to the chance occurrence of FRs. For example, lower ephaptic transmission

contributes to decreased spike-timing reliability during sharp-waves ripples and has been suggested to lead to pathological FRs in rats (Foffani et al., 2007). However, this could be driven by decreased neuronal count (Foffani et al., 2007). Even electrical coupling via gap junctions, which has been reported to be a core mechanism of generation of FRs (Draguhn et al., 1998; Schmitz et al., 2001; Traub et al., 2001) could modulate FRs incidence through its impact on synchronization (Bennett and Zukin, 2004; Hürkey et al., 2023). Hence, previous literature may have focused mainly on mechanisms that affect network properties, but not directly FRs.

In contrast, an intriguing property of FRs, which would support the hypothesis that they arise from specific mechanisms, and not inherent properties of the network, is their highly stereotypical morphology (Sheybani et al., 2018). In fact, previous research has provided evidence that FRs of the seizure-onset zone are more stereotypical than those generated elsewhere (Liu et al., 2018). Nevertheless, this is not inconsistent with our findings: our results do not indeed exclude the possibility that some FRs are not consecutive to the chance occurrence of plesiochronous APs. In fact, they support the conclusion that a subset of FRs are distinct entities. Importantly, however, those constitute a minority of all detected FRs, which is lower than expected from their prominence as a biomarker of epilepsy. This could explain divergent findings concerning their specificity to the epileptogenic zone (Dimakopoulos et al., 2024; Jacobs et al., 2010, 2008; Klimes et al., 2019; Nevalainen et al., 2020; Roehri et al., 2018; Sheybani et al., 2019, 2018; Zweiphenning et al., 2022). The reason why FRs have been relatively successful in the delineation of the seizure-onset zone (Dimakopoulos et al., 2024; Jacobs et al., 2010, 2008; Klimes et al., 2019; Roehri et al., 2018; Zweiphenning et al., 2022) could thus reflect the fact that changes in network properties that promote the emergence of FRs are also associated with epileptogenicity; but this does not mean that FRs have their own specific generative mechanisms. This is a crucial difference in our quest to understand the mechanisms underlying FRs, and their coupling with epileptogenic zones.

One central point that must be emphasized is the validity of our shuffling procedure. The algorithm shuffles only the high-frequency component of the signal, bypassing lower frequency activity that could contribute to higher frequency artifacts (although the FR detection algorithm used here is meant to control for this (Roehri et al., 2018)). Shuffled data exhibits comparable spectral composition to the original signals. Furthermore, our results are supported by five other shuffling procedures, which failed to identify an increased incidence of FRs in physiological data. Hence, we argue that FRs in biological signals are only slightly more frequent than chance, and this can be captured only by the most sophisticated shuffling methods.

Finally, it is important to stress that our study does not suggest that FRs are artefactual. They are genuine oscillations, generated by clusters of APs. Suggesting that FRs are artifacts of the signal is different from stating that FRs appear as a result of the chance clustering of APs within an appropriate time window. The latter is correct and contributes to a significant proportion of FRs. This must be now taken into consideration when studying mechanisms of generation of FRs and seizures, and the role of FRs as disease biomarkers.

Methods

Mouse primary neuronal culture recording with multielectrode array (MEA)

Embryonic cortical neuronal cultures were prepared from E18-19 wild type C57BL/6J embryos, plated at density of 50k/well at DIV0 onto recording areas pre-coated with PLL (P2636-25MG) and laminin (L2020-1MG) onto Axion CytoView 24-well plate (M384-tMEA-24W, Axion systems). The MEA system was plated at very high density and this could have led to a ceiling; however, as shown in the simulations, relationship between neural density and FRs rate is neither linear nor monotonic. Each well contains 16 electrodes, covering estimated area 1.1mm x 1.1mm. Activity from the same well shares network properties and culture environment, but this is not fundamentally different from sampling > 1 brain region spatially close to each other. Neurons were maintained at 37 degrees, 5% CO₂ with appropriate humidity, with 25% media change every

week. Electrophysiological recordings were taken with Mastro Edge system (version 3.7.1.16) where the neurons were maintained at 37 degrees and 5% CO₂, for 10-20 minutes per session. Recordings were processed at 12.5 kHz sampling frequency, with low and high pass filter set at 3 kHz and 200 Hz, respectively (Axion Navigator). When PTX (picrotoxin) treatment was applied, 50 mM picrotoxin was dissolved in DMSO, where 50 μ M was used for triggering neuronal network activities at DIV20. Baseline data were recorded prior to picrotoxin treatment, and post-picrotoxin treatment recordings were taken 24 hrs afterwards. The analysis of spiking, bursting and network burst were carried out with Axion navigator (Axion systems). Raw spiking data was exported with Neural Metric Tool (Axion systems) into csv. format for subsequent analysis. All experiments were carried in compliance with Home Office Project Licence (PP3944290).

Rat recordings and preprocessing

All experimental protocols were conducted in compliance with the Association for Assessment and Accreditation of Laboratory Animal Care (AAALAC) International standards and were approved by the Institutional Animal Care and Use Committee (IACUC) of the Hebrew University of Jerusalem. This study utilized male Sprague–Dawley rats (150–175 gm; the Hebrew University strain) obtained from the Harlan Laboratories Israel Ltd. (Jerusalem, Israel). All animals were housed under controlled conditions (23 \pm 1 $^{\circ}$ C, 50–60% humidity, 12 h light/dark cycle) with free access to food and water. A minimum acclimatization period of one week was allowed before any experimental procedure to ensure adaptation to the housing environment.

Surgical procedure: ECoG transmitter implantation

All animals underwent for implantation of high frequency electrocorticography transmitters (ECoG) under general inhalation anesthesia (induction at 3% isoflurane, maintenance at 1.8–2.3%; Terrell™, USP, Piramal Critical Care). Animals were positioned in a stereotaxic frame (Kopf Instruments, CA, USA) for stereotaxic surgeries. Presurgical analgesia was administered subcutaneously including buprenorphine (0.2 mg/kg; Rich Pharma) and meloxicam (1 mg/kg; Chanelle Pharma). Animals were implanted subcutaneously with a high-frequency single-channel ECoG transmitter (model A3049T5, sampling rate 2048 Hz; Open-Source Instruments, USA) featured with two subdural intracranial electrodes. The recording electrode was placed epidurally above the right dorsal hippocampus (AP -2.8 mm, ML +1.5 mm), while the reference electrode was positioned contralaterally (AP -6.0 to -7.0 mm, ML +3.5 mm). Epidural recordings are highly effective in capturing fast-ripples generated in the hippocampus (Sheybani et al., 2018 [DOI](#)). The electrodes were secured to the skull with screws and tissue adhesive to ensure stable signal acquisition. Following implantation, the cranial incision was sealed with dental cement. Postoperative care including warmed Ringer's solution for rehydration and amoxicillin (100 mg/kg; Betamox LA) to prevent post-surgical infection were administered subcutaneously. Animals were monitored until full recovery and returned to their home cages. One to two weeks recovery period was observed before subsequent experiments.

Induction of status epilepticus

All rats implanted with ECoG transmitters were subjected to status epilepticus (SE) induction using a single intraperitoneal injection of kainic acid (KA; 10 mg/kg; 5 mg/mL in 0.9% saline; Hello Bio, UK). Following injection, animals were continuously monitored for seizure activity via a wireless ECoG telemetry system coupled with CCTV cameras, enabling real-time acquisition of seizure activity during SE development. SE was behaviorally defined by the experimenter as the onset of sustained class V seizures, according to a modified Racine scale (Racine, 1972 [DOI](#)), characterized by rearing, forelimb clonus, and loss of posture. Two hours after SE onset, diazepam (10 mg/kg, *i.p.*; Assival®, Teva Pharmaceuticals, Israel) was administered to terminate seizures and minimize mortality. Only animals that exhibited continuous convulsive activity throughout the 2-hour post-SE induction window were included in the study.

ECoG data acquisition and Analysis

All animals with subdural ECoG transmitters were housed individually under continuous 24/7 wireless video-ECoG (vECoG) monitoring. ECoG signals were wirelessly transmitted and recorded using Neuroarchiver software (Open-Source Instruments Inc.), enabling high-frequency, high-resolution data acquisition with real-time processing capabilities.

Recorded ECoG traces were segmented into 4-second epochs and analyzed across six quantitative parameters: total power, intermittency, coastline, coherence, asymmetry, and 0.2–640 Hz band power. Each feature was normalized to a 0–1 scale and compared against a user-generated seizure reference library containing validated seizure episodes derived from at least three different animals. Seizure identification was performed using an automated detection algorithm, which classified epochs as seizure-like events if their Euclidean distance from the reference library was <0.2, following established protocols [Open-Source Instruments, Event Detection; (https://www.opensourceinstruments.com/Electronics/A3018/Event_Detection.html)].

All automatically detected seizures were subsequently reviewed and confirmed by the blinded investigator. In addition, a subset of detected events was validated using time-synchronized video recordings from cage-mounted CCTV cameras (Microseven). These videos were independently assessed by a second blinded researcher to verify concordance between electrographic seizure activity and behavioral manifestations, thereby ensuring reliable event classification. Among the 10 rats, 8 developed seizures and only epileptic rats were included in analyses. Prior approval was granted by local Ethics Committee (Institutional Animal Care and Use Committee, The Hebrew University of Jerusalem; Protocol Code: MD-20-16254-5).

Patient recordings and preprocessing

We included microelectrodes recordings from ten patients. All patients had intracranial electrodes placed for presurgical evaluation of epilepsy and the research protocol did not intervene in the placement of electrodes. These participants were included in a project on memory and slow waves in epilepsy, part of which has already been published (Sheybani et al., 2023).

Behnke-Fried electrodes were inserted in the mesial temporal lobe and signals were recorded at 30 kHz using a Blackrock Neuroport system (Blackrock Neurotech LLC).

Signal artefacts were identified by eye and removed from all analyses. Before FR detection, we notch filtered the data at 50 Hz (49-51 Hz, *bandstop.m* in Matlab). Data were then downsampled to 3000 Hz, 4000 Hz, 5000 Hz, 6000 Hz, 8000 Hz, 10000 Hz and 15000 Hz after applying a low-pass anti-aliasing filter at half the new sampling frequency. This was intended to test whether sampling frequency affects the proportion of FRs as distinct phenomena. Prior approval was granted by local Ethics Committee (15/LO/1783).

FR detection

We used the widely used Delphos detector (Roehri et al., 2016), which has been validated for the detection of FRs (Roehri et al., 2017). The detector measures specific time width and frequency spread of candidate events, which are identified as islands in normalized time-frequency images. This detector has been used in multiple studies focusing on epileptic discharges and high-frequency oscillations (Lambert et al., 2020; Roehri et al., 2018; Schönberger et al., 2021; Shamas et al., 2023). Default settings were used, notably the frequency boundaries for FRs (200–499 Hz). While multiple studies have established that FRs arise from timely generated APs (Foffani et al., 2007; Ibarz et al., 2010; Staba, 2012), ripples reflect post-synaptic potentials (Staba, 2012). This major difference makes the hypothesis that ripples could also emerge from chance firing invalid, explaining why we focus here on FRs generation, not ripples generation.

Detection of FRs in rats could not be visually checked given the large amount of data (c. 11,905 hours of recording). To exclude the possibility that they reflect movement-related artifacts – although Delphos is meant to control for lower frequency artifacts (Roehri et al., 2018) – we computed the proportion of FRs that occur during gamma surges, in both the wake and sleep conditions. To do so, we filtered the signals within the gamma range (20-80 Hz) and estimated

dynamic amplitude using the Hilbert transform. We then defined gamma surges as any epoch of 20 ms around EEG amplitude peaks that were greater than two standard deviations above the mean gamma amplitude across the whole recording. A given FR was considered to overlap with a gamma surge if more than 50% of its duration occurred during such epochs. We also verified our findings using a second, fully independent and published HFO-detector (Padmasola et al., 2024 [↗](#); Sheybani et al., 2019 [↗](#), 2018 [↗](#)). Briefly, the detector identifies candidate FRs in the filtered data (butterworth, order 2, 250-500 Hz) as oscillations with ≥ 4 cycles whose amplitude is higher than 3 times the surroundings 500 ms baseline. These criteria are based on published literature (Bragin et al., 1999 [↗](#); Lévesque et al., 2011 [↗](#)). Candidate FRs that coincided with ripples, high-gamma or gamma activity of a higher intensity are discarded.

To test the circular-to-linear correlation between daily fluctuation of delta amplitude and FRs incidence, the phase of delta amplitude fluctuation was extracted for the frequency defined by the peak periodicity, i.e., 24 hours (see Frequency analysis below).

Virtual simulations

To construct virtual simulations, we first selected one microwire signal based on a lack of movement artefact and presence of > 1 single unit to ensure good signal-to-noise ratio. We then inserted action potentials (APs) corresponding to the mean waveform of all detected APs in Keles et al. (Keles et al., 2024 [↗](#)). The number of APs varied depending on the number of virtual neurons (50 steps from 1 to 2000) and mean firing rate (50 steps from 1 to 20) based on realistic firing (Liebe et al., 2025 [↗](#)) and including a margin to study what can be expected from higher firing rate. To adjust synchronization, we computed inter-spike intervals (ISIs) using an exponential cumulative distribution function (CDF) and varied the mean parameter μ from 1 – to provide a very exponential distribution of ISIs, i.e., high synchronization – to the total number of APs – to provide an almost linear distribution of ISIs, i.e., low synchronization. APs were then inserted into the signal by convolving the signal with the mean waveform of APs. The amplitude of APs was set to be 5.95 times the standard deviation of background noise, following Keles et al. (Keles et al., 2024 [↗](#)).

The computation of virtual simulations follows this step-by-step procedure:

[1] Computation of the mean waveform of all detected APs in Keles et al. (Keles et al., 2024 [↗](#)).

[2] Normalization of the mean AP amplitude to 5.95 times the standard deviation of background noise, based on Keles et al. (Keles et al., 2024 [↗](#)).

[3] Computation of ISIs

[3a] Computation of the total number of APs as the signal duration * mean firing frequency * number of neurons product

[3b] Computation of ISIs as the exponential CDF, varying the μ parameter, which defines the curvature of the CDF, from 1 (highly exponential) to the total number of APs (almost linear distribution of ISIs).

[3c] Randomization of the ISIs, so that long and short ISIs are not temporally clustered.

[3d] Computation of the number of APs per unit of time, based on the ISIs

This process computes one time series for the entire neural population, thus allowing to precisely control for the inter-neuronal synchronization, a parameter that is crucial in the field of FRs (Ibarz et al., 2010 [↗](#)).

The number of neurons recorded by the *in silico* probe was defined by the volume of tissue that can be captured by an electrode's tip, i.e., 200 μm (Harris et al., 2016 [↗](#)). This led to a neural density of $1.73 \cdot 10^3$ within such a sphere (Henery and Mayhew, 1989 [↗](#); Herculano-Houzel, 2009 [↗](#)).

Gradient boosted tree

To test whether neural count, firing rate and synchronization predict the incidence of FRs, we used a gradient boosted tree (GBT, Matlab function *fitensemble.m*) with default parameters (method: 'LSBoost', number of learning cycles: 100). We compared the actual prediction with the

distribution of H_0 , where the number of FRs has been shuffled across neural count, firing rate and synchronization. Across 500 permutations, we saved the coefficient of determination R^2 defined by:

$$1 - \frac{\sum (y_a - y_p)^2}{(y_a - \bar{y}_a)^2}$$

Where y_a is the actual value of FR count, and y_p is the predicted value of FR count. The actual R^2 was then compared with the distribution of chance-level R^2 for statistics.

Temporal shuffling procedure

To generate time-shuffled EEG signals, we used a wavelet-based iterative amplitude adjusted Fourier transform (wavelet-IAAFT) because it best conserved the spectral content and visual appearance of the original signal (see Fig. 1b [↗](#) for an example and Supplementary Fig. 3 [↗](#) for statistical analyses). Indeed, shuffled signals reliably replicated two key properties of the original signal: mean amplitude (original signal, mean \pm SD: 2.5 μ V, [\pm 1.2 μ V], shuffled signals: 2.7 μ V, [\pm 1.3 μ V], $p=0.12$, paired t-test) and dominant frequency within the FR range (original signal, median, IQ range: 411 Hz, [399-417 Hz], shuffled signal: 411 Hz, [400-416 Hz], $p=0.63$, Wilcoxon test, Supplementary Fig. 3 [↗](#)). Furthermore, this approach allows only preselected frequency components of the original signal to be shuffled, thus controlling for any potential contribution of low-frequency activity to the emergence of FRs (see Fig. 1b [↗](#), where the low frequency range is conserved, while the high-frequency range is shuffled). Specifically, this reduces the risk of detecting “false-ripples”, i.e., filtered artifacts of lower frequency range (Bénar et al., 2010 [↗](#)), although Delphos does control for this kind of artifact (Roehri et al., 2018 [↗](#)). This was particularly important for the rat data, where artifacts could not be visually checked (total of c. 11,905 hours of recording).

The algorithm works by decomposing the signal in the frequency domain using a 45-vanishing moment Daubechie wavelet. Then, across coefficients of interest (set at >200 Hz to shuffle only the spectral content that is relevant to FRs), the code extracts the phase of the signal using a fast Fourier transform, generates new (and uniform) phases and then reconstructs the signal iteratively until convergence of amplitude ranks with the original signal. Convergence was assessed using Kullback-Leibler divergence. In animals, shuffling was performed on 1-hour long signals to preserve changes in excitability across time. The code is available on https://github.com/lshyebani/FR_project [↗](#).

Since the shuffling procedure is central to the present work, we added 5 supplementary ways to randomize time-series. We used Fourier transform (FT)-based phase randomization, amplitude adjusted Fourier transform (AAFT)-based phase randomization, autoregressive-based (AR) randomization of residuals, iterative AAFT until convergence of amplitude distribution (IAAFT-1 in Supplementary Fig. 9 [↗](#)) and IAAFT until convergence of spectral power (IAAFT-2 in Supplementary Fig. 9 [↗](#)). FT, AAFT, IAAFT-1 and IAAFT-2 are published methods (Lancaster et al., 2018 [↗](#)). AR was written in-house. Parts of this code were written with the help of artificial intelligence (ChatGPT and Copilot).

Frequency analyses

To compute periodicities of FR incidence and delta amplitude, we first smoothed the data with a sliding window (moving median) of 12 hours to remove small fluctuations in the signals. This was based on visual evidence of slower rhythms for FR incidence and delta amplitude (Fig. 5a [↗](#)). Within animals, we then extracted segments of data for analysis that were at least 48 hours long. We then computed the power spectral density of these signals using Welch’s method (*pwelch* in Matlab) with default parameters (8 segments with 50% overlap, sampling frequency of h^{-1}). We proceeded through the same analyses on shuffled data, where incidence of FR or fluctuation of delta amplitude have been randomly permuted across time, 200 times. Periodicities were then identified by plotting the result of the frequency analyses on a 1/frequency axis (i.e., period).

The time-frequency analysis displayed in [Figure 2c](#) was obtained using a continuous wavelet transform (*cwt.m* in Matlab) and default parameters. For time efficiency, given the large number of virtual EEGs that were generated (125,000) and the consecutively high number of detected FRs, we sub-selected 0.1% of all detected FRs in the virtual signals, which accounted for 5865 events.

Statistical analyses

We used 2-way ANOVA with Fisher's LSD post-hoc test and Bonferroni corrections to adjust *p*-values for multiple comparisons. In human subjects, to test for changes in FR rate across sampling frequencies and conditions (original vs shuffled signal), we used a linear mixed model (LMM):

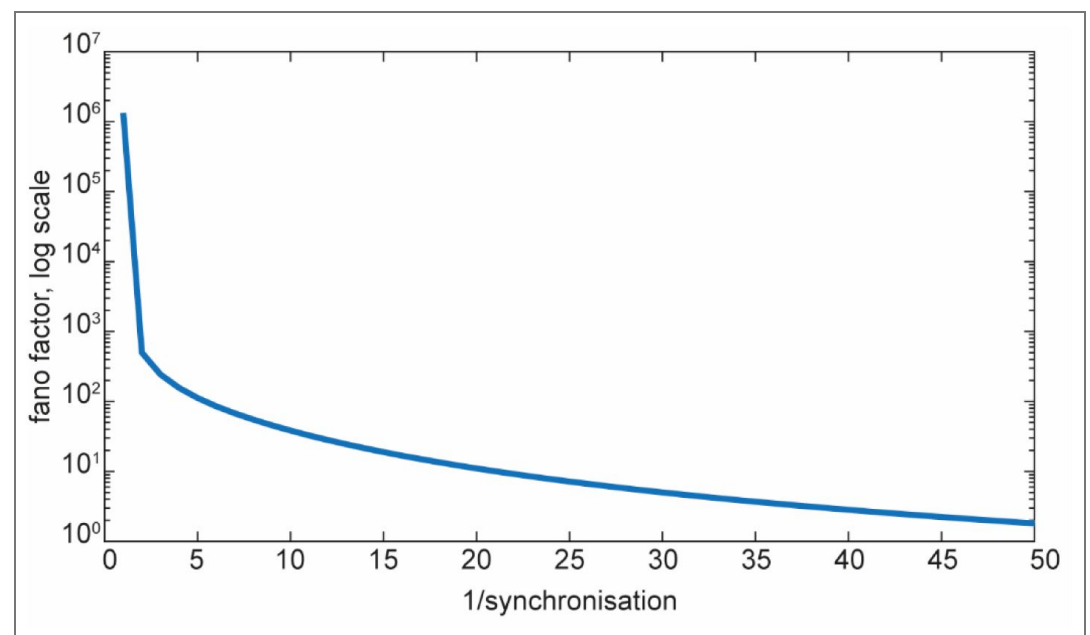
FR incidence $\sim 1 + \text{sampling_frequency} + \text{condition} + \text{sampling_frequency} * \text{condition} + (1 + \text{sampling_frequency} | \text{subjects})$

The LMM was performed in Jamovi (version 2.6.22), using the toolbox Gamlj3 (v. 3.4.2). Fixed effects were statistically tested with Omnibus tests.

Use of Large Language Models

Code for data analyses was written with the help of ChatGPT and Copilot. After using these tools, the authors reviewed and edited the code as needed and take full responsibility for its correctness.

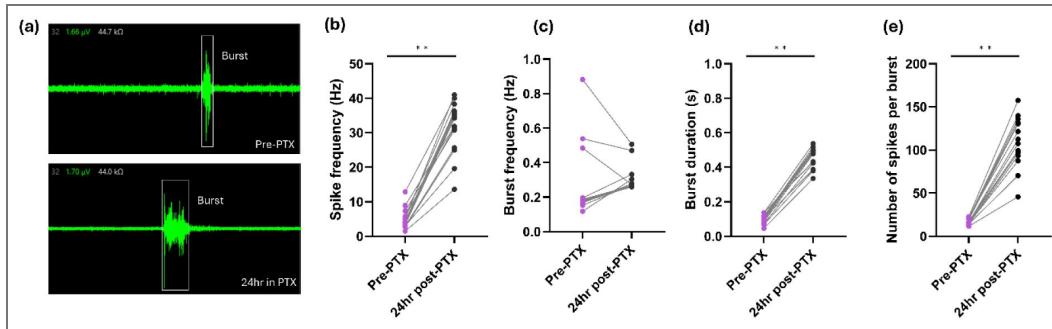
Supplementary Figures



Supplementary Figure 1. Fano factor and level of synchronization The fano factor, defined by the variance of interspike interval divided by its mean, is exponentially related to the level of synchronization of the model.

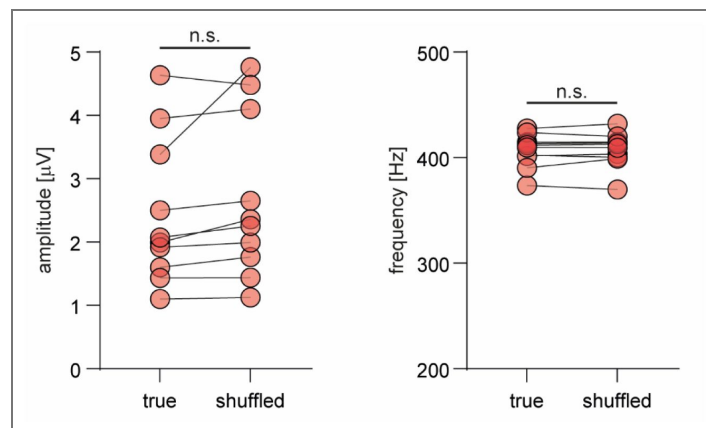
Supplementary Fig. 2. Markers of epileptic activities in MEA are increased after picrotoxin (PTX) application

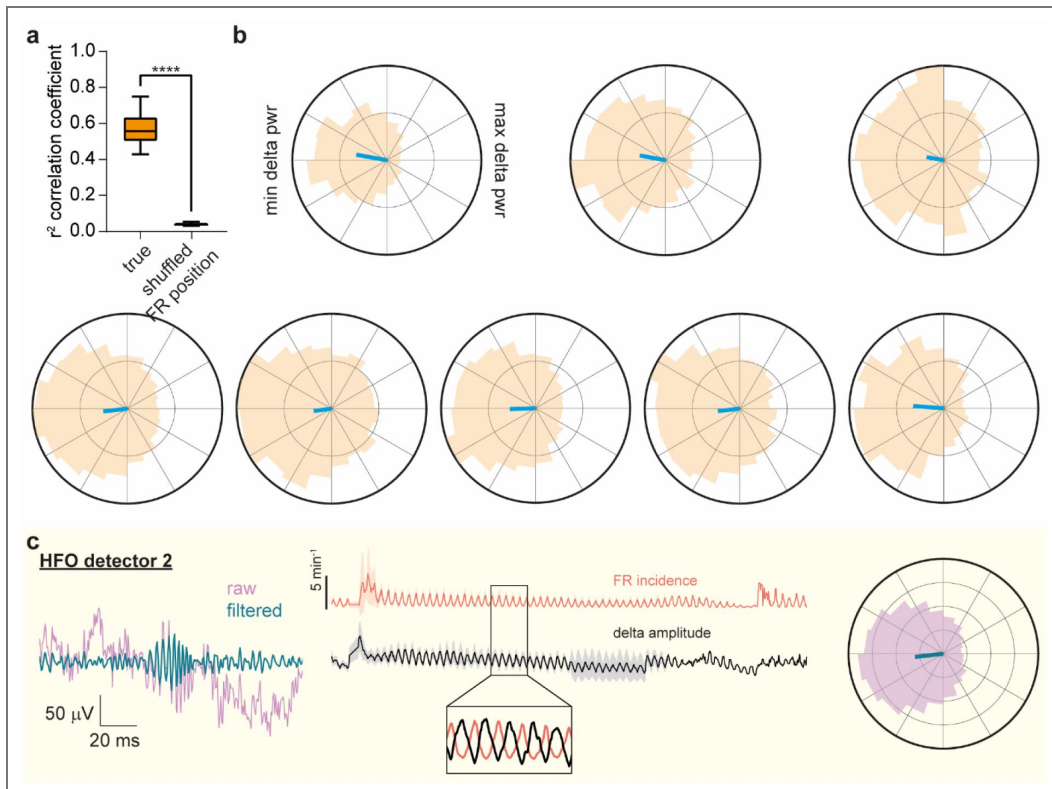
Neuronal subgroup firing events measured by MEA *in vitro* model. **(a)** Example waveforms before and after picrotoxin treatment, where a burst event is highlighted. **(b)** Spike frequency, **(c)** burst frequency, **(d)** burst duration, and **(e)** number of spikes per burst (2-way ANOVA, $p < 0.001$).



Supplementary Fig. 3. Validation of shuffling procedure for high-frequency signals

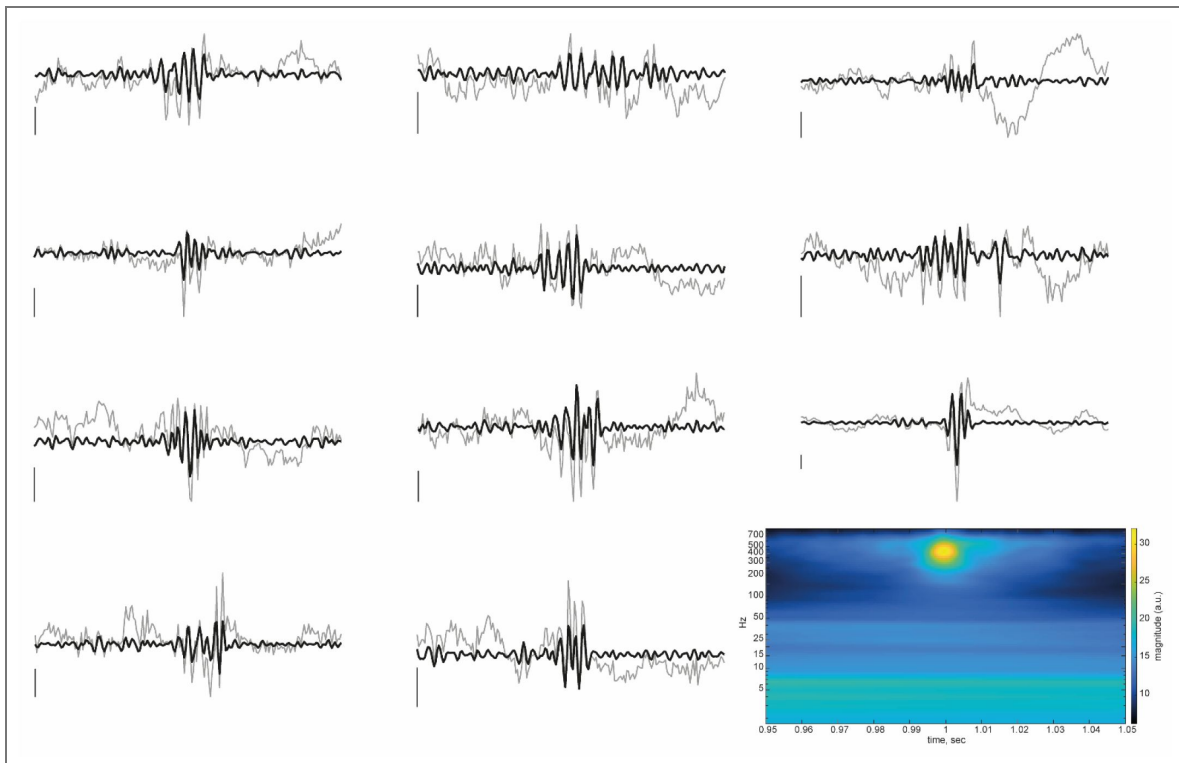
To verify that the signal shuffling did not distort high frequency content, we compared the amplitude (left) and oscillatory frequency (right) of signals filtered within the frequency range of FRs (200-500 Hz) between the original and shuffled signals. There were no significant differences in either measure, confirming the reliability of the shuffling method in preserving the content in high-frequency activity. This validation was performed on human data at a sampling frequency of 3000 Hz.





Supplementary Figure 4. Distribution of FRs incidence along phases of daily delta amplitude fluctuations: group analysis

(a) Circular-to-linear correlation coefficient between phase of delta amplitude trace and incidence of FRs (left box-and-whiskers). The correlation is significantly higher (r^2 coefficient, mean, \pm SD: 0.57, [0.10]) than if FRs occurrence across days is shuffled (r^2 coefficient: 0.03, [0.01], $p < 0.0001$, paired t-test). **(b)** Circular plot between daily delta amplitude fluctuation ($-\pi$ to π) and incidence of FRs. Each panel corresponds to one animal. The maximal incidence of FRs is seen at lowest amplitude of delta fluctuations. **(c)** The inverse relationship between FR incidence and delta fluctuations was further assessed with a second, independent HFO detector. One example FR is depicted (left), as well as the daily fluctuations of FR incidence (middle). Consistent with the results from the original detector, FR incidence was inversely proportional to delta amplitude. Hence, FR incidence peaked at delta troughs (right, circular histogram including all animals).

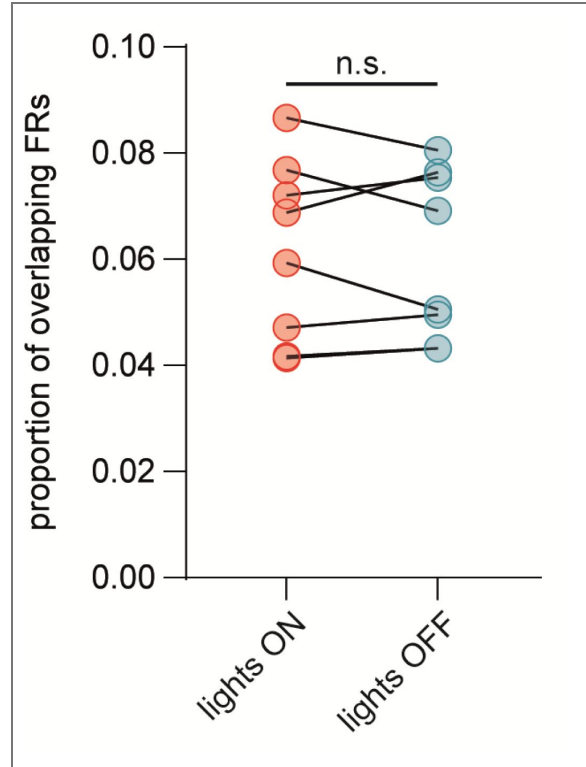


Supplementary Figure 5. Examples of FRs in rats

Examples of FRs in different rats and the time-frequency representation of all detected FRs. See [Supplementary Figure 6](#) for an objective assessment of “false FRs”. Scale: windows of 100 ms, 80 μ V.

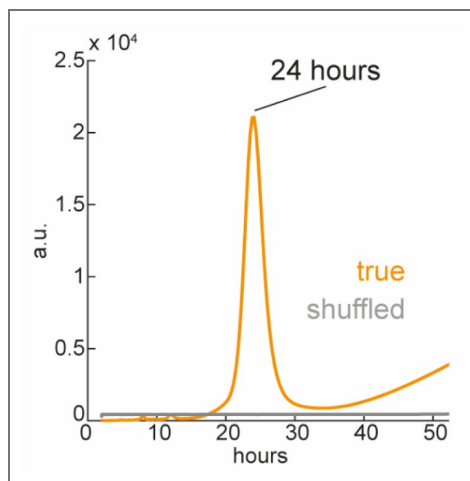
Supplementary Figure 6. Lights ON and OFF are not associated with a different proportion of FRs overlapping with muscle artefact (broadband high-frequency activity)

We computed the proportion of FRs occurring during periods of broadband high-frequency activity (20-80 Hz) as a way to verify that detected FRs are not “false ripples”. The proportion of such doubtful FRs was very low and, importantly, there was no difference between conditions lights ON and OFF (mean, \pm SD, lights ON: 6%, \pm 2%, lights OFF: 6%, \pm 2%, $p=0.74$).



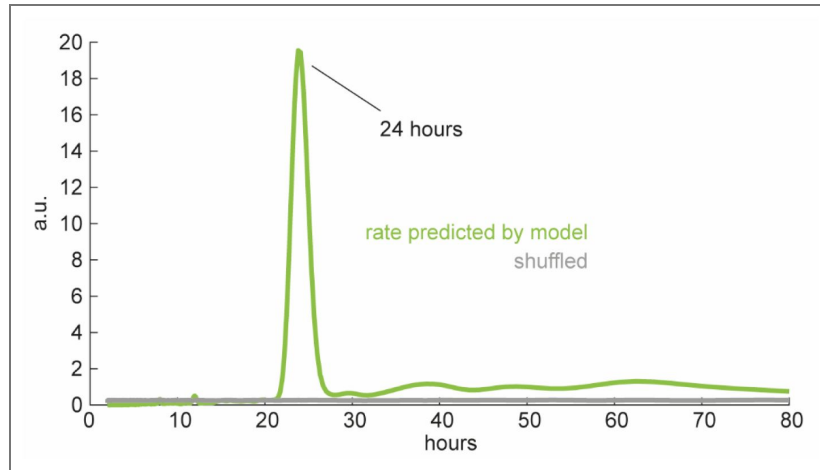
Supplementary Figure 7. FR periodogram identifies a peak of incidence each 24 hours

The periodogram is obtained by computing a frequency analysis over the time-resolved incidence trace of FRs and converting the frequency unit (x-axis) into periods (in hours). A clear peak at 24 hours can be identified, confirming the visually observed daily fluctuation of FRs.



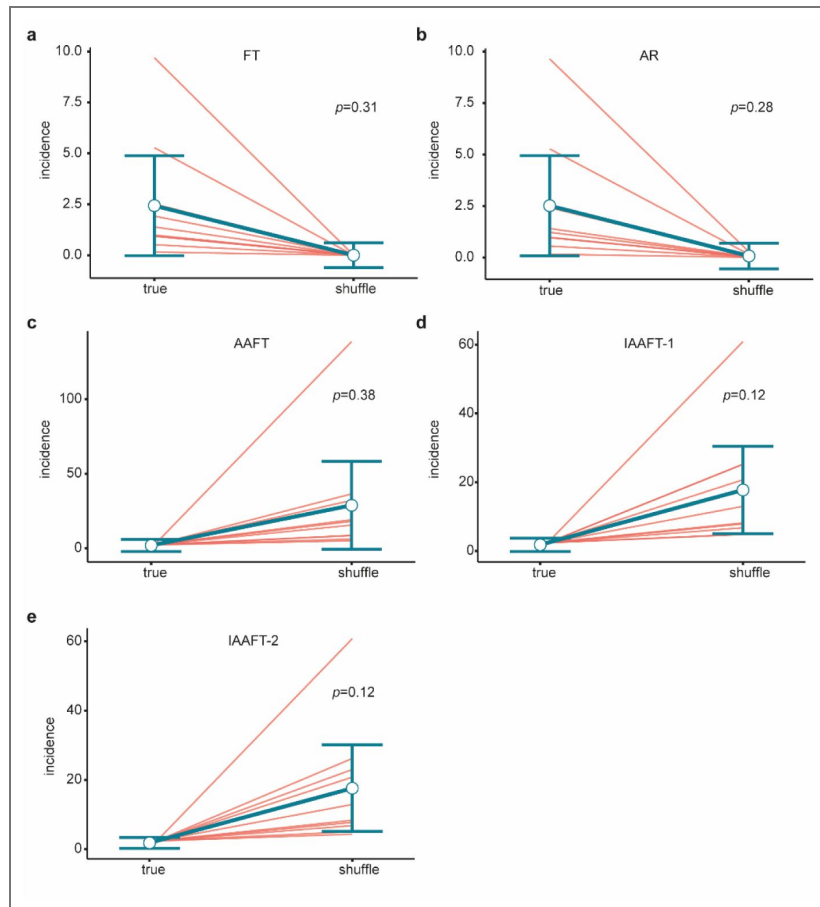
Supplementary Fig. 8. Periodogram of FRs incidence in virtual EEGs

Similar to the rodent data, the incidence rate of FRs in virtual EEGs also displays a period of 24 hours.



Supplementary Fig. 9. FRs are not more frequent than expected by chance when computed with alternative shuffling procedures

We used a (a) Fourier-transform (FT) based, (b) auto-regression (AR), (c) amplitude adjusted Fourier-transform (AAFT), (d) iterative AAFT until convergence of amplitude distribution (IAAFT-1) and (e) IAAFT until convergence of spectrum (IAAFT-2). None displayed a significantly different incidence of FRs between the original and shuffled data.



Data availability

MEA and rodent data can be obtained upon reasonable request from the corresponding author. We will share clinical data on request, provided that request is consistent with the terms of our ethics data collection and analysis.

Acknowledgements

This work was funded by a Guarantors of Brain fellowship and a Swiss National Science Foundation grant to LS (PZ00-3_233452) and supported by the National Institute for Health and Care Research University College London Hospitals Biomedical Research Centre. DB was supported by a UKRI Frontier Research grant (EP/X023060/1).

We are very grateful to Dr. Roman Rodionov for his help in early preprocessing steps of human microwire recordings at UCL. We are very grateful to Dr. Nicolas Roehri for his help in using Delphos for fast-ripples detection.

Additional information

Declaration of generative AI and AI-assisted technologies in the writing process

In early versions of the manuscript, LS used ChatGPT and Copilot for English editing. After using these tools, the authors reviewed and edited the content as needed and take full responsibility for the content of the published article.

Code availability

Code for the project is available from https://github.com/lshybani/FR_project [↗](#).

Funding

Funder	Grant reference number	Author
Guarantors of Brain (Brain The Charity)	Post-doctoral clinical fellowship	Laurent Sheybani
Swiss National Science Foundation	PZ00-3_233452	Laurent Sheybani
UKRI Frontiers Research grant	EP/X023060/1	Daniel Bush

Author ORCID iDs

Laurent Sheybani: <https://orcid.org/0000-0003-4824-6408>

Umesh Vivekananda: <https://orcid.org/0000-0001-6116-2335>

Neil Burgess: <https://orcid.org/0000-0003-0646-6584>

Beate Diehl: <https://orcid.org/0000-0002-6896-854X>

James A Bisby: <https://orcid.org/0000-0002-5334-3969>

Tawfeeq Shekh-Ahmad: <https://orcid.org/0000-0002-6165-2219>

Gabriele Lignani: <https://orcid.org/0000-0002-3963-9296>

Daniel Bush: <https://orcid.org/0000-0002-5097-8117>

Matthew C Walker: <https://orcid.org/0000-0002-0812-0352>

References

Bagshaw AP, Jacobs J, LeVan P, Dubeau F, Gotman J (2009) Effect of sleep stage on interictal high-frequency oscillations recorded from depth macroelectrodes in patients with focal epilepsy. *Epilepsia* **50**:617-628 <https://doi.org/10.1111/j.1528-1167.2008.01784.x>

- Bénar CG**, Chauvière L, Bartolomei F, Wendling F (2010) Pitfalls of high-pass filtering for detecting epileptic oscillations: A technical note on “false” ripples. *Clinical Neurophysiology* **121**:301-310 <https://doi.org/10.1016/j.clinph.2009.10.019>
- Bennett MVL**, Zukin SR (2004) Electrical Coupling and Neuronal Synchronization in the Mammalian Brain. *Neuron* **41**:495-511 [https://doi.org/10.1016/s0896-6273\(04\)00043-1](https://doi.org/10.1016/s0896-6273(04)00043-1)
- Bragin A**, Engel Jr J, Wilson CL, Fried I, Mathern GW (1999) Hippocampal and entorhinal cortex high-frequency oscillations (100-500 Hz) in human epileptic brain and in kainic acid-treated rats with chronic seizures. *Epilepsia* **40** <https://doi.org/10.1111/j.1528-1157.1999.tb02065.x>
- Bragin A**, Wilson CL, Engel J (2000) Chronic Epileptogenesis Requires Development of a Network of Pathologically Interconnected Neuron Clusters: A Hypothesis. *Epilepsia* **41**:S144-S152 <https://doi.org/10.1111/j.1528-1157.2000.tb01573.x>
- Cohen MX** (2017) Where Does EEG Come From and What Does It Mean?. *Trends in Neurosciences* **40**:208-218 <https://doi.org/10.1016/j.tins.2017.02.004>
- Curot J**, Barbeau E, Despouy E, Denuelle M, Sol JC, Lotterie J-A, Valton L, Peyrache A (2023) Local neuronal excitation and global inhibition during epileptic fast ripples in humans. *Brain* **146**:561-575 <https://doi.org/10.1093/brain/awac319>
- Demont-Guignard S**, Benquet P, Gerber U, Biraben A, Martin B, Wendling F (2012) Distinct hyperexcitability mechanisms underlie fast ripples and epileptic spikes. *Annals of Neurology* **71**:342-352 <https://doi.org/10.1002/ana.22610>
- Dimakopoulos V**, Gotman J, Klimes P, Von Ellenrieder N, Tan SB, Smith G, Gliske S, Maltseva M, Manalo MK, Pail M, *et al.* (2024) Multicentre analysis of seizure outcome predicted by removal of high frequency oscillations. *Brain* awae361 <https://doi.org/10.1093/brain/awae361>
- Draguhn A**, Traub R, Schmitz D, Jefferys J (1998) Electrical coupling underlies high-frequency oscillations in the hippocampus in vitro. *Nature* **394**:189-92 <https://doi.org/10.1038/28184>
- Dümpelmann M**, Jacobs J, Schulze-Bonhage A (2015) Temporal and spatial characteristics of high frequency oscillations as a new biomarker in epilepsy. *Epilepsia* **56**:197-206 <https://doi.org/10.1111/epi.12844>
- Duncan JS**, Sander JW, Sisodiya SM, Walker MC (2006) Adult epilepsy. *The Lancet* **367**:1087-100 [https://doi.org/10.1016/S0140-6736\(06\)68477-8](https://doi.org/10.1016/S0140-6736(06)68477-8)
- Dzhala VI**, Staley KJ (2004) Mechanisms of Fast Ripples in the Hippocampus. *The Journal of Neuroscience* **24**:8896-8906 <https://doi.org/10.1523/JNEUROSCI.3112-04.2004>
- Ewen JB**, Babiloni C, Collins GS, Ethridge LE, Gotman J, Ikeda A, Karoly PJ, Potter WZ, Rampp S, Seeck M, *et al.* (2025) The GREENBEAN checklist for reporting studies evaluating the effectiveness of EEG-based biomarkers. *Clinical Neurophysiology* **176**:2110777 <https://doi.org/10.1016/j.clinph.2025.2110777>
- Fabo D**, Bokodi V, Szabó J-P, Tóth E, Salami P, Keller CJ, Hajnal B, Thesen T, Devinsky O, Doyle W, *et al.* (2023) The role of superficial and deep layers in the generation of high frequency oscillations and interictal epileptiform discharges in the human cortex. *Scientific Reports* **13**:9620 <https://doi.org/10.1038/s41598-022-22497-2>
- Fedele T**, Tzovara A, Steiger B, Hilfiker P, Grunwald T, Stieglitz L, Jokeit H, Sarnthein J (2020) The relation between neuronal firing, local field potentials and hemodynamic activity in the human amygdala in response to aversive dynamic visual stimuli. *NeuroImage* **213**:116705 <https://doi.org/10.1016/j.neuroimage.2020.116705>
- Foffani G**, Uzcategui YG, Gal B, Menendez de la Prida L (2007) Reduced Spike-Timing Reliability Correlates with the Emergence of Fast Ripples in the Rat Epileptic Hippocampus. *Neuron* **55**:930-941 <https://doi.org/10.1016/j.neuron.2007.07.040>
- Frauscher B**, Ellenrieder N, Dubeau F, Gotman J (2016) EEG desynchronization during phasic REM sleep suppresses interictal epileptic activity in humans. *Epilepsia* **57**:879-888 <https://doi.org/10.1111/epi.13389>

- Gliske SV**, Irwin ZT, Chestek C, Hegeman GL, Brinkmann B, Sagher O, Garton HJL, Worrell GA, Stacey WC (2018) Variability in the location of high frequency oscillations during prolonged intracranial EEG recordings. *Nature Communications* **9**:2155 <https://doi.org/10.1038/s41467-018-04549-2>
- Harris KD**, Quiroga RQ, Freeman J, Smith SL (2016) Improving data quality in neuronal population recordings. *Nature Neuroscience* **19**:1165-1174 <https://doi.org/10.1038/nn.4365>
- Henery CC**, Mayhew TM (1989) The cerebrum and cerebellum of the fixed human brain: efficient and unbiased estimates of volumes and cortical surface areas. *Journal of Anatomy* [PubMed](#)
- Herculano-Houzel S** (2009) The human brain in numbers: a linearly scaled-up primate brain. *Frontiers in Human Neuroscience* **3** <https://doi.org/10.3389/neuro.09.031.2009>
- Hürkey S**, Niemeyer N, Schleimer J-H, Ryglewski S, Schreiber S, Duch C (2023) Gap junctions desynchronize a neural circuit to stabilize insect flight. *Nature* **618**:118-125 <https://doi.org/10.1038/s41586-023-06099-0>
- Ibarz JM**, Foffani G, Cid E, Inostroza M, Menendez de la Prida L (2010) Emergent Dynamics of Fast Ripples in the Epileptic Hippocampus. *Journal of Neuroscience* **30**:16249-16261 <https://doi.org/10.1523/JNEUROSCI.3357-10.2010>
- Jacobs J**, LeVan P, Chander R, Hall J, Dubeau F, Gotman J (2008) Interictal high-frequency oscillations (80-500 Hz) are an indicator of seizure onset areas independent of spikes in the human epileptic brain. *Epilepsia* **49**:1893-1907 <https://doi.org/10.1111/j.1528-1167.2008.01656.x>
- Jacobs J**, Zijlmans M, Zelmann R, Chatillon C-É, Hall J, Olivier A, Dubeau F, Gotman J (2010) High-frequency electroencephalographic oscillations correlate with outcome of epilepsy surgery. *Annals of Neurology* **67**:209-220 <https://doi.org/10.1002/ana.21847>
- Keles U**, Dubois J, Le KJM, Tyszka JM, Kahn DA, Reed CM, Chung JM, Mamelak AN, Adolphs R, Rutishauser U (2024) Multimodal single-neuron, intracranial EEG, and fMRI brain responses during movie watching in human patients. *Scientific Data* **11**:214 <https://doi.org/10.1038/s41597-024-03029-1>
- Kim J**, Koo B-K, Knoblich JA (2020) Human organoids: model systems for human biology and medicine. *Nature Reviews Molecular Cell Biology* **21**:571-584 <https://doi.org/10.1038/s41580-020-0259-3>
- Klimes P**, Cimbalka J, Brazdil M, Hall J, Dubeau F, Gotman J, Frauscher B (2019) NREM sleep is the state of vigilance that best identifies the epileptogenic zone in the interictal electroencephalogram. *Epilepsia* **60**:2404-2415 <https://doi.org/10.1111/epi.16377>
- Köhling R**, Staley K (2011) Network mechanisms for fast ripple activity in epileptic tissue. *Epilepsy Research* **97**:318-323 <https://doi.org/10.1016/j.eplepsyres.2011.03.006>
- Krumholz A**, Wiebe S, Gronseth GS, Gloss DS, Sanchez AM, Kabir AA, Liferidge AT, Martello JP, Kanner AM, Shinnar S (2015) Evidence-based guideline: Management of an unprovoked first seizure in adults. *Neurology* **84**:1705-13 <https://doi.org/10.1212/WNL.0000000000001487>
- Lambert I**, Tramon-Negre E, Lagarde S, Roehri N, Giusiano B, Trebuchon-Da Fonseca A, Carron R, Benar C, Felician O, Bartolomei F. (2020) Hippocampal Interictal Spikes during Sleep Impact Long-Term Memory Consolidation. *Annals of Neurology* <https://doi.org/10.1002/ana.25744>
- Lancaster G**, Iatsenko D, Pidde A, Ticcinelli V, Stefanovska A. (2018) Surrogate data for hypothesis testing of physical systems. *Physics Reports* **748** <https://doi.org/10.1016/j.physrep.2018.06.001>
- Lévesque M**, Bortel A, Gotman J, Avoli M (2011) High-frequency (80–500Hz) oscillations and epileptogenesis in temporal lobe epilepsy. *Neurobiology of Disease* **42**:231-241 <https://doi.org/10.1016/j.nbd.2011.01.007>
- Liebe S**, Niediek J, Pals M, Reber TP, Faber J, Boström J, Elger CE, Macke JH, Mormann F (2025) Phase of firing does not reflect temporal order in sequence memory of humans and recurrent neural networks. *Nature Neuroscience* <https://doi.org/10.1038/s41593-025-01893-7>
- Lisgaras CP**, Scharfman HE (2023) High-frequency oscillations (>250–500 Hz) in animal models of Alzheimer’s disease and two animal models of epilepsy. *Epilepsia* **64**:231-246 <https://doi.org/10.1111/epi.17462>

- Liu S, Gurses C, Sha Z, Quach MM, Sencer A, Bebek N, Curry DJ, Prabhu S, Tummala S, Henry TR, *et al.* (2018) Stereotyped high-frequency oscillations discriminate seizure onset zones and critical functional cortex in focal epilepsy. *Brain* **141**:713-730 <https://doi.org/10.1093/brain/awx374>
- Logothetis NK (2002) The neural basis of the blood–oxygen–level–dependent functional magnetic resonance imaging signal. *Philosophical Transactions of the Royal Society of London Series B: Biological Sciences* **357**:1003-1037 <https://doi.org/10.1098/rstb.2002.1114>
- Manning JR, Jacobs J, Fried I, Kahana MJ (2009) Broadband Shifts in Local Field Potential Power Spectra Are Correlated with Single-Neuron Spiking in Humans. *The Journal of Neuroscience* **29**:13613-13620 <https://doi.org/10.1523/JNEUROSCI.2041-09.2009>
- Mégevand P, Spinelli L, Genetti M, Brodbeck V, Momjian S, Schaller K, Michel CM, Vuilleumoz S, Seeck M (2014) Electric source imaging of interictal activity accurately localises the seizure onset zone. *Journal of Neurology, Neurosurgery & Psychiatry* **85**:38-43 <https://doi.org/10.1136/jnnp-2013-305515>
- Melani F, Zemann R, Mari F, Gotman J (2013) Continuous High Frequency Activity: A peculiar SEEG pattern related to specific brain regions. *Clinical Neurophysiology* **124**:1507-1516 <https://doi.org/10.1016/j.clinph.2012.11.016>
- Menendez de la Prida L, Staba RJ, Dian JA (2015) Conundrums of High-Frequency Oscillations (80–800 Hz) in the Epileptic Brain: Journal of Clinical Neurophysiology. *J Clin Neurophysiol* **32**:207-219 <https://doi.org/10.1097/WNP.0000000000000150>
- Minthe A, Janzarik WG, Lachner-Piza D, Reinacher P, Schulze-Bonhage A, Dümpelmann M, Jacobs J (2020) Stable high frequency background EEG activity distinguishes epileptic from healthy brain regions. *Brain Communications* **2**:fcaa107 <https://doi.org/10.1093/braincomms/fcaa107>
- Miyawaki H, Watson BO, Diba K (2019) Neuronal firing rates diverge during REM and homogenize during non-REM. *Scientific Reports* **9**:689 <https://doi.org/10.1038/s41598-018-36710-8>
- Nevalainen P, von Ellenrieder N, Klimeš P, Dubeau F, Frauscher B, Gotman J (2020) Association of fast ripples on intracranial EEG and outcomes after epilepsy surgery. *Neurology* **95**:e2235-e2245 <https://doi.org/10.1212/WNL.00000000000010468>
- Osorio-Forero A, Foustoukos G, Cardis R, Cherrad N, Devenoges C, Fernandez LMJ, Lüthi A (2024) Infralow noradrenergic locus coeruleus activity fluctuations are gatekeepers of the NREM–REM sleep cycle. *Nature Neuroscience* <https://doi.org/10.1038/s41593-024-01822-0>
- Padmasola GP, Friscourt F, Rigoni I, Vuilleumoz S, Schaller K, Michel CM, Sheybani L, Quairiaux C (2024) Involvement of the contralateral hippocampus in ictal-like but not interictal epileptic activities in the kainate mouse model of temporal lobe epilepsy. *Epilepsia* <https://doi.org/10.1111/epi.17970>
- Quiroga RQ, Nadasdy Z, Ben-Shaul Y (2004) Unsupervised Spike Detection and Sorting with Wavelets and Superparamagnetic Clustering. *Neural Computation* **16**:1661-1687 <https://doi.org/10.1162/089976604774201631>
- Racine RJ (1972) Modification of seizure activity by electrical stimulation: II. Motor seizure. *Electroencephalography and Clinical Neurophysiology* **32**:281-294 [https://doi.org/10.1016/0013-4694\(72\)90177-0](https://doi.org/10.1016/0013-4694(72)90177-0)
- Ray S, Crone NE, Niebur E, Franaszczuk PJ, Hsiao SS (2008) Neural Correlates of High-Gamma Oscillations (60-200 Hz) in Macaque Local Field Potentials and Their Potential Implications in Electroencephalography. *Journal of Neuroscience* **28**:11526-11536 <https://doi.org/10.1523/JNEUROSCI.2848-08.2008>
- Roehri N, Lina J-M, Mosher JC, Bartolomei F, Bénar C-G (2016) Time-Frequency Strategies for Increasing High-Frequency Oscillation Detectability in Intracerebral EEG. *IEEE Transactions on Biomedical Engineering* **63**:2595-2606 <https://doi.org/10.1109/TBME.2016.2556425>
- Roehri N, Pizzo F, Bartolomei F, Wendling F, Bénar C-G (2017) What are the assets and weaknesses of HFO detectors? A benchmark framework based on realistic simulations. *PLOS One* **12**:e0174702 <https://doi.org/10.1371/journal.pone.0174702>

- Roehri N, Pizzo F, Lagarde S, Lambert I, Nica A, McGonigal A, Giusiano B, Bartolomei F, Bénar C-G (2018) High-Frequency Oscillations Are Not Better Biomarkers of Epileptogenic Tissues Than Spikes. *Annals of Neurology* **83**:84-97 <https://doi.org/10.1002/ana.25124>
- Roehri N, Vulliemoz S, Lagarde S (2024) The challenge of assessing invasive biomarkers for epilepsy surgery. *Brain* **147**:e52-e54 <https://doi.org/10.1093/brain/awae164>
- Saglam-Metiner P, Yildirim E, Dincer C, Basak O, Yesil-Celiktas O (2024) Humanized brain organoids-on-chip integrated with sensors for screening neuronal activity and neurotoxicity. *Microchimica Acta* **191**:71 <https://doi.org/10.1007/s00604-023-06165-4>
- Sanchez-Vives MV, McCormick DA (2000) Cellular and network mechanisms of rhythmic recurrent activity in neocortex. *Nature Neuroscience* **3**:1027-1034 <https://doi.org/10.1038/79848>
- Schlingloff D, Freund TF, Hangya B, Gulyás A (2025) Collapsing Perisomatic Inhibition Leads to Epileptic Fast-Ripple Oscillations Caused by Pseudosynchronous Firing of CA3 Pyramidal Neurons. *The Journal of Neuroscience* **45**:e0500252025 <https://doi.org/10.1523/JNEUROSCI.0500-25.2025>
- Schmitz D, Schuchmann S, Fisahn A, Draguhn A, Buhl EH, Petrasch-Parwez E, Dermietzel R, Heinemann U, Traub RD (2001) Axo-axonal coupling: a novel mechanism for ultrafast neuronal communication. *Neuron* **31**:831-840 [https://doi.org/10.1016/s0896-6273\(01\)00410-x](https://doi.org/10.1016/s0896-6273(01)00410-x)
- Schönberger J, Knopf A, Klotz KA, Dümpelmann M, Schulze-Bonhage A, Jacobs J (2021) Distinction of Physiologic and Epileptic Ripples: An Electrical Stimulation Study. *Brain Sciences* **11**:538 <https://doi.org/10.3390/brainsci11050538>
- Shamas M, Yeh HJ, Fried I, Engel J, Staba RJ (2023) High-rate leading spikes in propagating spike sequences predict seizure outcome in surgical patients with temporal lobe epilepsy. *Brain Communications* **5**:fcad289 <https://doi.org/10.1093/braincomms/fcad289>
- Shandilya MCV, Addo-Osafo K, Ranasinghe KG, Shamas M, Staba R, Nagarajan SS, Vossel K (2024) High-frequency oscillations in epileptic and non-epileptic Alzheimer's disease patients and the differential effect of levetiracetam on the oscillations. *Brain Communications* **7** <https://doi.org/10.1093/braincomms/fcaf041>
- Sheybani L, Birot G, Contestabile A, Seeck M, Kiss JZ, Schaller K, Michel CM, Quairiaux C (2018) Electrophysiological Evidence for the Development of a Self-Sustained Large-Scale Epileptic Network in the Kainate Mouse Model of Temporal Lobe Epilepsy. *The Journal of Neuroscience* **38**:3776-3791 <https://doi.org/10.1523/JNEUROSCI.2193-17.2018>
- Sheybani L, Frauscher B, Bernard C, Walker M (2025a) Mechanistic insights into the interaction between epilepsy and sleep. *Nature Reviews Neurology* <https://doi.org/10.1038/s41582-025-01064-z>
- Sheybani L, van Mierlo P, Birot G, Michel CM, Quairiaux C (2019) Large-Scale 3–5 Hz Oscillation Constrains the Expression of Neocortical Fast Ripples in a Mouse Model of Mesial Temporal Lobe Epilepsy. *eNeuro* **6** <https://doi.org/10.1523/ENEURO.0494-18.2019>
- Sheybani L, Vivekananda U, Rodionov R, Diehl B, Chowdhury FA, McEvoy AW, Miserocchi A, Bisby JA, Bush D, Burgess N, et al. (2023) Wake slow waves in focal human epilepsy impact network activity and cognition. *Nature Communications* **14**:7397 <https://doi.org/10.1038/s41467-023-42971-3>
- Sheybani L, Vivekananda U, Sinha N, Conrad E, Litt B, Burgess N, Bush D, Walker MC (2025b) Dynamic Interplay Between Wake Slow Waves and Epileptiform Discharges in the Epileptogenic Zone. *Neurology* **105**:e214001 <https://doi.org/10.1212/WNL.0000000000214001>
- Staba RJ (2012) Normal and Pathologic High-Frequency Oscillations. In: Noebels JL, Avoli M, Rogawski MA, et al (Eds). *Jasper's Basic Mechanisms of the Epilepsies* (4th edition)
- Staba RJ, Wilson CL, Bragin A, Fried I, Engel J (2002) Sleep States Differentiate Single Neuron Activity Recorded from Human Epileptic Hippocampus, Entorhinal Cortex, and Subiculum. *The Journal of Neuroscience* **22**:5694-5704 <https://doi.org/10.1523/JNEUROSCI.22-13-05694.2002>
- Timofeev I, Chauvette S (2017) Sleep slow oscillation and plasticity. *Current Opinion in Neurobiology* **44**:116-126 <https://doi.org/10.1016/j.conb.2017.03.019>

- Traub RD, Whittington MA, Buhl EH, LeBeau FEN, Bibbig A, Boyd S, Cross H, Baldeweg T (2001) A Possible Role for Gap Junctions in Generation of Very Fast EEG Oscillations Preceding the Onset of, and Perhaps Initiating, Seizures. *Epilepsia* **42**:153-170 <https://doi.org/10.1046/j.1528-1157.2001.26900.x>
- Valero M, Averkin RG, Fernandez-Lamo I, Aguilar J, Lopez-Pigozzi D, Brotons-Mas JR, Cid E, Tamas G, Menendez de la Prida L. (2017) Mechanisms for Selective Single-Cell Reactivation during Offline Sharp-Wave Ripples and Their Distortion by Fast Ripples. *Neuron* **94**:1234-1247.e7. <https://doi.org/10.1016/j.neuron.2017.05.032>
- Van Schalkwijk FJ, Helfrich RF (2026) Aperiodic 1/f noise drives ripple activity in humans. *Nature Communications* **17**:746 <https://doi.org/10.1038/s41467-026-68404-5>
- Von Ellenrieder N, Dubeau F, Gotman J, Frauscher B (2017) Physiological and pathological high-frequency oscillations have distinct sleep-homeostatic properties. *NeuroImage: Clinical* **14**:566-573 <https://doi.org/10.1016/j.nicl.2017.02.018>
- von Ellenrieder N, Frauscher B, Dubeau F, Gotman J (2016) Interaction with slow waves during sleep improves discrimination of physiologic and pathologic high-frequency oscillations (80-500 Hz). *Epilepsia* **57**:869-878 <https://doi.org/10.1111/epi.13380>
- Vossel KA, Ranasinghe KG, Beagle AJ, Mizuiri D, Honma SM, Dowling AF, Darwish SM, Van Berlo V, Barnes DE, Mantle M, et al. (2016) Incidence and impact of subclinical epileptiform activity in Alzheimer's disease. *Annals of Neurology* **80**:858-870 <https://doi.org/10.1002/ana.24794>
- Watson BO, Levenstein D, Greene JP, Gelinas JN, Buzsáki G (2016) Network Homeostasis and State Dynamics of Neocortical Sleep. *Neuron* **90**:839-852 <https://doi.org/10.1016/j.neuron.2016.03.036>
- Woodcock S, Falletta J (2024) A numerical evaluation of the Finite Monkeys Theorem. *Franklin Open* **9**:e100171 <https://doi.org/10.1016/j.fraope.2024.100171>
- Ylinen A, Bragin A, Nadasdy Z, Jando G, Szabo I, Sik A, Buzsaki G (1995) Sharp Wave-Associated High-Frequency Oscillation (200 Hz) in the Intact Hippocampus-Network and Intracellular Mechanisms. *Journal of Neuroscience* **15**:30-46 <https://doi.org/10.1523/JNEUROSCI.15-01-00030.1995>
- Zanos TP, Mineault PJ, Pack CC (2011) Removal of Spurious Correlations Between Spikes and Local Field Potentials. *Journal of Neurophysiology* **105**:474-486 <https://doi.org/10.1152/jn.00642.2010>
- Zijlmans M, Jacobs J, Zelmann R, Dubeau F, Gotman J (2009) High-frequency oscillations mirror disease activity in patients with epilepsy. *Neurology* **72**:979-986 <https://doi.org/10.1212/01.wnl.0000344402.20334.81>
- Zijlmans M, Jiruska P, Zelmann R, Leijten FSS, Jefferys JGR, Gotman J (2012) High-frequency oscillations as a new biomarker in epilepsy. *Annals of Neurology* **71**:169-178 <https://doi.org/10.1002/ana.22548>
- Zijlmans M, Zweiphenning W, Van Klink N (2019) Changing concepts in presurgical assessment for epilepsy surgery. *Nature Reviews Neurology* **15**:594-606 <https://doi.org/10.1038/s41582-019-0224-y>
- Zweiphenning W, Klooster MAV 'T, Van Klink NEC, Leijten FSS, Ferrier CH, Gebbink T, Huiskamp G, Van Zandvoort MJE, Van Schooneveld MMJ, Bourez M, et al. (2022) Intraoperative electrocorticography using high-frequency oscillations or spikes to tailor epilepsy surgery in the Netherlands (the HFO trial): a randomised, single-blind, adaptive non-inferiority trial. *The Lancet Neurology* **21**:982-993 [https://doi.org/10.1016/S1474-4422\(22\)00311-8](https://doi.org/10.1016/S1474-4422(22)00311-8)

Peer reviews

Reviewer #1 (Public review):

Summary:

This is a study utilizing several types of analyses (computational modeling, neuronal cultures, rodent epilepsy model, and human intracranial multi-scale recordings) to address a highly relevant conceptual question: Are fast ripples (FRs) distinct pathological entities or largely

emergent products of stochastic spike clustering? The results can potentially reshape current approaches to incorporating fast ripples into the epilepsy surgery evaluation.

Strengths:

The conceptualization of fast ripples as potentially arising by chance is highly novel and builds effectively on questions raised in prior studies that have never been satisfactorily resolved.

The integration across biological scales and models is a major strength. The state dependency analysis provides additional, strong support. The methodology and statistical approaches used are thoughtfully presented and rigorously applied.

In particular, this paper provides a strong response to the findings from Gliske et al, Nat Commun 2018. This study utilized long-term data analysis to uncover low rates of FRs detected from most recording sites, suggesting spurious detections, although FRs were concentrated within seizure onset areas.

Weaknesses:

The authors clearly aimed to use a statistical rather than a mechanism-based approach in this work. However, the paper's framing of true fast ripples as oscillatory events with stochastic fast ripples considered as confounders does not take prior investigations into biological mechanisms, particularly prior studies that point to an important role for stochastic fast ripples in some contexts. Incorporating recognition of these mechanisms would strengthen the manuscript and provide a more complete and nuanced characterization.

Some examples from the literature:

Eissa et al, eNeuro 2016, a paper that closely parallels this manuscript but took a mechanistic rather than statistical approach, showed that fast ripples can arise from population paroxysmal depolarizations - a key feature of epileptiform discharges - as temporally clustered, jittered population firing, with FRs appearing in LFP or EEG due to summated postsynaptic potentials (which are slower than action potentials and can generate signals in the high gamma range).

Foffani et al., 2007, Neuron, and Ibarz et al., 2010, J Neurosci, argue that FRs are pseudo-oscillations created by jittered neuronal populations in the setting of altered spike timing.

Smith et al., 2020, Sci Rep, contrasts FR characteristics in different regimes, i.e., intact inhibition early in a seizure vs. implied collapse of inhibition after recruitment. Schlingloff et al., 2025, J Neurosci, reported analogous findings in an animal model.

The computational model and subtraction approach provide a strong case for the random emergence of clustered activity in the high gamma band, given its assumptions. However, any such modeling effort needs to account for inhibitory activity, including impaired inhibitory function that is expected in epileptic brain regions, which has a strong modulating effect on excitatory firing and is thought to play a significant role in FR generation.

The shuffling procedure aims to preserve the power spectrum but randomizes high frequency phase (>200 Hz). However, this procedure removes biologically meaningful spike timing correlations, as well as structured cross-frequency coupling. The subtraction method thus likely underestimates the incidence of structured "distinct" FRs, while perhaps overestimating "chance" FRs due to biologically infeasible activity, making the statement that most FRs are due to chance correlation too strong.

The kainate findings underscore this point: the increase in the number of FR detections could be, as the authors state, an increase in chance clustering due to increased network

excitability generally. However, the likelihood of a parallel increase in pathological FRs cannot be ruled out, given likely pro-epileptic alterations in spike timing and circuit function.

<https://doi.org/10.7554/eLife.110803.1.sa2>

Reviewer #2 (Public review):

Summary:

This paper asks an important question that has not been discussed much in the extensive literature on the High Frequency Oscillations (HFOs) that have been extensively studied in patients with epilepsy and experimental models of epilepsy. The question is whether the Fast Ripples (FRs), the HFOs in the 250-500 Hz frequency band, represent a pathological phenomenon or represent a physiological phenomenon that occurs in the healthy brain but happens to be more frequent in epileptic tissue. It is an important question that has not been systematically addressed until now. The authors conclude, from very extensive simulations, from extensive experimental animal studies (the systemic kainate model of epilepsy in rats), and from a modest amount of human data, that FRs occur in healthy brains as a result of the chance occurrence of bursts of action potentials, and that in epileptic tissue, their frequency of occurrence is approximately 30% higher than what is expected by chance. They conclude that FRs are not a separate phenomenon of epileptic tissue. This finding is reinforced by the recent findings of FRs in experimental models of Alzheimer's disease.

Strengths:

This is a valuable study because it asks an important and original question and because it evaluates it from several angles (simulation, tissue culture, experimental animals, and human patients). The simulations and the analyses of real data are performed very carefully and with original and solidly documented approaches, using extensive simulations and extensive data sets in the cultured cell data and in the in vivo experiments. The paper is clearly written and well-illustrated.

Weaknesses:

I found only one serious weakness in this study, but it is one that is of importance. Although the original work on FRs was done in an experimental model of epilepsy, the field really became prominent when ripples and fast ripples were found first in microelectrode recordings of epileptic patients and then in the intracerebral EEG of such patients. Numerous studies have been performed since then, with a valuable meta-analysis including 700 patients (Wang Z, Guo J, van 't Klooster M, Hoogteijling S, Jacobs J, Zijlmans M. Prognostic Value of Complete Resection of the High-Frequency Oscillation Area in Intracranial EEG: A Systematic Review and Meta-Analysis. *Neurology*. 2024 May 14;102(9). Although the consensus at this point is that FRs are not the ideal and totally specific marker of epileptic tissue that many thought it could be, FRs are nevertheless much more frequent in epileptic tissue than in non-epileptic tissue and are a solid biomarker. It is also well established that they are much more frequent in NREM sleep than in wakefulness, as reported in the original paper of Staba et al (Staba RJ, Wilson CL, Bragin A, Jhung D, Fried I, Engel J Jr. High-frequency oscillations recorded in human medial temporal lobe during sleep. *Ann Neurol*. 2004 Jul;56(1):108-15., not mentioned in this paper) and in the study of Bagshaw et al (2009). In this last paper, using SEEG in various brain regions, the average rate of FRs in NREM sleep is about 6 times that in wakefulness. In the paper by Staba, with microelectrodes in mesial temporal structures, it is about twice. As a separate issue, the paper of Fraucher et al (Fraucher B, von Ellenrieder N, Zemann R, Rogers C, Nguyen DK, Kahane P, Dubeau F, Gotman J. High-Frequency Oscillations in the Normal Human Brain. *Ann Neurol*. 2018 Sep;84(3):374-385), which is not quoted, found that, in an extensive sample, non-epileptic human tissue sampled with SEEG generated extremely rare FRs (an average rate of 0.04/min/channel, i.e. 1 every 25 min).

The results above are mentioned because they do not fit with the data provided in the present study: FRs are much more frequent in NREM sleep than in wakefulness in human epileptic patients, and they are much more frequent (not 30% more, but many hundreds of percent more) in epileptic tissue than in non-epileptic human tissue. The fundamental phenomenon of interest is, I believe, the FRs in epileptic patients. The animal experiments, tissue studies, and simulations are models to study the human phenomenon. With respect to the modulation by sleep and the differentiation between epileptic and non-epileptic tissue, it seems that the systems studied in this paper are not good models of the human condition. The human results presented in the study only reflect wakefulness recordings, which is not the condition in which most HFO studies have been done and in which most HFOs occur. The authors refer to the study of long-term fluctuations in HFO rates by Gliske et al. (2018) to say that one has to be careful with the results regarding sleep, for example, Bagshaw et al (2009), but the clear predominance in of HFOs in NREM sleep has been observed by many studies. The cautions regarding fluctuations over extended periods also apply to the awake human data analyzed in this study.

The study's conclusions regarding the generation of FRs are therefore questionably applicable to the human condition. I do not dispute their validity for the models and situations in which they were studied.

<https://doi.org/10.7554/eLife.110803.1.sa1>

Reviewer #3 (Public review):

Summary:

An outstanding question in the field of high-frequency oscillations (HFOs) in the context of epilepsy is how these oscillations emerge, considering that they occur at such high frequencies, i.e., 250Hz, well above the firing ability of single neurons. One hypothesis that has been suggested in the past is that neurons that fire in an out-of-phase fashion, or rather at random intervals, may contribute to a spectrum of HFOs ranging from 250-500Hz that are observed in epilepsy. However, how possible it is that random action potentials could aggregate to the extent that they could give rise to HFOs in the so-called fast ripple (FRs) frequency range (>200 according to the authors) remains unclear. To test this hypothesis, they used computational modeling to randomly insert action potentials in a signal, and they found that this approach is sufficient to generate FRs. Some of the predictors of whether FRs could occur were neuronal count, firing rate, and synchronization. Besides computational modeling, they used different model systems to test whether that would be possible to be observed in neuronal cultures, in epileptic rats (intrahippocampal kainic acid model), and human data. Neuronal cultures treated with picrotoxin did not show evidence that FRs could be generated beyond chance aggregation of action potentials. They then asked whether synchronization and firing rate could play a role in the emergence of FRs. They found that changes in neural firing and synchronization, such as those occurring during differences phase of the sleep-wake cycle, could affect the number of FRs occurring by chance aggregation, with more FRs seen during periods of wakefulness, a result that they replicated in human data.

The authors largely achieve their proposed aims of demonstrating that random neuronal firing can, in principle, generate FRs. Results from this study could influence current thinking around mechanisms generating FRs in epilepsy. The use of different computational approaches and model systems could offer new analytical methodologies for the study of FRs in the context of brain disease.

Strengths:

- (1) The authors used a multi-level approach combining computational modeling with experimental datasets, including neuronal cultures, a rat model of temporal lobe epilepsy, and human data.
- (2) Identification of key parameters such as neuronal count, firing rate, synchronization, and brain state in observed incidence of FRs generated through random aggregation of neural firing.
- (3) Cross-species validation increases the likelihood of generalizability of the findings.

Weaknesses:

- (1) Some of the simulated FRs appear short in duration and may not meet standard detection and definition criteria, potentially influencing validity.
- (2) The neuronal culture approach does not directly test random insertion of action potentials, limiting interpretation.
- (3) Sleep is treated as a homogeneous state in the rat dataset, without accounting for stage-specific differences in synchronization, which may affect the results and interpretation.
- (4) The analyses conducted in human data lack direct comparison with sleep data.

<https://doi.org/10.7554/eLife.110803.1.sa0>